
Preparation and scoring of protein nano- and microcrystals for synchrotron and free-electron laser X-ray radiation sources

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Robin Schubert

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1. Gutachter: Prof. Christian Betzel

2. Gutachter: Prof. Henning Tidow

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PUBLICATIONS ASSOCIATED WITH THIS THESIS

Robin Schubert, Arne Meyer, Karsten Dierks, Svetlana Kapis, Rudolph Reimer, Howard Einspahr, Markus Perbandt and Christian Betzel, *Reliably distinguishing protein nanocrystals from amorphous precipitate by means of depolarized dynamic light scattering*, *Journal of Applied Crystallography* (2015) 48, 1476–1484

Robin Schubert, Svetlana Kapis, Yannig Giquel, Gleb Bourenkov, Thomas R Schneider, Michael Heymann, Christian Betzel, Markus Perbandt, *A multicrystal diffraction data-collection approach for studying structural dynamics with millisecond temporal resolution*. *IUCrJ* (2016). 3, 393–401

Robin Schubert, Sandra Koszak, Markus Perbandt, Rob Meijers, Stephane Boivin, *Complementarity of Thermofluor and Dynamic Light Scattering for protein buffer optimization*. In preparation for submission to the *Journal of Structural Biology*

Robin Schubert, Arne Meyer, Karsten Dierks, Markus Perbandt, Christian Betzel, *Dynamic light scattering provides new insights into the process of nucleation monitored by feedback-controlled protein crystallization*. In preparation for submission to the *Journal Angewandte Chemie*

Related publications:

Chen-Yan Zhang, Yan Wang, **Robin Schubert**, Yue Liu, Li-Xue Yang, Meng-Ying Wang, Hui-Meng Lu, Yong-Ming Liu, Yun-Zhu Guo, Zi-Qing Wu, Ke-An Chen, Christian Betzel, Da-Chuan Yin, *The effect of audible sound on protein crystallization*, *Crystal Growth and Design* (2016) 16 (2), 705–713

Clemens Falker, Alexander Hartmann, Inga Guett, Frank Dohler, Hermann Altmepfen, Christian Betzel, **Robin Schubert**, Dana Thurm, Florian Wegwitz, Pooja Joshi, Claudia Verderio, Susanne Krasemann, Markus Glatzel, *Exosomal PrPC drives fibrillization of amyloid beta and counteracts amyloid beta-mediated neurotoxicity*, *Journal of Neurochemistry* (2016) 137 (1), 88-100

SUMMARY

Accompanying with the construction of high brilliant X-ray radiation sources like third generation synchrotrons and free-electron lasers (FELs) it became possible to use protein micro- and nanocrystals for protein structure determination. Therefore, the interest in nano- and microcrystals increased substantially and a strong demand arose in developing new methods for preparation and scoring of protein crystals with this size. In this study, several methods related to nano- and microcrystal production and scoring could be established or adapted, including protein buffer optimization, controlled induction of nucleation, non-invasive reliable nanocrystal detection in solution and potential applications of microcrystals for X-ray crystallography at synchrotrons.

It could be demonstrated that the protein buffer composition, which is a crucial parameter for maintaining protein stability, homogeneity and purity, can be optimized in a multi-condition approach with the use of Dynamic Light Scattering (DLS). Further, it was shown that DLS and Thermofluor provide complementary information and thus both methods should be combined in order to identify an ideal buffer composition that fulfils all criteria known to be beneficial for crystal formation.

Furthermore, DLS was used to obtain new information about the nucleation process of macromolecules. The growth kinetics of protein clusters were analyzed and revealed that the rate of mass-transport during cluster evolution is mainly diffusion-limited. The obtained results support the proposed theory of a two-step mechanism of nucleation and might demonstrate the first microscopic evidence of a transition from a cluster with high protein concentration to a crystal with higher structural order. Further, it was shown that DLS measurements can also be performed in micro-sized cavities of microfluidic devices and might circumvent the current limitation that the qualitative and quantitative evaluation of the crystallization process in microfluidic devices is solely based on visual inspection using a light microscope.

Beyond that, a novel and unique non-invasive and non-destructive method called Depolarized Dynamic Light Scattering (DDLS) could be established, which is capable of identifying nanocrystals in solution and allows following the nucleation and early stages of protein crystallization in real time. The obtained results provide clear evidence, that DDLS allows distinguishing between well-ordered crystalline particles and amorphous protein aggregates online during the crystallization process.

Additional emphasis was placed on developing new promising applications of microcrystals for data collection at synchrotrons. A simple fixed target approach and data collection protocol was established that allows the rapid collection of complete diffraction data sets from less than 50 microcrystals at room-temperature. Due to the high temporal resolution of 40 milliseconds between each dataset, dynamic processes like site-specific or global radiation damage and potentially also chemical reactions,

catalyzed by biological macromolecules, can be followed using this approach. Furthermore, it was shown that site-specific X-ray radiation damage can be used for phasing a multi-microcrystal diffraction dataset, when recording diffraction data at cryogenic temperature. This is particularly interesting, because it was not known if the non-isomorphism from multiple crystals would disguise the differences in structure factors upon induced radiation damage.

Accessorily, the structure of aminopeptidase P (APP) from the human malaria parasite *Plasmodium falciparum* was solved to high resolution using X-ray crystallography. The APP exhibits a three-domain architecture and was found as a homodimer in the crystal as well as in solution. The resulting structural APP model shows a high structural homology to human APP and *Caenorhabditis elegans* APP and in particular, the active site with a di-nuclear manganese cluster is highly conserved. The information indicates that *P. falciparum* and human APP share a common mode of substrate binding and a similar catalytic mechanism. The results contribute and support the development of antimalarial drugs.

ZUSAMMENFASSUNG

Einhergehend mit der Entwicklung von hoch brillanten Röntgenquellen wie Synchrotrons der dritten Generation und Freien-Elektronen Lasern (FELs) wurde es möglich, Nano- und Mikrokristalle zur Strukturaufklärung von Proteinen zu verwenden. Daher nahm das Interesse an Nano- und Mikrokristallen substantiell zu und es entstand ein großer Bedarf an der Entwicklung von neuen Methoden für deren Herstellung und Qualitätsabschätzung. Im Rahmen dieser Promotionsarbeit wurden mehrere Methoden entwickelt oder adaptiert, die sich mit der Nano- und Mikrokristallherstellung und -identifizierung beschäftigen. Dies umfasst Methoden zur Pufferoptimierung, zur kontrollierten Induktion der Nukleation und zur nicht-invasiven verlässlichen Detektion von Nanokristallen in Lösung, sowie möglichen Anwendungen von Mikrokristallen für die Diffraktionsdatensammlung an Synchrotrons.

Es konnte gezeigt werden, dass die Pufferzusammensetzung, die einen entscheidenden Parameter für den Erhalt der Proteinstabilität, -homogenität und -reinheit darstellt, in einem multifunktionalen Ansatz unter Verwendung der dynamischen Lichtstreuung (DLS) optimiert werden kann. Außerdem wurde gezeigt, dass mittel DLS und Thermofluor komplementäre Informationen erhalten werden. Daher sollten beide Methoden kombiniert werden, um eine Pufferzusammensetzung, die alle für die Kristallisation vorteilhaften Kriterien erfüllt, zu identifizieren. Des Weiteren wurde DLS verwendet, um neue Informationen über den Nukleationsprozess von Makromolekülen zu gewinnen. Es wurde die Wachstumskinetik von Proteinclustern analysiert und die Ergebnisse zeigten, dass der Massenzuwachs während der Cluster-Evolution hauptsächlich diffusionslimitiert ist. Die erhaltenen Ergebnisse unterstützen zudem die Hypothese eines Zwei-Schritt-Mechanismus der Nukleation und stellen möglicherweise den ersten mikroskopischen Nachweis eines Übergangs von einem Cluster mit hoher Proteindichte zu einem Cluster mit hoher struktureller Ordnung dar. Zudem konnte gezeigt werden, dass DLS Messungen ebenfalls in den kleinen Kavitäten eines Mikrofluidikchips durchgeführt werden können. Die derzeitige Einschränkung von Mikrofluidik Anordnungen ist, dass die qualitative und quantitative Evaluation des Kristallisationsprozesses nur aufgrund einer visuellen Begutachtung mit Hilfe eines Lichtmikroskops durchgeführt werden kann. Durch den Einsatz von DLS kann diese Limitierung nun umgangen werden.

Darüber hinaus wurde eine einzigartige nicht-invasive und nicht-destruktive Methode basierend auf dem Prinzip der depolarisierten dynamischen Lichtstreuung (DDLS) etabliert. DDLS ermöglicht es, Nanokristalle in Lösung zu identifizieren und deren frühzeitiges Wachstum während der Kristallisation in Echtzeit zu verfolgen. Zudem zeigen die erhaltenen Ergebnisse, dass eine Unterscheidung zwischen

kristallinen Partikeln mit hoher intrinsischer Ordnung und amorphen Aggregaten während des Kristallisationsprozesses mit Hilfe von DDLS möglich ist.

Ein weiterer Schwerpunkt wurde auf die Entwicklung von neuen vielversprechenden Anwendungen von Mikrokristallen zur Datensammlung an Synchrotrons gelegt. Es wurde ein Ansatz zur Probenmontage sowie eines Datensammelprotokolls etabliert, über den mit kurzem Zeitaufwand vollständige Datensätze von Mikrokristallen bei Raumtemperatur gesammelt werden können. Der Ansatz zeichnet sich dadurch aus, dass eine zeitliche Auflösung von 40 Millisekunden zwischen den einzelnen Datensätzen erreicht wird. Dies ermöglicht die Verfolgung von dynamischen Prozessen wie ortsspezifischem und globalem Strahlenschaden oder die Beobachtung von chemischen Reaktionen, die über Enzyme katalysiert werden. Darüber hinaus wurde demonstriert, dass die Phaseninformation eines bei kryogenen Temperaturen aufgenommenen Multi-Mikrokristall-Diffraktionsdatensatzes anhand von ortsspezifischem Strahlenschaden ermittelt werden kann. Dies ist im Besonderen interessant, da bislang unklar war, ob der Nicht-Isomorphismus zwischen den einzelnen Kristallen die durch den Strahlenschaden hervorgerufenen Unterschiede in den Strukturparametern überlagern würde.

Zusätzlich wurde die Röntgenstruktur der Aminopeptidase P (APP) des humanen Malariaerregers *Plasmodium falciparum* zu hoher Auflösung aufgeklärt. Es zeigte sich, dass APP aus drei Domänen aufgebaut ist und sowohl im Kristall als auch in Lösung als Dimer vorliegt. Das erhaltene Strukturmodell von APP weist eine hohe strukturelle Homologie zu humanem APP und zu APP von *Caenorhabditis elegans* auf. Besonders das aktive Zentrum, welches ein zweikerniges Mangan-Cluster enthält, ist hoch konserviert. Die Ergebnisse weisen darauf hin, dass *P. falciparum* APP und humanes APP ein gemeinsames Muster der Substratbindung haben und ihr katalytischer Mechanismus ähnlich ist. Diese Informationen können dazu beitragen neue Wirkstoffe gegen Malaria zu entwickeln.

INTRODUCTORY PREFACE – CRYSTALLOGRAPHY TODAY

The discovery of X-rays by Wilhelm Conrad Röntgen in 1895 was of fundamental importance for the understanding of molecular processes and investigation of atomic structures (Röntgen, 1898). The era of X-ray crystallography was born in 1912 when a copper sulfate crystal was placed in the X-ray beam to test the wave-like nature of the X-rays in an experiment proposed by Max von Laue (Friedrich *et al.*, 1913). The experiment, nowadays called Laue-Crystallography, was interpreted and improved by W. L. Bragg and W. H. Bragg, who thereby solved the first crystal structure of sodium chloride in 1913 (Bragg & Bragg, 1913). This was the first technique that allows determining atomic bond distances, bond angles as well as dihedral angles and turned out to be one of the most important scientific breakthroughs in chemistry, physics and biology of the last century.

However, it took several years until the first crystal structure of a macromolecule was solved. The first enzyme, jack bean urease, was crystallized by James Sumner in 1926, but the first protein from which a crystal structure could be determined was sperm whale myoglobin in 1958 (Kendrew *et al.*, 1958). From the 1990s onwards the number of deposited macromolecular structures, archived online at the Protein Data Bank (PDB), started to grow rapidly. Today more than 120000 entries are deposited (rcsb.org). The remarkably increasing number became possible with substantial achievements in the fields of molecular biology and protein purification as well as a better understanding of the crystallization process and the constant development of improved X-ray radiation sources. Currently synchrotrons are the most commonly used radiation sources for experiments requiring high intense X-ray beams. Synchrotrons of the first generation with an electron storage ring were built in the 1970s and nowadays synchrotrons of the third generation are used. The largest and most powerful radiation sources among these are DIAMOND (Oxfordshire, England), Spring-8 (Harima Science Park City, Japan), APS (Chicago, USA), ESRF (Grenoble, France) and PETRA III (Hamburg, Germany).

In classical protein crystallography, one single protein crystal with dimensions between 50 μm and 500 μm is mounted on a goniometer at cryogenic temperature and rotated in the X-ray beam, while recording many diffraction patterns. With increasing flux of the new synchrotron radiation sources, the minimal required crystals size to measure reliable Bragg intensities at high diffraction angles constantly decreased. At modern micro-focus beamlines, a monochromatic X-ray beam is focused on a spot with a diameter about 5 μm and delivers about 10^{12} photons per second (Smith *et al.*, 2012). Such high flux densities lead to the problem, that the total X-ray dose has to be distributed by either exposing multiple positions of a single crystal (Riekkel *et al.*, 2005) or by exposing several microcrystals (Coulibaly *et al.*, 2007), in order to avoid global and specific radiation damage multiple partial datasets

are merged to obtain complete data sets. To facilitate this, a new sample mounting system for *in-situ* crystallography has been developed by McPherson in 2000 and several others were published over the last years. Among these are also many approaches to collect diffraction data at room-temperature, which have the benefit of avoiding artefacts due to the cryo-freezing process and allow studying dynamic processes. Low X-ray absorbing 96-well plates have been developed in order to reduce sample manipulation after crystal formation (Kisselman *et al.*, 2011; Axford *et al.*, 2012; Axford *et al.*, 2016). Microfluidic chips are used as X-ray compatible multilayer crystallization platforms or as counter-diffusion crystallization devices (Guha *et al.*, 2012; Pinker *et al.*, 2013; Perry *et al.*, 2013; Mueller *et al.*, 2015). Also other fixed target approaches have been tested (Coquelle *et al.*, 2015; Huang *et al.*, 2015) and capillaries have been used in which microcrystals are slowly flowing through the X-ray beam (Stellato *et al.*, 2014). All these methods facilitate the collection of complete diffraction data-sets by recording a limited number of diffraction patterns from suspensions of microcrystals.

In parallel, X-ray sources of the fourth generation have been designed and are currently constructed at several locations worldwide. These instruments are called free-electron lasers (FELs) and in contrast to synchrotrons they consist of a high-energy electron linear accelerator, equipped with very long undulators to produce X-rays in a microbunching process (Tremaine *et al.*, 2002). The emitted hard X-rays are delivered in pulses and each pulse contains up to about 10^{13} coherent photons and has a duration of 100 fs or even less. The resulting peak brilliance is about ten orders of magnitude higher compared to third-generation synchrotrons (Su *et al.*, 2015). Currently only four XFELs are in operation worldwide, the **Free Electron laser Radiation for Multidisciplinary Investigations** (FERMNI, ELETTRA, Italy), the **Free-electron LASer in Hamburg** (FLASH, DESY, Germany), the **Spring-8 Angstrom Compact free electron LAser** (SACLA, RIKEN, Japan) and the **Linac Coherent Light Source** (LCLS, SLAC, USA). But several more are under construction, like the SwissFEL at the Paul Scherrer Institute and the European XFEL in Hamburg, which will be operational in 2017. Along with these new radiation sources a revolutionary new method called serial femtosecond X-ray crystallography (SFX) has been developed (Chapman *et al.*, 2011; Schlichting, 2015; Martin-Garcia *et al.*, 2016). The first reported protein structure with high resolution determined by SFX has been published by Boutet *et al.* (Boutet *et al.*, 2012). In SFX the X-ray pulses are focused on protein micro- or nanocrystals to record the Bragg intensities (reflections). The transferred electromagnetic energy of the high intense X-ray exposure fully ionizes all atoms of the molecule and thus the crystal is destructed by a coulomb burst. However, the required exposure time for a diffraction pattern is short enough to record a single diffraction pattern before the crystal order gets lost. Therefore, this phenomenon is called *diffraction before destruction* (Chapman *et al.*, 2011; Neutze *et al.*, 2000). Consequently, only one single diffraction pattern can be recorded from each exposed crystal and several thousand different crystals have to be

exposed to X-rays in random orientation to obtain a complete dataset by merging all individual diffraction pattern (Boutet *et al.*, 2012; Liu *et al.*, 2013; White *et al.*, 2012).

In order to record sufficient amount of diffraction pattern sample delivery methods are required which allow a rapid replenishment of microcrystals in the focal point of the X-ray beam. The most successfully used method uses a gas dynamic virtual nozzle (GDVN), which focusses a liquid jet by a surrounding helium stream (DePonte *et al.*, 2008). The nozzle is based on mounting a small capillary inside a larger one. While the crystal suspension is delivered in the inner one, the outer capillary accommodates the high-pressured gas, resulting in a jet with a diameter of a few micrometer (Weierstall *et al.*, 2012). Typical problems are clogging of the nozzle, damage of fragile crystals due to sheer stress and a high sample consumption (Stevenson *et al.*, 2014a; Schlichting & Miao, 2012). To reduce the sample consumption an electrospinning liquid microjet has been developed, which uses an electric field instead of a stream of gas to focus the crystal suspension (Sierra *et al.*, 2012). The disadvantage is that the samples have to be suspended in a high viscous medium. A viscous medium like LCP is also used in slow jet injectors, where a viscous crystal suspension is extruded either with (Botha *et al.*, 2015) or without (Sugahara *et al.*, 2015) a surrounding gas stream for jet focusing. Alternatively, also solid support approaches have been tested with the benefit of a strongly increased hit rate of the X-ray beam with the protein crystal. Microfluidic devices have been used for this approach (Mueller *et al.*, 2015) as well as polymer fixed targets (Zarrine-Afsar *et al.*, 2012; Feld *et al.*, 2015). The bottleneck of the latter methods is the slow data acquisition due to the limited speed of the sample holder movement.

Both, serial crystallography approaches at third generation synchrotrons as well as free-electron lasers have extended the range of usable crystal sizes for macromolecular crystallography to the low micro- and nanometer regime. Therefore, the conventional goal to produce a single protein crystal with a size as big as possible does not hold true anymore if serial crystallography is applied.

In general, the use of nano- and microcrystals for X-ray crystallography comprises several advantages over large protein crystals. Small protein crystals, containing only a few hundred up to a few thousand unit cells, are expected to show a reduced long-range disorder compared to larger crystals. Due to the reduced mosaicity the diffraction data is of higher quality and allows for improved structure determination (Martin-Garcia *et al.*, 2016). Further, depending on the data collection strategy the contribution of radiation damage can be significantly reduced by exposing multiple crystals to X-rays while keeping the total amount of crystalline sample low. And most importantly, multi-crystal approaches at room-temperature imply substantial advantages when following biological processes by time-resolved experiments. When using light sensitive proteins or photoactivatable compounds a small crystal size is beneficial, because it allows a homogenous activation upon light irradiation, even if the penetration depth of the electromagnetic wave is limited (Levantino *et al.*, 2015). For

experiments relying on diffusion of a substrate into the crystal for initiation of the reaction, the crystal size is directly related to the diffusion time of the substrate to reach the center of the crystal, which limits the maximal temporal resolution of the experiment (Schmidt, 2013).

OUTLINE AND AIMS OF THE THESIS

Beginning with the invention of a revolutionary new method called serial femtosecond X-ray crystallography (SFX) (Chapman *et al.*, 2011; Schlichting, 2015; Martin-Garcia *et al.*, 2016) the general interest in protein micro and nanocrystals for protein structure determination did substantially increase. In SFX protein nano- or microcrystals are exposed to highly intense X-ray pulses produced by X-ray free electron lasers (XFELs). Because all atoms inside the crystal are fully ionized by the transferred electromagnetic energy of the X-ray pulse only one single diffraction image can be recorded from each crystal (Neutze *et al.*, 2000). Consequently, several thousands of nano- or microcrystals with homogeneous size have to be exposed by X-rays to obtain a complete dataset. Therefore, a strong demand exists in adapting and developing new methods for preparation and scoring of protein nano- and microcrystals.

This thesis is subdivided into two sections, A and B. Section A contains the main part of the thesis and deals with the development and adaptation of novel methods for nano- and microcrystal preparation, their identification, as well as their application for X-ray crystallography. In particular, the method of Dynamic Light Scattering (DLS) should be applied, because the size range of particles that can be investigated with this technique covers the complete size range that is relevant in nanocrystallography, from monomeric protein up to nanocrystals and small microcrystals. The first part of the thesis focusses on optimizing protein buffer components, because an optimal solvent composition is a crucial step towards the growth of protein crystals. It is intended to use DLS to assess buffer quality in large scale screenings and the results are expected to provide insights whether the obtained information are complementary or consistent to those from Thermofluor experiments.

The next core aspect in this work aims to provide new insights into some fundamental aspects of the protein nucleation process. For this, the XtalController technology shall be used, because it allows a unique feedback controlled navigation in the phase diagram. It is intended to gain new information about the nucleation process and its application in nanocrystallography. In particular, the results might provide new experimental insights into the theory of a two-step mechanism in nucleation. Moreover, opportunities of microfluidics are to be considered because they can provide a similar flexibility to navigate through the phase diagram. However, up to now the evaluation of the crystallization experiment in microfluidic approaches is based on visual inspection of the droplets. Therefore, it is investigated whether DLS measurements can be performed in the nano-sized volumes of microfluidic devices to get faster feedback information during crystallization experiments.

The second core aspect of this study represents the development of a novel, fast and reliable biophysical method for nanocrystal detection. For this, the potential of non-invasive Depolarized Dynamic Light Scattering (DDLS) is illuminated. Crystallization experiments are monitored online to distinguish between the nucleation and growth of ordered crystals and the formation of amorphous precipitation in solution.

Further focus will be placed on elucidating applications of protein microcrystals for X-ray crystallography at synchrotron radiation sources. A simple fixed target approach and data collection protocol shall be established for micro-focus beamlines that facilitates the diffraction data collection from microcrystals at room-temperature. Potential applications of this approach towards monitoring site-specific radiation damage, conformational changes and possibly even enzymatic reactions should be elucidated. Additional emphasis is placed on the investigation of site-specific radiation damage in multi-crystal diffraction datasets as a potential source for obtaining phase information.

In terms of this investigation the protein APP, which is a key enzyme in the hemoglobin degradation pathway of the human malaria parasite *Plasmodium falciparum*, shall be structurally characterized. For this, a protocol for the expression and purification of APP has to be established and crystallization conditions are screened in case a sufficiently pure protein solution can be obtained. X-ray Crystallography might provide interesting information about the still poorly understood substrate specificity of APP and can contribute towards the development of new inhibitors that are specific for *P. falciparum* APP. Additionally, the methods developed within section A can potentially be applied to characterize APP.

SECTION A

DEVELOPMENT AND ADAPTATION OF NOVEL METHODS FOR NANO- AND MICROCRYSTAL PREPARATION

Before the development of the SFX method, nanocrystals have been mostly seen as a first step towards the growth of single large crystals. Consequently, the growth of nanocrystals has been largely unexplored so far. With SFX the interest to obtain nanocrystals and small microcrystals in large quantities and great size homogeneity has increased strongly over the last years. It results in a great demand in the development and adaptation of existing methods for the preparation and characterization of small crystals. A fundamental understanding of the phase diagram of the target protein and a better general understanding of the thermodynamics of the crystallization process is of great importance to obtain well-ordered nano- and microcrystals instead of amorphous precipitate. Instead of slowly decreasing the solubility of the protein, in nanocrystallization the solubility is typically decreased rapidly in order to induce multiple nucleation events in the same time and thus obtaining showers of microcrystals (Kupitz *et al.*, 2014; McPherson & Cudney, 2014).

Several approaches have been published where commonly used crystallization methods have been adapted towards the preparation of nanocrystals. Certainly, ordinary vapor diffusion techniques can be used for nanocrystallization, yet resulting in samples volumes which are too low for many applications. The batch method has been used for rapid mixing of high concentrated protein and precipitant solutions resulting in a different starting point in the phase diagram, compared to setups for large protein crystals (Schlichting, 2015). It has also been shown that suitable crystal slurries can be obtained by simply crushing larger protein crystals (Stevenson *et al.*, 2014b). However, the success rate of this approach strongly depends on the protein and eventually leads to a decreased diffraction power in many cases. When free interface diffusion is used for nanocrystal preparation a protein solution is added in small increments to a highly concentrated precipitant solution. After entering the precipitant, nucleation events take place at the interface of the protein droplet and the surrounding

precipitant. A further crystal growth is quenched by fast sedimentation of the nanocrystals in the precipitant solution and can be regulated varying the gravity force in a centrifuge (Kupitz *et al.*, 2014). A very innovative approach for preparation of nano- and microcrystals has also been demonstrated by crystallizing proteins *in vivo* using insect cells or yeast cells (Redecke *et al.*, 2013; Jakobi *et al.*, 2016). It could be shown that these crystals are also suitable for X-ray diffraction experiments. It is assumed that the crystallization occurs upon accumulation of the target protein in compartments and organelles, like the endoplasmic reticulum or peroxisomes (Koopmann *et al.*, 2012; Duszenko *et al.*, 2015; Doye & Poon, 2006). However, the general mechanism of the crystallization process and the broad application to a variety of different proteins has to be further elucidated.

In addition to the preparation methods, the reliable identification of sub-micrometer sized crystals is challenging, because they are too small to be identified by light microscopy. Therefore, ultraviolet fluorescence as well as two-photon ultraviolet fluorescence has been used to differentiate between macromolecules and salt particles (Dierks *et al.*, 2010), but the recorded intensity greatly depends on the number of disulfide bonds or aromatic residues within the macromolecule and the method does not identify crystallinity. Second harmonic generation (SHG) has been demonstrated as a suitable technique for crystal detection (Wampler *et al.*, 2008). Nevertheless, the method can only be applied to crystals with low symmetry and considerable size in order to produce a sufficiently intense SHG signal (Kissick *et al.*, 2011). Recently, the method has been extended to the nanocrystal size regime by combining the SHG signal with a correlation spectroscopy approach (Dow *et al.*, 2016). Transmission electron microscopy can be used to identify and visualize protein nanocrystals as well (Stevenson *et al.*, 2014b; Falkner *et al.*, 2005), although it requires a labor-intensive sample preparation involving chemical crosslinking or a cryo-preparation. Therefore, X-ray powder diffraction is still the most powerful method for sample characterization and widely used, because it provides qualitative information about the diffraction power of the protein crystals (Dreele, 2007). However, it is an invasive method which requires a rather large sample volume and a readily available X-ray source. Although each characterization method has its potential, the individual limitations lead to the fact that none of them has been established as a gold standard. Therefore, the development of novel, fast and reliable methods for nanocrystal preparation and quality assessment are of great demand.

CHAPTER 1

1. THERMOFLUOR AND DYNAMIC LIGHT SCATTERING FOR SAMPLE BUFFER OPTIMIZATION PRIOR CRYSTALLIZATION

1.1 Introduction

The structural characterization of proteins often requires a large scale production and purification of the protein of interest. Throughout all purification steps it is important to stabilize the recombinant protein, because degradation and folding instability leads to aggregation or precipitation of the protein. Therefore, the protein has to be isolated in an environment that contains stabilizing factors in order to maintain the proteins function and homogeneity. It is in particular critical for the growth of well-diffracting protein crystals to obtain information about the proteins biophysical properties like solubility, homogeneity and stability (Segelke, 2001). Hence for yielding an optimized solvent environment for the protein of interest it is important to screen a wide range of solvent parameters, such as buffer pH, ionic strength, ligands and additives (Vedadi *et al.*, 2006; Mezzasalma *et al.*, 2007). Further, it has been shown that the thermal stability of a protein is a helpful measure to identify stabilizing additives which increase the success rate in crystallization experiments (Ericsson *et al.*, 2006; Santos *et al.*, 2012). It has also been demonstrated that a low or multistep melting temperature is unfavorable for the formation of protein crystals (Dupeux *et al.*, 2011). A widely used method to assess the thermal stability of a protein is called Differential Scanning Fluorimetry (Pantoliano *et al.*, 2001), which was later commonly named Thermofluor (TF) (Matulis *et al.*, 2005). The method is based on detecting fluorescence from a fluorescent dye that is binding to exposed hydrophobic regions of a protein. While in solution the fluorescent dye (SYPRO orange) is quenched, but it regains its fluorescence when binding in a hydrophobic pocket (Steinberg *et al.*, 1996a; Steinberg *et al.*, 1996b). When the temperature of a protein solution is constantly increased, the protein starts to unfold gradually. Thereby, the detected fluorescence signal increases because the fraction of the dye that can bind to hydrophobic areas is increasing. As a result, the melting temperature of the protein can be calculated from the melting curve. The values can be compared by screening different buffer compositions and thus a comparative identification of stabilizing agents can be achieved.

A complementary method for characterizing a protein sample in solution before crystallization is Dynamic Light Scattering (DLS). It has been shown that a small size distribution of particles in solution increases the probability for successful crystallization and therefore is favored compared to a polydisperse sample (Baldwin *et al.*, 1986; Zulauf & D'Arcy, 1992; Ferré-D'Amaré & Burley, 1994; D'Arcy, 1994; Niesen *et al.*, 2008; Price *et al.*, 2009). Additionally, for the proteins acyl coenzyme A (Yoshida *et al.*, 2005), MnmG (Shi *et al.*, 2009), HypE (Rangarajan *et al.*, 2008), Cj1293 (Goon *et al.*, 2003) and YdiF (Rangarajan *et al.*, 2005) among others it has been demonstrated that DLS can be used to optimize the buffer composition of the proteins before crystallization, resulting in well diffracting protein crystals.

This chapter is hence reporting the investigation of utilizing DLS for high-throughput buffer compound screening. More precisely, it was tested whether the commercially available RUBIC screens (Boivin *et al.*, 2013), which have been specifically designed for Thermofluor screenings, can be used for DLS based scoring as well. TF is based on hydrophobic patch exposition and consequently reports about the protein stability without addressing the dispersity of the solution. In contrast, DLS measurements can identify the distribution of particle sizes in a specific buffer environment and be used for a comparative analysis of protein dispersity. It was investigated to what extend the obtained information are consistent, or if advanced information regarding an optimization of the buffer composition can be obtained by the complementary DLS approach. For this, the protein thioredoxin from *Wuchereria bancrofti* was used as a model protein, which could be readily produced in sufficient amounts.

1.2 Material and Methods

1.2.1 Sample preparation

The protocol for the recombinant production and purification of the protein thioredoxin (*Wuchereria bancrofti*) has been initially established by Dr. Nasser Yousef (University Hamburg) and was adapted by Svetlana Kapis (University Hamburg). For the production of thioredoxin the plasmid pRSET-B containing the thioredoxin gene was transformed into the *Escherichia coli* strain BL21(DE3)pLysS (Novagen, Schwalbach, Germany). The *E. coli* cells have been grown at 310 K in lysogeny Broth-Lennox medium supplemented with 34 mg · mL⁻¹ chloramphenicol and 100 mg · mL⁻¹ ampicillin for plasmid selection. After the cell suspension reached an OD₆₀₀ of 0.6 gene expression was induced with 0.5 mM Isopropyl-β-D-thiogalactopyranosid (IPTG). Four hours after initiation of expression the cells were harvested by centrifugation and the resulting cell pellet was resuspended in lysis buffer (20 mM Tris-HCl, pH 8.0, 5 mM EDTA). Bacterial cells have been disrupted by sonication and clarified from cell debris by 40 min centrifugation at 17,000 x g at 4 °C. Soluble thioredoxin was obtained in the

supernatant and purified by anion-exchange chromatography using a Q-Sepharose fast flow column (GE Healthcare Life Sciences, Freiburg, Germany). After equilibration of the column with lysis buffer (see above) the protein solution was incubated for 1 h at 4 °C on the matrix. Subsequently, the matrix was first washed with lysis buffer to remove unbound protein and then with wash buffer (20 mM Tris-HCl, pH 8.0, 5 mM EDTA, 20 mM NaCl) in order to remove unspecifically bound protein. Finally, thioredoxin was eluted using elution buffer (20 mM Tris-HCl, pH 8.0, 5 mM EDTA, 150 mM NaCl). In a second purification step a size exclusion chromatography (HiLoad 16/600 Superdex 200 prep grade, GE Healthcare, Freiburg, Germany) was performed with elution buffer (see above). The purified recombinant thioredoxin was obtained from the elution fractions containing the monomeric protein and was concentrated up to 34 mg · mL⁻¹. For concentrating the protein an Amicon centrifugal filter concentrator (Merck Millipore, Schwalbach, Germany) with a 3 kDa molecular weight cutoff was used. Before using the purified protein for Thermofluor (TF) or Dynamic Light Scattering (DLS) experiments it was filtered by using a 0.2 µm centrifugal filter (VWR, Darmstadt, Germany) and was centrifuged for 15 minutes at 16100 x g at 4 °C.

1.2.2 Thermofluor experiments

The thermal stability of thioredoxin was determined by TF experiments from all conditions of the RUBIC buffer (MD1-96) and RUBIC additive screen (MD1-97) (Molecular Dimensions, Suffolk, UK), according to the recommended protocol (Boivin *et al.*, 2013). A relatively high protein concentration of 3 mg · mL⁻¹ (180 µM) was used for the experiments, because of the small molecular weight (≈16 kDa). For the TF experiments with the RUBIC buffer screen, 2 µL of the thioredoxin solution were mixed with 2 µL SYPRO Orange (62X stock) and 21 µL of the buffer screen condition. For the RUBIC additive screen 2 µL of thioredoxin were added to 2 µL SYPRO Orange (62-X stock), 5 µL ultrapure water and 16 µL of the additive screen condition. The Thermofluor assay was performed in 96-well PCR plates in a MyiQ RT-PCR machine (Biorad, Schwabing-Freimann, Germany) with a temperature gradient sampling from 5 °C to 95 °C with a stepwise increment of 1 °C per minute after a 5-minute equilibration at 5 °C. The normalized detected fluorescence intensity was plotted versus temperature by using the software Origin (OriginPro 9.1, OriginLab, Northampton, USA). Melting temperature in each screen condition is derived from the temperature at which the normalized fluorescence intensity reached 50%.

1.2.3 DLS experiments

DLS experiments of thioredoxin were performed in microbatch plates (HR3-081, Hampton Research, Aliso Viejo, USA). To fit the RUBIC buffer screen as well as the RUBIC additive screen into the target

microbatch plate, each screen was divided into two plates with 48 conditions each. The plates were prepared by using the micro dispensing system Oryx4 (Douglas instruments, Hungerford, UK) in microbatch mode and were covered with paraffin oil to avoid sample evaporation. For the RUBIC buffer screen, 160 nl protein were mixed with 840 nl buffer stock in order to obtain the recommended final concentration of the buffer condition. The RUBIC additive screen was prepared by pipetting 640 nl additive screen condition, 200 nl ultrapure water and 160 nl protein. The resulting protein concentration for both screens was $4.25 \text{ mg} \cdot \text{mL}^{-1}$ and the total amount of used protein was similar to the Thermofluor experiments. DLS experiments were performed using the DLS plate reader SpecroLight600 (XtalConcepts, Hamburg, Germany). The autocorrelator of the instruments covers a sample time range from $0.4 \mu\text{s}$ to 30 s. For the subsequent calculations the refractive index of water (1.33) was used due to the low molar concentration of buffer components. The decay time constant, used for the calculation of the hydrodynamic radius (R_H), is derived from the autocorrelation function (ACF) by using the CONTIN algorithm (Provencher, 1982) in the instrument software package. Each DLS measurement was performed for 20 seconds and was conducted three times in order to obtain reliable results. The temperature was kept constant at $20 \text{ }^\circ\text{C}$ during the measurements. For visual inspection of the obtained data, a radius distribution of the particles in solution was created by plotting the relative signal intensity versus the hydrodynamic radius using the software Origin (OriginPro 9.1, OriginLab, Northampton, USA).

1.3 Results and Discussion

1.3.1 Optimization of sample buffer pH based on Thermofluor and DLS

Protein stability and homogeneity are factors that are highly correlated with the protein solubility and the probability of a protein to assemble to well-ordered crystals. Therefore, the composition of the protein buffer is a crucial variable for successful crystallization experiments. In order to facilitate the optimization of the buffer components the RUBIC buffer and additive screens have been developed and cover a broad range of buffer components, pH values, ionic strengths, additives and ligands.

By using the RUBIC buffer screen the effect of different buffer substances and pH on thioredoxin was tested. From all 96 screening conditions a significant fluorescence signal was detected with increasing temperature, resulting in evaluable melting curves of the TF experiment. The screen contains a set of conditions, which allow investigating the effect of the pH without altering the buffer chemistry. For this, a complex buffer system composed of succinic acid, sodium phosphate monobasic monohydrate and glycine (SPG) is used and can be adjusted to a pH range of 4.0 to 10.0. The results from the TF experiments are presented in Figure 1-1 and reveal a clear trend of higher thermal stability towards

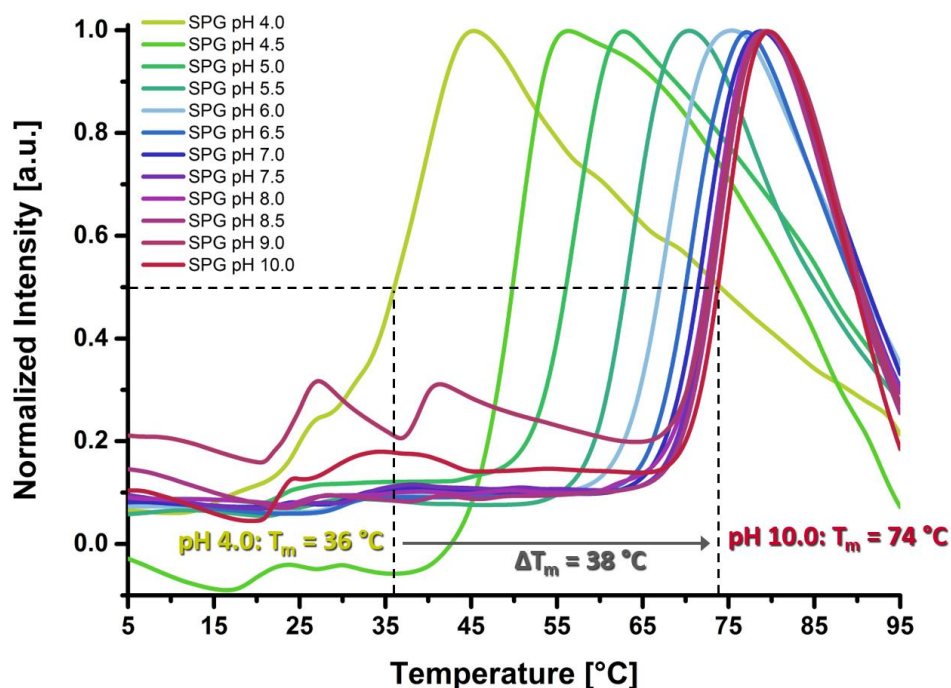


Figure 1-1: Melting curves of thioredoxin obtained from Thermofluor experiments with RUBIC buffer screen.

The normalized fluorescence intensity is plotted against the temperature. On the basis of the complex buffer system (SPG) a broad range of pH values can be tested without changing the buffer chemistry. A strong pH dependency for thioredoxin can be seen with a higher thermal stability towards higher pH values.

higher pH values. A melting temperature of 36 °C was determined at pH 4.0 and increased constantly with higher pH values, up to 74 °C at pH 10.0. This difference of 38 °C reveals a strong pH dependency of the thioredoxin protein and a preference for basic pH regarding protein stability.

However, TF experiments only yield relative information on thermal stability of proteins by comparing among different buffer environments, but will not result in information on aggregation states of proteins under these conditions. Therefore, the aggregation behavior of the protein was investigated in parallel by DLS for the same conditions. The DLS measurements have been conducted in microbatch plates under paraffin oil, to improve the optical path of the DLS laser and therewith increase the reliability of the measurements. The distribution of the hydrodynamic radius of the thioredoxin in solution could be successfully determined from all 96 conditions of the RUBIC buffer screen. Similar to the TF results in Figure 1-1, the pH dependency of thioredoxin with SPG buffer is presented in Figure 1-2. The results show that at low pH values a significant fraction of the protein is aggregated. This is in good agreement with the low melting temperature at low pH valued determined by TF. Around pH 6.0 no larger aggregates with a hydrodynamic radius above 10 nm have been detected. Interestingly, the amount of aggregated thioredoxin strongly increased again at higher pH values. This demonstrates that for protein crystallization experiments a distinct optimum around pH 6 can be identified by DLS,

based on a monodisperse radius distribution, which has been shown to be beneficial for the crystallization success rate (Zulauf & D'Arcy, 1992). It should be noted that the thioredoxin protein is known to crystallize well in a condition containing SPG buffer with a pH of 6.5 in the presence of PEG 1500 (see section 3.2.2). Contrarily, in the TF experiments a melting temperature of 67 °C was measured at pH 6.0 and the highest thermal stability was obtained at the highest pH values (74 °C at pH 10.0). Thus, a buffer with a pH of 10 would have been chosen for crystallization trials, although DLS shows that the protein is not monodisperse in this condition. Consequently, the obtained results demonstrate that DLS can provide highly valuable complementary information for the determination of the optimal buffer composition.

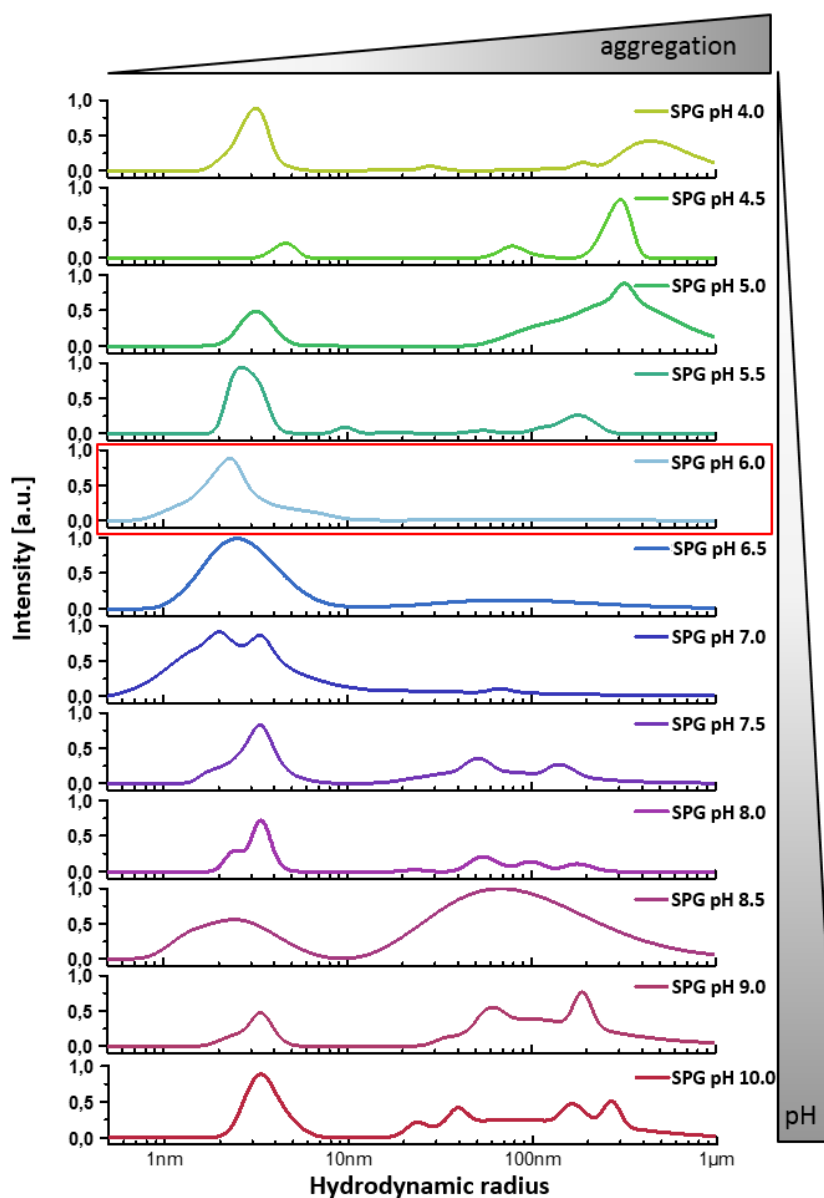


Figure 1-2: Identifying a pH-dependent aggregation of thioredoxin by DLS.

By plotting the relative intensity versus the hydrodynamic radius, the radius distribution of thioredoxin particles in solution is shown for various pH values. At low and high pH values a significant fraction of the protein is aggregated, while around pH 6 (red box) no particles with a radius larger than 10 nm are detected.

1.3.2 Identifying useful buffer additives for protein stabilization

In addition to the RUBIC buffer screen, also the RUBIC additive screen was used for sample buffer optimization and it was tested whether or not DLS can provide additional information to the Thermofluor experiments. The TF experiments provided evaluable melting curves for 92 out of the 96 screening conditions. The four non-evaluable conditions showed strong background fluorescence at low temperatures and did not show a typical melting curve progression (conditions contained 1 mM FeCl₂, 1 mM DDM, 5 mM Betaine and 5 mM Oxaloacetate). For all other conditions a melting temperature could be determined from the melting curves. Compared to the water control ($T_m = 64\text{ }^\circ\text{C}$) increasing as well as decreasing thermal stability was observed.

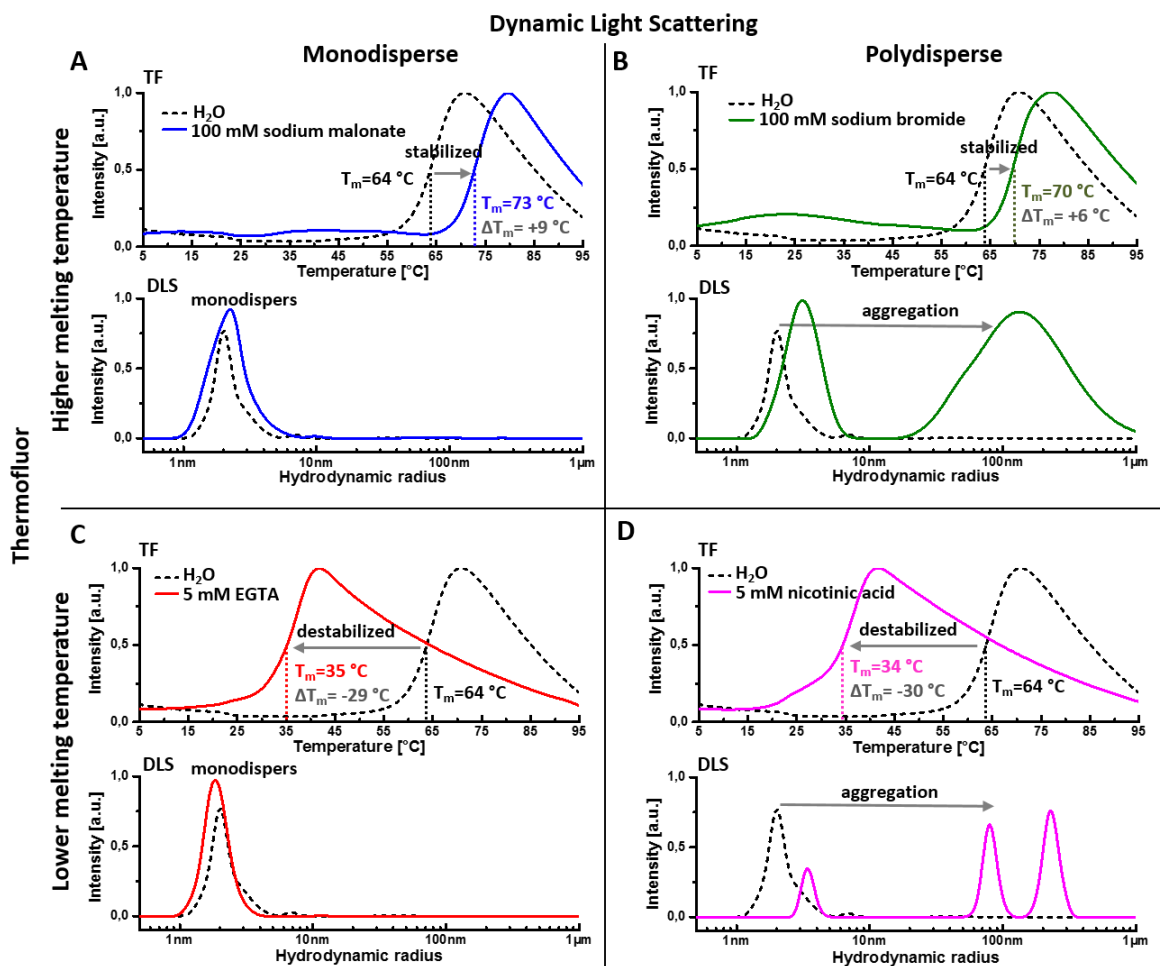


Figure 1-3: Additive compound screening by Thermofluor (TF) and Dynamic Light Scattering (DLS).

The melting curves from the Thermofluor experiments are obtained by plotting the normalized fluorescence intensity against the temperature (upper graphs). The melting temperature is derived from the point where the normalized signal intensity reaches 50% and the values are compared to the water control (dashed line). For comparison, the hydrodynamic radius distributions from the same samples, obtained by DLS measurements, are presented (lower graphs). [A] Sodium malonate leads to a stabilized ($\Delta T_m = 9\text{ }^\circ\text{C}$) and monodisperse thioredoxin protein. [B] Sodium bromide results in stabilized ($\Delta T_m = 6\text{ }^\circ\text{C}$) but aggregated protein. [C] EGTA destabilizes the protein ($\Delta T_m = -29\text{ }^\circ\text{C}$) but the thioredoxin remains monodisperse. [D] Nicotinic acid leads to destabilization ($\Delta T_m = -30\text{ }^\circ\text{C}$) and aggregation of the protein.

In parallel, DLS measurements have been performed at all conditions of the RUBIC additive screen. Exemplarily, the TF and DLS results of some meaningful screening conditions are presented in Figure 1-3. In condition A and B it can be seen that the components increased the thermal stability of thioredoxin, while other conditions (C and D) strongly destabilized the protein. Interestingly, the obtained hydrodynamic radius distributions of the conditions with increased thermal stability showed that the thioredoxin protein remained monodisperse in some cases (Figure 1-3 A), while it was strongly aggregated in others (Figure 1-3 B). Also the opposed case was observed, monodisperse (Figure 1-3 C) as well as aggregated (Figure 1-3 D) protein has been identified in conditions with strongly decreased stability. This means, that regarding thermal stability and aggregation state all combinations can occur, stabilized and monodisperse protein (A), stabilized and aggregated protein (B), destabilized but still monodisperse protein (C), as well as destabilized and aggregated protein (D). Unambiguously, the first case is the most promising condition for subsequent crystallization trials, because stabilized and monodisperse protein provides the highest chance for successful crystal formation (Niesen *et al.*, 2008). The obtained results clearly demonstrate that aggregated protein will not necessarily lead to an increased accessibility of hydrophobic patches for the fluorescent dye SYPRO-Orange and therewith to a decreased melting temperature in TF experiments. Further, it was shown that DLS can provide valuable additional information for identifying the optimal buffer composition for crystallization trials. It could be shown that both methods, DLS and TF, should be combined to find the most promising conditions during sample buffer optimization.

1.4 Conclusions

It is well known that the composition of the protein sample buffer is crucial for maintaining protein stability, homogeneity as well as purity and that these factors have a great impact on the success rate of conducted crystallization experiments. The results presented in this chapter show that DLS can be successfully applied as a high-throughput screening method using the RUBIC sample buffer and additive screens. Importantly, the total amount of used protein for the DLS measurements was identical to the TF assays, which has been conducted according manufacturer protocol. The presented data of the complementary methods DLS and TF demonstrate, that the thermal stability of a protein in solution is not related to its oligomeric state or tendency to aggregate. In the buffer screen a clear pH optimum regarding monodisperse protein was identified by DLS, whereas the melting temperature determined by TF revealed a different trend. In the additive screen all combinations were found in terms of decreased or increased thermal stability and monodisperse and aggregated protein. This clearly demonstrates that both methods should be combined in order to identify a buffer composition that fulfills all criteria known to be beneficial for crystal formation.

CHAPTER 2

2. THE NUCLEATION PROCESS OF MACROMOLECULE CRYSTALLIZATION

In protein crystallography a protein solution is typically brought into supersaturation to induce the thermodynamically driven crystal formation. Over the last decades a variety of methods were developed to gradually decrease the solubility of a protein solution by increasing the precipitant concentration. In classical crystallography the formation of a few crystal nuclei, which can then grow to individual large protein crystals by addition of free protein from the bulk, is favored (McPherson, 1999). For the preparation of protein nanocrystals these methods need to be modified in order to increase the number of nucleation events in the crystallization droplet (Kupitz *et al.*, 2014; McPherson & Cudney, 2014). Additionally, a better understanding of the nucleation process itself is of great use to adapt the existing methods to the new requirements in nanocrystallography. Albeit the fact that the field of protein crystallography already exists for several decades, the fundamental understanding of the nucleation process is still incomplete and an active area of ongoing research (Sleutel & van Driessche, 2014; Ataka & Asai, 1990; Chayen *et al.*, 2006; Feher & Kam, 1985; Galkin & Vekilov, 1999, 2001; Haas, 2000; Malkin & McPherson, 1994; Nicolis & Maes, 2012; Penkova *et al.*, 2006; Wolde, 1997; Yau & Vekilov, 2001).

In the classical nucleation theory, the crystal formation is considered to be a first-order phase transition. Consequently, it is characterized by the crystallization enthalpy ($\Delta H^{\circ}_{\text{cryst}}$) and the surface free energy (α) with both being non-zero. The thermodynamics of this theory has first been described by J. W. Gibbs (Gibbs, 1876, 1878). According to this theory a nucleation event in a supersaturated solution is non-favored because of the positive surface free energy. P. Vekilov (2010) described the surface free energy gain upon phase boundary creation in a nucleation event for a cubic crystal by $6a^2n^{2/3}\alpha$ (n being the number of molecules in the cluster with size a). In addition to this, the cluster formation leads to a free energy loss of $-n\Delta\mu$ when the chemical potential (μ) of the supersaturated solution is higher than that of a protein in a crystal nucleus ($\Delta\mu > 0$). Consequently, the formation of a crystal nucleus will lead to an increase in free energy and is unfavorable until a critical size (n^*) is reached. For nuclei overcoming this size barrier by fluctuations, further crystal growth occurs spontaneously and is accompanied by a decrease in free energy.

The dependency described in this paragraph is visualized in Figure 2-1 A and can be summarized by the following equation

$$\Delta G(n) = -n\Delta\mu + 6\alpha^2 n^{2/3} \alpha. \quad (1)$$

A simplified version of the phase diagram can be defined by three phases (Figure 2-1 B), the dilute solution, a dense liquid and a crystalline state. These states can be described by the two parameters concentration and internal order. According to the classical theory a nucleation event can be considered as a simultaneous transition of both parameters, from the dilute solution with low concentration and low internal order to a crystalline state with high concentration and high internal order. This path is visualized by the diagonal arrow shown in Figure 2-1 B. Based on this, the classical theory was extended to a theory of a two-step mechanism of nucleation, proposed by P. Vekilov (2004). In this theory it is assumed that for many proteins the nucleation process occurs in two consecutive steps. Firstly, a transition to a higher concentration by the formation of a dense liquid and secondly, the transition to a higher order inside these clusters (Figure 2-1 B) (Vekilov, 2010; Sleutel & van Driessche, 2014; Gliko *et al.*, 2005; Pan *et al.*, 2007). This two-step nucleation theory has additional plausibility, because it allows to explain the large discrepancy between the predicted nucleation rates by the classical nucleation theory and the experimentally determined nucleation rates (Vekilov, 2004, 2010). The size of the formed clusters was identified to range between onehundred and a few hundred nanometers, while their volume fraction in solution remains low ($< 10^{-3}$ %) (Gliko *et al.*, 2007).

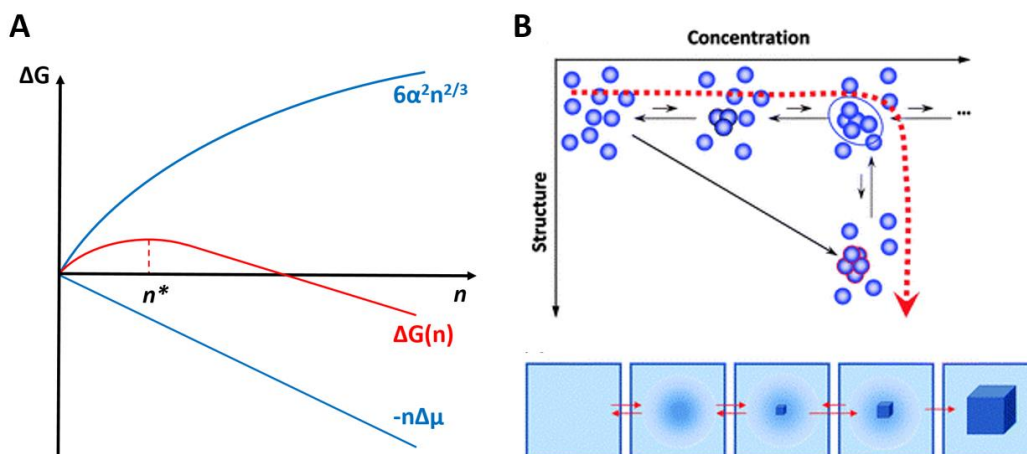


Figure 2-1: Schematic presentation of the two-step mechanism of nucleation.

(A) Thermodynamic effects during crystal nucleation (n = number of molecules in crystal; $\Delta\mu$ = solution supersaturation; α = surface free energy; ΔG = free energy; n^* critical cluster). (B) The nucleation process of particles in solution can be considered as a transition of two parameters, concentration and internal order. In classical nucleation theory both transitions occur simultaneously (diagonal path), while in the two-step mechanism protein dense clusters occur before the transition to a higher order takes place inside these clusters (Modified from Vekilov 2010).

Due to the small size of the clusters and low frequency in occurrence in the supersaturated solution, experimental evidence for the hypothesis that the second step during nucleation, a transition to a higher order, occurs inside these clusters is still rare (Sauter *et al.*, 2015; Maes *et al.*, 2015). This roots in the fact that following the nucleation process and early crystal growth by optical microscopy is not possible, because of the resolution limit of this method. Alternative methods need to be applied to study the nucleation process in detail. For several reasons dynamic light scattering (DLS) depicts to be one of the most suitable method for this. The size of the particles that can be investigated by DLS covers a large range from one nanometer up to a few micrometers. Thereby, essentially the complete size range in nanocrystallography can be investigated, from soluble proteins with a hydrodynamic radius of a few nanometers up to micrometer sized protein crystals. Additionally, DLS is an extreme sensitive method to detect a small number of larger particles in solution. This is explained by the fact that the scattering intensity of a particle in solution increases proportional to the particle radius by the power of six (Rayleigh scattering, Strutt, 1871). Consequently, the occurrence of larger particle clusters during nucleation can be detected by DLS, even if the frequency of their occurrence in the crystallization solution is very low.

2.1 Investigation of the nucleation process using the XtalController technology

2.1.1 Introduction

In protein crystallography, the protein solution has to be dragged into supersaturation to overcome the energy barrier and to induce the nucleation process as well as crystal growth. Unfortunately, the phase diagram looks different for every protein and cannot be predicted *a priori*. Therefore, many different methods have been developed to increase the precipitant concentration over time allowing charting different paths through the phase diagram. Among these are vapor diffusion techniques, batch methods and various types of free interface diffusion (McPherson, 1999). They all have in common that only limited control is obtained about the active manipulation of the solution in the phase diagram after the experiment is initiated. Since the region for inducing many nucleation events and those resulting in amorphous precipitate are not far apart in the phase diagram, a precise knowledge and control about the position in the phase diagram is highly beneficial.

In order to allow a feedback controlled navigation in the phase diagram the XtalController technology was developed by the group of Prof. Betzel in collaboration with the university of Lübeck and the company XtalConcepts (Meyer *et al.*, 2012). In the instrument a single droplet of protein solution is placed on a highly sensitive microbalance in a precisely temperature and humidity controlled experiment chamber. Two piezoelectric pumps are placed above the droplet and allow a contact-free nanoliter increment addition of water and precipitant. By recording the weight of the droplet, the evaporation rate can be determined and counteracted by a water pump. In general, the position in the phase diagram can be followed and controlled during all experimental steps, like precipitant or water addition and evaporation or dilution of the droplet. Additionally, macroscopic changes in the crystallization droplet are recorded by a CCD camera and DLS measurements can be continuously performed throughout the whole experiment, providing information about the radius distribution of the particles in solution. By this combination, a unique feedback control about the navigation in the phase diagram is obtained. Based on initial findings in previous experiments, conducted by Dr. Arne Meyer (XtalConcepts), this setup will now be used to obtain new information about the nucleation process and its application in nanocrystallography. In the experiments described in this chapter it was intended to induce the nucleation process by a single-step injection of precipitant and to follow the process online by DLS, in order to obtain new experimental insights into the theory of a two-step mechanism in nucleation. The proteins APP (*Plasmodium falciparum*), TRX (*Wuchereria bancrofti*), ML1 (*Viscum album*), ThiM (*Staphylococcus aureus*) and thaumatin (*Thaumatococcus daniellii*) were investigated to enhance the validity of drawn conclusions about general nucleation mechanisms.

2.1.2 Material and Methods

2.1.2.1 Protein sample preparation

- The protein sample mistletoe lectin 1 (ML1) from *Viscum album* was purified by Dr. Arne Meyer (XtalConcepts, Hamburg, Germany) as described previously (Meyer *et al.*, 2008). In brief, the protein was isolated from crude material of the European mistletoe by flash-freezing, grinding into powder and dissolving in ultrapure water. After centrifugation, ML1 was purified from the supernatant by aminophenyl-boronic-acid affinity chromatography. Finally, ML1 was dialyzed against 0.2 M glycine-HCl buffer at pH 2.5 and was concentrated up to $3.2 \text{ mg} \cdot \text{mL}^{-1}$ using a Amicon centrifugal filter concentrator (Merck Millipore, Schwalbach, Germany) with an MWCO = 3 kDa.
- The protein thioredoxin (TRX) from *Wuchereria bancrofti* was produced and purified as described in section 1.2.1.
- The protein 5-(hydroxyethyl)-4-methylthiazole kinase (ThiM) from *Staphylococcus aureus* was produced and purified by Dr. Madeleine Künz (University Hamburg) as described with small modifications previously (Drebes *et al.*, 2016; Drebes *et al.*, 2011). In brief, the protein ThiM was produced by gene expression in *E. coli* BLR (DE3) (Stratagene, Germany) grown in LB-medium containing $100 \text{ mg} \cdot \text{mL}^{-1}$ ampicillin. Gene expression was induced by 200 ng mL^{-1} AHT at OD_{600} of 0.5 at 37 °C for 4 hours. The cell pellet was resuspended in lysis buffer (50 mM Tris buffer pH 8.0, 150 mM NaCl, 10 mM imidazole), sonicated and centrifuged for 1 hour at 4 °C with $17\,000 \times g$. The ThiM protein was purified using affinity chromatography (Ni-NTA) and eluted using elution buffer (50 mM Tris buffer pH 8.0, 150 mM NaCl, 10 mM imidazole) after washing with lysis buffer (see above). After dialysis over night against imidazole free lysis buffer a second purification step was performed using size exclusion chromatography with lysis buffer (see above). The protein was concentrated from the elution fractions up to $24 \text{ mg} \cdot \text{mL}^{-1}$ using a Amicon centrifugal filter concentrator (Merck Millipore, Schwalbach, Germany) with an MWCO = 10 kDa.
- The protein aminopeptidase P (APP) from *Plasmodium falciparum* was produced according to the protocol described in section 5.2.1 and 5.2.2.
- The protein thaumatin from *Thaumatococcus daniellii* was purchased (Sigma, Taufkirchen, Germany). The lyophilized protein was dissolved in buffer containing 50 mM Bis-Tris pH 6.5 to a concentration of $34 \text{ mg} \cdot \text{mL}^{-1}$.

For all proteins the final protein concentration was determined using a Nanodrop ND-2000 (Thermo-Scientific, Erlangen, Germany). The protein solution was filtered through a $0.2 \mu\text{m}$ centrifugal filter

(VWR, Darmstadt, Germany) and was centrifuged for 15 minutes at 16100 x g prior usage for crystallization experiments with the XtalController.

2.1.2.2 XtalController Setup

The XtalController instrument has been developed in collaboration with the university Lübeck, Institute of Biochemistry, and was manufactured by XtalConcepts (Hamburg, Germany). The instrument consists of an experimental chamber, which is precisely temperature and humidity controlled with 0.01 °C resolution, as well as the microscope and laser optics. A schematic illustration of the experimental chamber as well a photographic presentation of the XtalController instrument is shown in Figure 2-2.

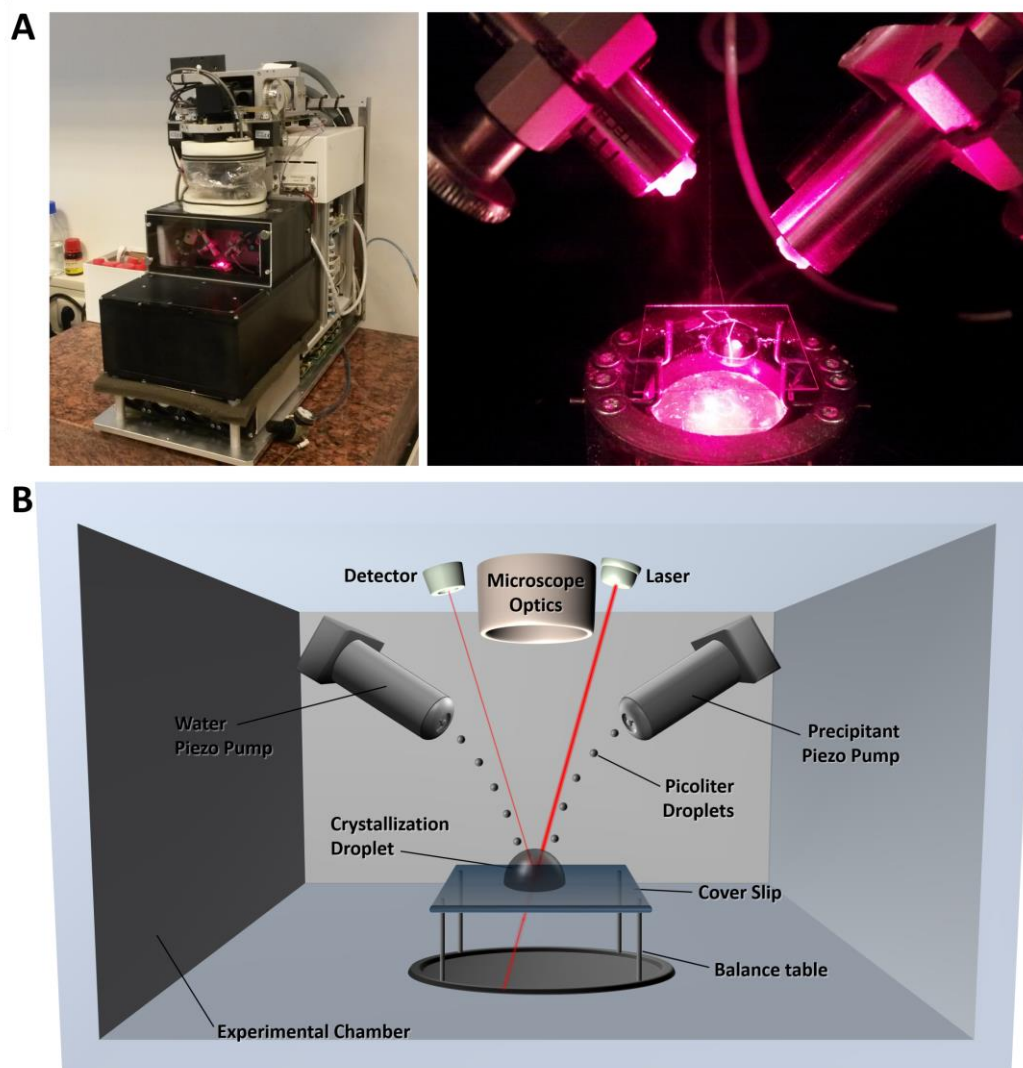


Figure 2-2: Setup of the XtalController instrument.

(A) Photographic presentation of the XtalController instrument and the experimental chamber with the piezoelectric pumps, crystallization droplet and DLS laser. (B) Schematic presentation of the temperature- and humidity-controlled experimental chamber of the XtalController instrument.

The crystallization experiment is performed as a sitting drop on a cover slip, placed on a microbalance with a resolution of 0.1 μg . The microbalance allows to calculate the actual protein and precipitant concentration in the droplet over time, based on mass changes due to evaporation or addition of precipitant. Water as well as precipitant can be added to the droplet via contact free piezoelectric pumps. The volume of a single injected droplet is around 70 pL and a repetition rate of 10000 droplets per second can be achieved. The small increment injection of precipitant allows to minimize concentration gradients and convection within the crystallization droplet. The microscope optics is equipped with different magnifications lenses resulting in a maximal spatial resolution of 2.5 μm , recorded on a CCD camera. For the DLS measurements a laser with a wavelength of 660 nm and an output power of 100 mW is used and the scattered light is detected at an angle of 150 degrees. For all calculations the refractive index of water (1.33) was used. The autocorrelator of the instrument covers a time range from 0.4 μs to 30 s. From the recorded autocorrelation function (ACF) the decay time constants of the different particles in solution is derived using the CONTIN algorithm (Provencher, 1982). The viscosity of the sample solution is taken into account for the hydrodynamic radius calculation of the particles using the Stokes-Einstein equation (equation 2 in 3.2.4).

2.1.2.3 Experimental procedure

In the experimental setup a clean and siliconized cover slip was placed on the microbalance in the experimental chamber of the XtalController. The temperature was precisely controlled and constantly kept at 20 $^{\circ}\text{C}$ for all crystallization experiments and the value of the dew point was set just below the temperature in order to reach a relative humidity near 99 %. The high relative humidity was chosen in order to minimize the evaporation of water from the crystallization droplet and therewith the convection. In a typical XtalController experiment a sample volume of 5 μL to 10 μL was placed in the middle of the cover slip. The water pump was programmed to compensate for evaporation, based on the initially recorded weight of the microbalance, in order to keep the protein concentration in the droplet stable. DLS measurements were performed regularly in a time interval of one minute during the first 100 minutes of any experiment, followed by longer time intervals of five minutes in the later phase of the experiment. A camera image of the sample droplet was recorded in between two DLS measurements to observe macroscopic changes during the crystallization experiment. Each DLS measurement was conducted for 30 seconds. The first DLS measurements are used to determine the hydrodynamic radius of the protein prior addition of precipitant. Subsequently, an automatic sequence, typically consisting of three steps, was started for the precipitant injection. In the first step the droplet was kept constant for 100 seconds. During this time the speed of water evaporation is determined and used to compensate for water evaporation during precipitant injection. In the second step the precipitant injection is performed. The duration of this step varied from 20 minutes to one

hour, depending on the precipitant stock concentration (Table 1) and the final target concentration after injection. Finally, the droplet condition was kept constant until the end of the experiment unless further precipitant injection was necessary. The exact values for the initial sample volume, protein and precipitant concentration can be read from the experimental curves of the XtalController experiments in the result section.

In a separate experiment, isotropic particle counter standards with a diameter of 400 nm (3K-400, Sigma-Aldrich, Taufkirchen, Germany) have been used to calculate the viscosity of the different precipitant stock solutions. For this, a correction factor was determined from the difference of the measured hydrodynamic radius of the particles in water and the precipitant stock. In combination with the calculated precipitant concentration in the crystallization droplet for all time points of an XtalController experiment, the correct viscosity was taken into account for the calculation of the hydrodynamic radius of the particles in solution.

Table 1: List of precipitant stocks used for XtalController experiments.

Protein	Precipitant composition	Precipitant viscosity
ML1	3.0 M ammonium sulfate	1.40 cP
TRX	0.05 M SPG buffer pH 6.5, 20 % (w/v) PEG 1500	3.73 cP
ThiM	0.1 M HEPES pH 7.5, 0.9 M lithium sulfate	1.61 cP
Thaumatin	1.4 M sodium tartrate	3.27 cP
APP	0.05 M HEPES pH 7.5, 20 % (w/v) PEG 1500	3.73 cP

2.1.2.4 Electron microscopy for sample characterization

The characterization of the sample content from the XtalController experiments was performed by electron microscopy imaging at the Heinrich-Pette-Institute for experimental virology (Hamburg, Germany) in collaboration with Dr. Rudolph Reimer. All protein samples were transferred from the cover slip in the experimental chamber of the XtalController to a 1.5 ml Eppendorf tube and prepared as mentioned in the following paragraph. The tube was centrifuged at 2600 x g for 5 minutes at 20 °C in order to pelletize all larger particles in solution. The supernatant was exchanged by a solution containing the exact precipitant concentration at the end of the experiment, which has been derived from the curves of the XtalController, supplemented with 2.5 % (v/v) glutaraldehyde, gently mixed and incubated for 48 hours to stabilize the particles in solution. After chemical cross-linking samples have been centrifuged for 5 minutes at 2600 x g at 20 °C and the supernatant was replaced by ultrapure water in order to get rid of all salts in solution. The sample was centrifuged again for 5 minutes at

2600 x g at 20 °C and the volume of the sample was reduced to 5 μL to concentrate the particles for electron microscopy imaging.

For the scanning electron microscopy, the specimens were prepared by drying 5 μL of the stabilized aqueous solutions on round glass cover slips (10 mm diameter). The cover slips were fixed on SEM specimen mount stubs (Electron Microscopy Sciences, Hatfield, USA) and a film of gold with a thickness of approximately 10 nm was sputtered onto the sample by using a Q150T sputter coater (Quorum Technologies, East Sussex, UK) in order to avoid charging during electron microscopy. Images of the samples were recorded using a Philips XL-30 environmental scanning electron microscope operated at 10 to 15 kV in high vacuum mode and a specimen distance of 8 mm.

For the transmission electron microscopy, a negative stain of the sample was performed to increase the contrast for imaging. A volume of 2 μL of the sample was pipetted onto the carbon film of a mesh copper grid (400 x 400 μm squares) (Electron Microscopy Sciences). Before loading the sample, the grid was freshly glow-discharged for 1 minute at 25 mV (EmiTech KX100). Subsequently, 2 μL of sample were applied on the grid and have been incubated for 60 seconds before blotting the liquid with Whatman paper. For the negative staining with 2 % (w/v) uranyl acetate the inverted grid was applied onto a droplet of staining solution and incubated for 30 seconds, followed by two washing steps with ultrapure water. An FEI Tecnai G20 transmission electron microscope operated at 120 kV was used for imaging, equipped with a single-tilt specimen holder. Images were recorded with a FEI Eagle 4k CCD camera.

2.1.3 Results and Discussion

2.1.3.1 Following the nucleation process using the XtalController technology

The XtalController allows the nanoliter increment addition of precipitant to the protein droplet while constantly evaluating the particle radius distribution by means of DLS. Experiments using the XtalController have been performed with different proteins in order to obtain new insights into the process of nucleation during the crystallization process.

The first experiment has been conducted using the protein APP from *Plasmodium falciparum* (see Chapter 5). For the experiments 5 μL of the APP protein solution with a concentration of 11.6 $\text{mg} \cdot \text{mL}^{-1}$ was placed on the cover slip sitting on a microbalance. The initial hydrodynamic radius of the protein was about 6 nm, corresponding to a molecular weight of around 190 kDa, which is in agreement to the APP dimer with a molecular weight of 152 kDa. The radius distribution as well as the recorded weight and the calculated concentration of protein and precipitant over time can be seen in

Figure 2-3 A. After a few initial DLS measurements the injection of precipitant (Table 1) was started and continued until a change in the radius distribution was observed. A second radius fraction around 150 nm became visible after approximately 45 minutes, when the precipitant concentration reached 5 % PEG1500 and the protein concentration decreased to $8.5 \text{ mg} \cdot \text{mL}^{-1}$. From this time point onwards the condition of the droplet was kept constant by counteracting evaporation with water injection. Over 4 hours no significant change in the radius distribution pattern was visible. The second radius fraction indicates low supersaturation and might result in single large crystals after a long incubation time, or if the drop volume is slowly further decreased. In order to produce protein nanocrystals a higher supersaturation is needed, leading to many nucleation events. Therefore, in a second experiment the precipitant injection was continued until a concentration of 12 % PEG1500 was reached (Figure 2-3 B). The resulting protein concentration after precipitant injection decreased to $4.5 \text{ mg} \cdot \text{mL}^{-1}$. During the precipitant injection a second radius fraction became visible and its size continued to grow while more precipitant was added. After the injection was finished the radius of the particles in this fraction was determined to be approximately 700 nm. The size of the particles grew further over time and three hours after initiation of the experiment particles with a radius of approximately $5 \mu\text{m}$ were detected. Simultaneously, the intensity of the lower radius fraction, corresponding to an APP dimer, diminished until no more particles with this size could be detected after 3.5 hours. At this stage, also precipitation was observed in the camera image, indicating that the supersaturation of the protein in the droplet was too high. Consequently, a precipitant concentration between the values of the first two experiments was chosen for the third experiment. Precipitant was injected to a final concentration of 9 % PEG1500, resulting in a protein concentration of $6 \text{ mg} \cdot \text{mL}^{-1}$ (Figure 2-3 C). As expected, also in this experiment a second radius fraction with a size around 100 nm became visible, indicating supersaturation of the protein solution. In contrast to the previous experiments, this radius fraction became more complex over time. Initially the size of the particles in this fraction increased to approximately $2 \mu\text{m}$ after 3 hours. Additionally, a third fraction with a size around 150 nm formed between the large particles and the dimer-fraction. In contrast to the experiment in Figure 2-3 B, also the radius fraction corresponding to the APP dimer, with a size below 10 nm, remained constant throughout the whole experiment duration. In order to visualize the transition from the dimeric APP in the beginning of the experiment to the complex radius distribution after injection of precipitant, the recorded autocorrelation function (ACF) is plotted over time for the first 2.5 hours of the experiment (Figure 2-3 C). It can be seen, that the ACF changed from a monomodal decay with a decay time constant of $27 \mu\text{s}$ to a multimodal decay, from which three decay time constants have been fitted by the CONTIN algorithm (12.7 ms, 1.4 ms and $81 \mu\text{s}$). Although the change in viscosity during precipitant injection has been taken into account for the hydrodynamic radius calculation, a slight increase in the radius of the APP dimer fraction is observed.

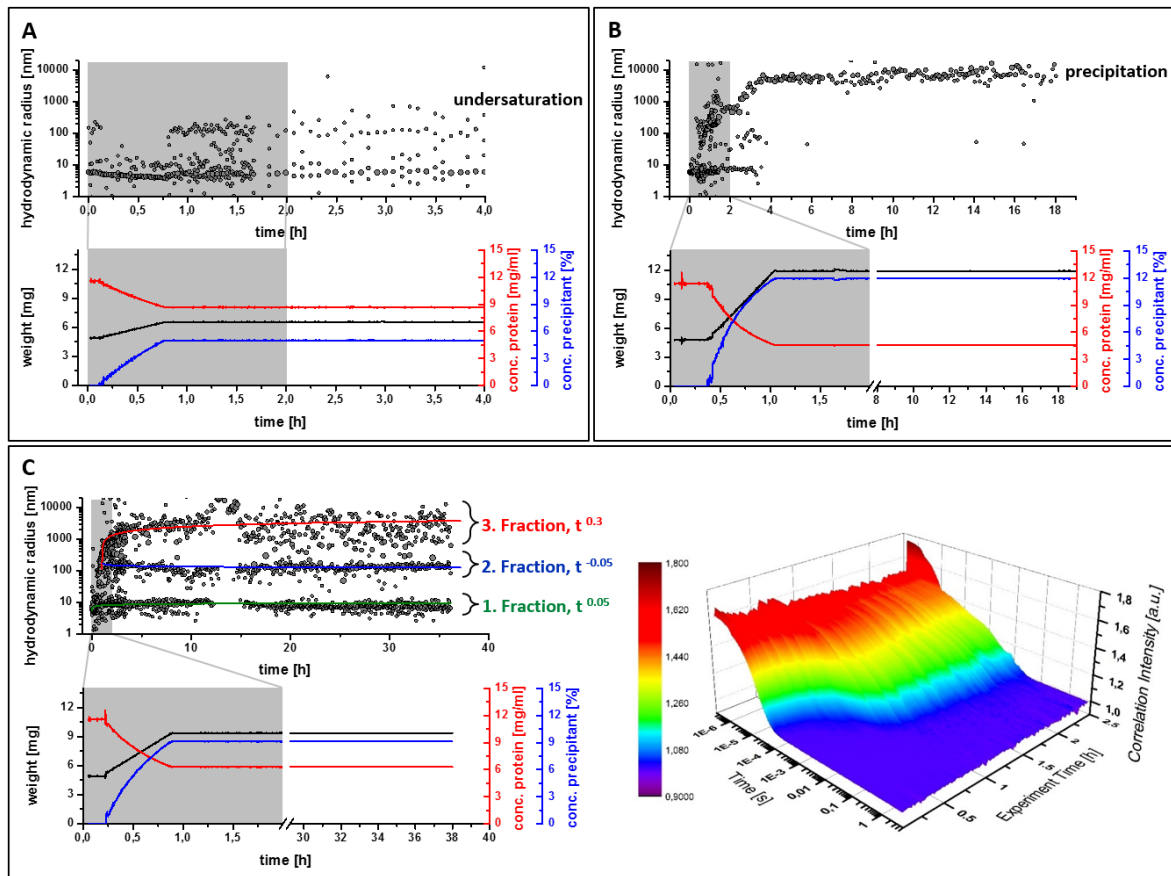


Figure 2-3: Controlled induction of APP nucleation by the XtalController.

In [A], [B] and [C] the upper graph shows the evolution of the hydrodynamic particle radii in the crystallization droplet over time. The lower graph shows the change in the recorded weight (black curve) of the sample over time and the hence calculated changes in protein (red curve) and precipitant concentration (blue curve). Please note the break in the x-axis in the lower graph for a better visualization of the precipitant injection. [A] Hydrodynamic radius evolution after 5 % precipitant addition, keeping the protein in undersaturation. [B] Precipitant addition up to 12 %, leading to protein precipitation. [C] Precipitant injection (9 %) induces nucleation and results in the formation of a complex radius distribution pattern with three distinct radius fractions. The size of the particles in the largest fraction grows proportional to $t^{0.3}$, while the other two fractions remain rather constant. The autocorrelation function (ACF) for the first 2.5 hours of the experiment is plotted in a surface presentation (right graph). A transition from a monomodal decay in the beginning of the experiment to a multimodal decay after addition of precipitant can be seen.

This indicates that electrostatic interactions, induced by the altered chemical environment upon precipitant injection, might have a small influence on the calculated absolute hydrodynamic radius.

The size of the observed particle clusters in the XtalController experiments shown in Figure 2-3 is in good agreement with the reported cluster sizes during nucleation in other studies (Galkin *et al.*, 2007; Gliko *et al.*, 2007). In general, it should be noted that the size of the clusters from different proteins and crystallization conditions varies from one hundred to several hundred nanometers, but their total volume fraction in solution remains far below 10^{-3} percent. The small number of clusters can still be identified by DLS, because the scattering intensity increases to the power of six with increasing radius of the scattering particles. The growth kinetics of the protein clusters, forming the different radius fractions, is analyzed to obtain more information about their composition. It has been shown by Lifshitz

& Slezov (1959) that the particle size of clusters increases asymptotically with the cube root of time when diffusion-limited growth in supersaturated solutions is present ($t^{0.33}$). This theory was extended by Wagner (1961), who described that the size evolves with $t^{0.5}$ in case of interface-limited growth. This LSW-theory presents the first quantitative description of a phenomenon called Oswald Ripening. In the experiment shown in Figure 2-3 C the size of the largest radius fraction (3. fraction) increases proportional to $t^{0.3}$. This demonstrates that the rate of mass increase during cluster evolution is constant and reveals that the cluster aggregation is mainly diffusion-limited. Therefore, it can be assumed that the larger clusters grow on behalf of released protein from smaller clusters by Oswald ripening and the process is driven by a minimization of surface free energy. However, in the presented experiment no significant reduction of the presence of the smaller radius fraction (2. fraction) is visible during the observed period. Interestingly, the size of the second radius fraction remains rather constant throughout the experiment and only occasionally particle sizes between fraction 2 and fraction 3 are observed. Presumably, the particles of the second radius fraction represent the smallest stable nuclei size (critical nuclei, n^*) according to the scheme in Figure 2-1 A.

Another Xtalcontroller experiment was conducted with thioredoxin and no supersaturation was obtained after injection of precipitant resulting in a final concentration of 3 % PEG1500 and a protein concentration of $14 \text{ mg} \cdot \text{mL}^{-1}$ (Figure 2-4 A). In contrast, the protein precipitated after a two-step injection of precipitant resulting in a concentration of 15 % PEG1500 and a corresponding protein concentration of $7 \text{ mg} \cdot \text{mL}^{-1}$ (Figure 2-4 B). In a third experiment a complex radius distribution pattern was obtained when injecting precipitant to a concentration of 10 % PEG1500 within 30 minutes, while the protein concentration only decreased to $16 \text{ mg} \cdot \text{mL}^{-1}$ (Figure 2-4 C). During the precipitant injection a second radius fraction occurred with a size of approximately 70 nm, which quickly grew to a few hundred nanometers. After approximately two hours the radius fraction separated into two fractions, with a smaller fraction remaining rather constant at a hydrodynamic radius of approximately 100 nm (2. fraction) and a larger fraction growing to approximately $1 \mu\text{m}$ (3. fraction). The growth kinetic of the larger fraction over time can again be well fitted by $t^{0.33}$. The emergence of the complex radius distribution pattern upon precipitant addition can also be observed in the transition from the monomodal ACF to a multimodal ACF, as shown in Figure 2-4 C.

Ammonium sulfate was used as precipitant for the XtalController experiments with ML1 and the formation of a second radius fraction could be observed after addition of precipitant to a concentration of 0.4 M (Figure 2-5 A). Rapidly, larger particles with a size above $1 \mu\text{m}$ were identified by DLS. To avoid precipitation of the sample water was added to the droplet to dilute the precipitant to a concentration of 0.3 M. The final protein concentration at this stage was $2 \text{ mg} \cdot \text{mL}^{-1}$. The size of the second radius fraction remained stable for a long time and only grew towards the end of the experiment.

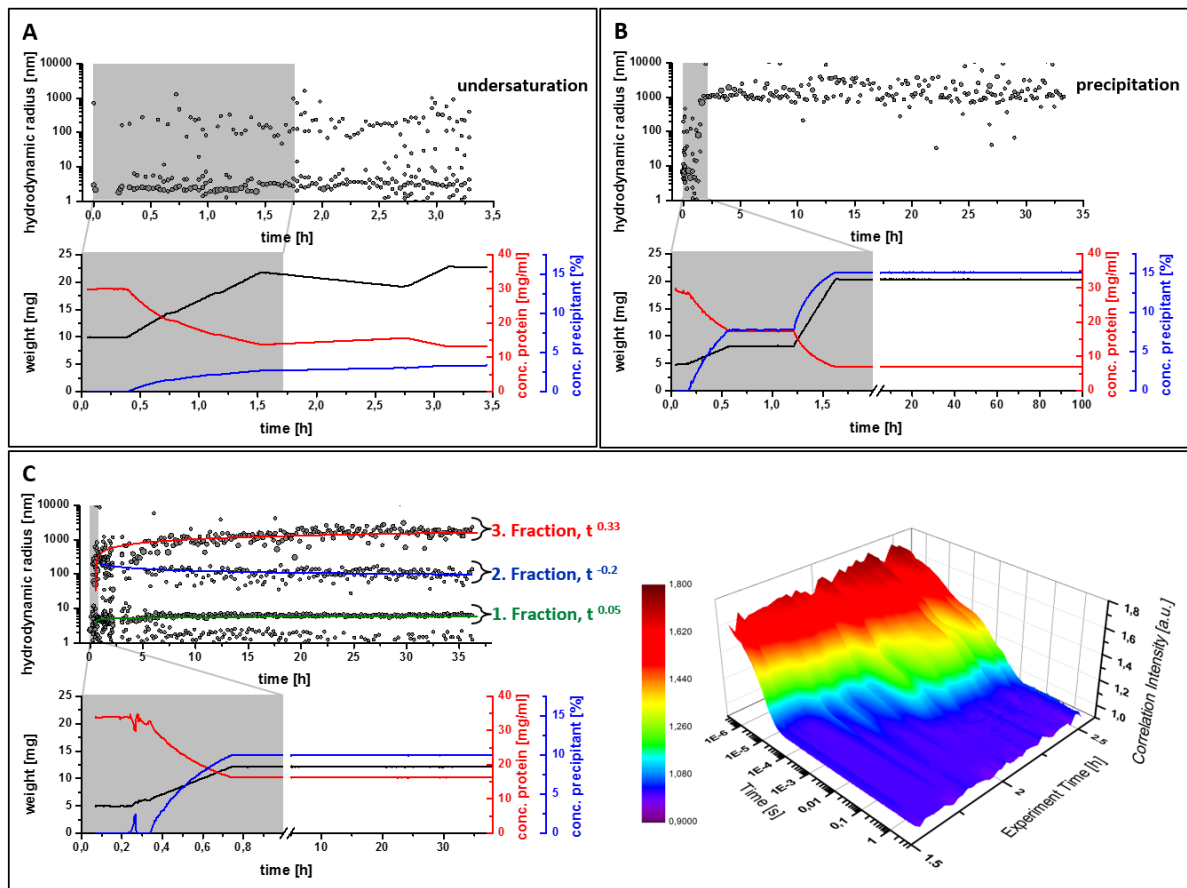


Figure 2-4: Controlled induction of thioredoxin nucleation by the XtalController.

In [A], [B] and [C] the upper graph shows the evolution of the hydrodynamic particle radii in the crystallization droplet over time. The lower graph shows the change in the recorded weight (black curve) of the sample over time and the hence calculated changes in protein (red curve) and precipitant concentration (blue curve). Please note the break in the x-axis in the lower graph for a better visualization of the precipitant injection. [A] Hydrodynamic radius evolution after precipitant addition to 3 %, keeping the protein in undersaturation. [B] Large amount of precipitant addition (15 %), leading to protein precipitation. [C] Precipitant injection up to 10 % induces nucleation and results in the formation of a complex radius distribution pattern with three distinct radius fractions. The size of the particles in the largest fraction grows proportional to $t^{0.33}$, while the other two fractions remain rather constant. The autocorrelation function (ACF) for the first 2.5 hours of the experiment is plotted in a surface presentation (right graph). A transition from a monomodal decay in the beginning of the experiment to a multimodal decay after addition of precipitant can be seen.

In a second experiment a higher initial protein concentration of $8 \text{ mg} \cdot \text{mL}^{-1}$ was used and the precipitant was directly injected to a final concentration of 0.6 M ammonium sulfate. After 30 minutes the monomeric ML1 was not detected by DLS anymore and the second radius fraction grew rapidly, resulting in precipitation of the ML1 protein (Figure 2-5 B). In the third experiment ammonium sulfate was injected to a final concentration of 0.75 M, but the initial protein concentration was as low as in the first experiment ($3.2 \text{ mg} \cdot \text{mL}^{-1}$). Just like in the experiments with APP and thioredoxin a second radius fraction with a size of approximately 100 nm formed, grew over time and split into two separate fractions (Figure 2-5 C). The larger fraction grew up to approximately $1 \mu\text{m}$, while the intermediate radius fraction remained constant at approximately 300 nm. Interestingly, the growth kinetic of the larger radius fraction was proportional to $t^{0.5}$, indicating interface-limited growth of the clusters.

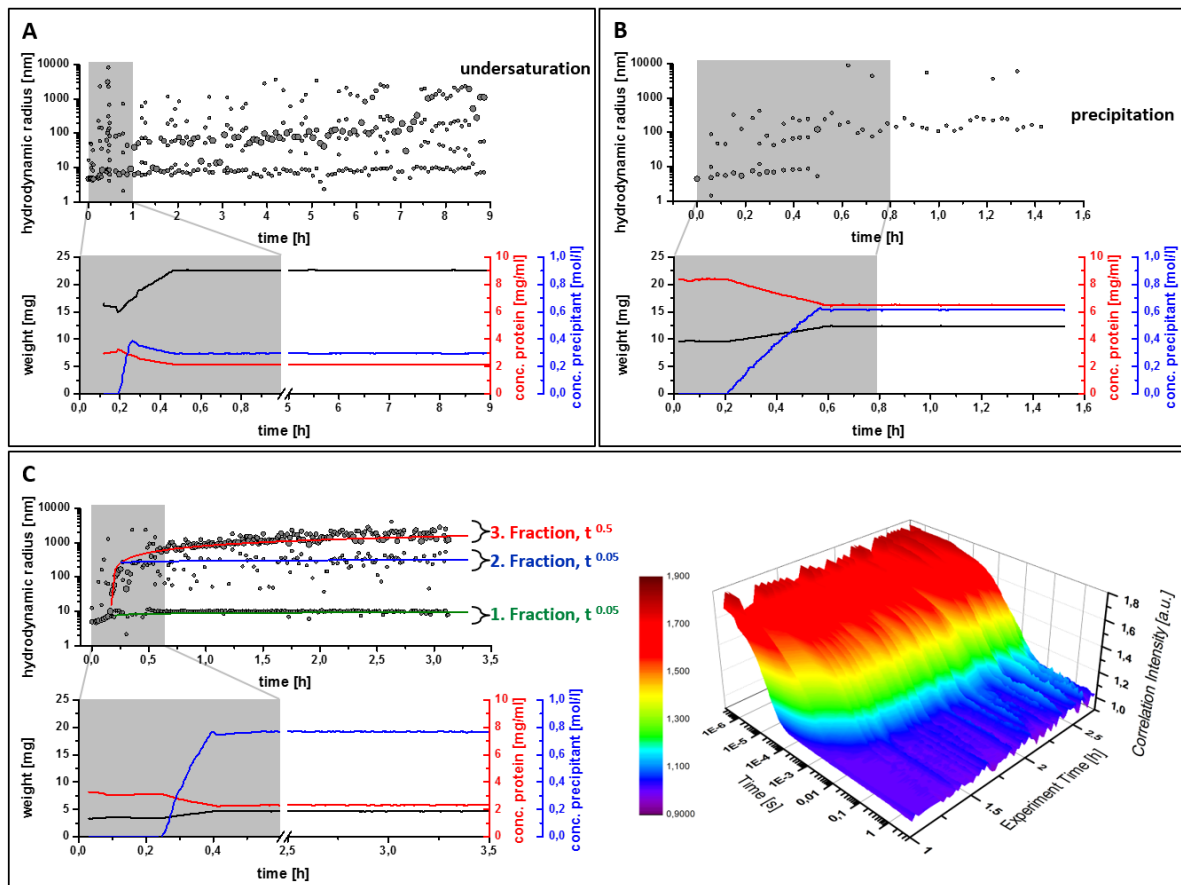


Figure 2-5: Controlled induction of ML1 nucleation by the XtalController.

In [A], [B] and [C] the upper graph shows the evolution of the hydrodynamic particle radii in the crystallization droplet over time. The lower graph shows the change in the recorded weight (black curve) of the sample over time and the hence calculated changes in protein (red curve) and precipitant concentration (blue curve). Please note the break in the x-axis in the lower graph for a better visualization of the precipitant injection. [A] Hydrodynamic radius evolution after 0.3 M precipitant addition, keeping the protein in undersaturation. [B] Large amount of precipitant addition (0.6 M), leading to protein precipitation. [C] Precipitant injection up to 0.8 M in combination with a lower protein concentration induces nucleation and results in the formation of a complex radius distribution pattern with three distinct radius fractions. The size of the particles in the largest fraction grows proportional to $t^{0.5}$, while the other two fractions remain rather constant. The autocorrelation function (ACF) for the first 2.5 hours of the experiment is plotted in a surface presentation (right graph). A transition from a monomodal decay in the beginning of the experiment to a multimodal decay after addition of precipitant can be seen.

For thaumatin and ThiM similar results were obtained and consequently only the experiments resulting in the complex radius distribution pattern are shown (Figure 2-6 A and B). Sodium tartrate was used as precipitant for thaumatin and the formation of the complex radius distribution could be observed after increasing the precipitant concentration to 0.5 M, resulting in a protein concentration of $26 \text{ mg} \cdot \text{ml}^{-1}$. A second radius fraction with a size around 100 nm formed, grew over time and split into two separate fractions. The larger fraction grew up to around $1 \mu\text{m}$ over time proportional to $t^{0.33}$, while the intermediate radius fraction remained constant around 150 - 200 nm. In the experiments with the protein ThiM, lithium sulfate was used as the precipitant and added to final concentration of 0.5 M, resulting in a protein concentration of $7 \text{ mg} \cdot \text{ml}^{-1}$. The growth kinetic of the largest radius

fraction was different than in the previous experiments and was proportional to $t^{0.15}$ (Figure 2-6 B). The content of the individual radius fractions from different proteins is further evaluated by electron microscopy and presented in section 2.1.3.2.

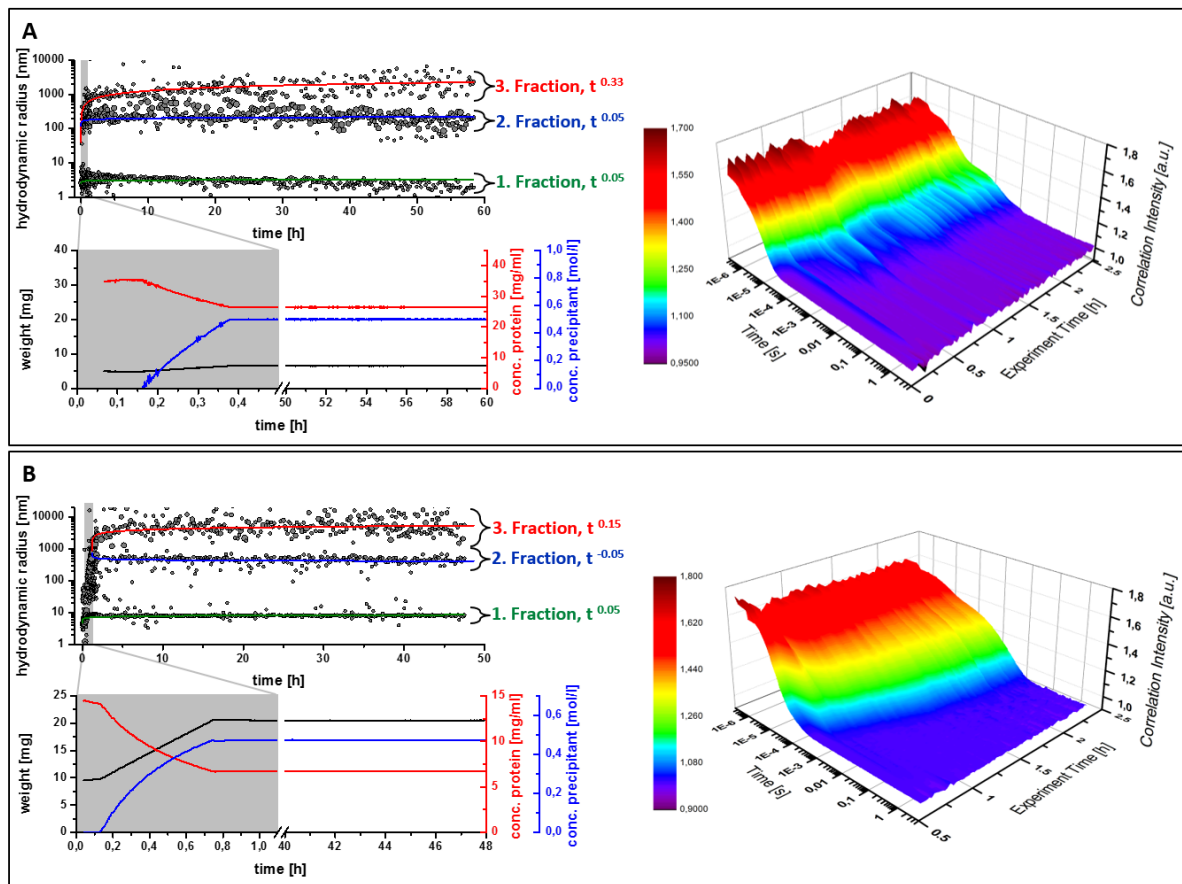


Figure 2-6: Controlled induction of nucleation by the XtalController with the proteins thaumatin and ThiM. In [A], [B] the upper graph shows the evolution of the hydrodynamic particle radii in the crystallization droplet over time. The lower graph shows the change in the recorded weight (black curve) of the sample over time and the hence calculated changes in protein (red curve) and precipitant concentration (blue curve). Please note the break in the x-axis in the lower graph for a better visualization of the precipitant injection. Precipitant injection induces nucleation and results in the formation of a complex radius distribution pattern with three distinct radius fractions. [A] The size of the thaumatin particles in the largest fraction grow proportional to $t^{0.33}$, while the other two fractions remain rather constant. [B] From ThiM the size of the particles in the largest fraction grows proportional to $t^{0.15}$, while the other two fractions remain rather constant. The autocorrelation function (ACF) for the first 2.5 hours of both experiments is plotted in a surface presentation (right graph). A transition from a monomodal decay in the beginning of the experiment to a multimodal decay after addition of precipitant can be seen.

2.1.3.2 Sample characterization using electron microscopy

It has been proposed by Vekilov (2004) that the nucleation process of crystallization for many proteins is a two-step mechanism, where the transition to a higher order occurs subsequently to a transition to a higher concentration. He proposed that liquid-liquid dense cluster form as stable intermediates in supersaturated protein solutions and that the nucleation of crystals occurs within these clusters

(Vekilov, 2010). This theory is supported by a study where the nucleation within protein clusters could be followed by depolarized oblique illumination dark-field microscopy (Maes *et al.*, 2015).

A detailed analysis of the particles detected by DLS in the XtalController experiments by visualizing methods is challenging. Evaluation by light microscopy methods is not possible because of the small particle size and the low contrast, but electron microscopy provides a promising tool for characterization of the different radius fraction contents. For this, the labile samples need to be chemically cross-linked to stabilize the particles in the high vacuum of the electron microscope. Firstly, the precipitated sample from ML1 (Figure 2-5 B) was evaluated by transmission electron microscopy to test if nanocrystals are present in the precipitate as well. The recorded images of the ML1 sample, negative stained with uranyl acetate, are shown in Figure 2-7. It can be seen that only amorphous aggregates are found in the sample and no crystalline particles are visible. By this, the assumption is confirmed that the disappearance of particles from the smallest radius fraction, corresponding to the hydrodynamic radius of the protein prior precipitant addition, is a clear indication of a beginning precipitation of the protein.

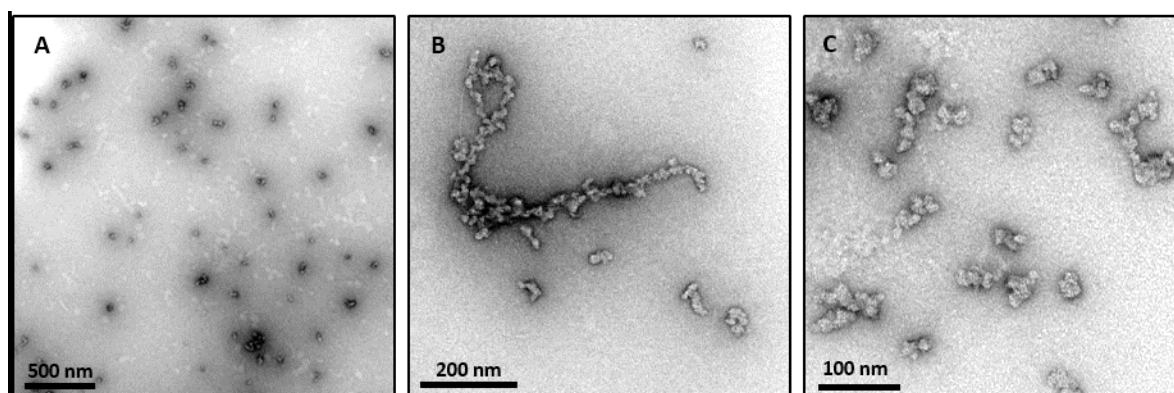


Figure 2-7: Transmission electron microscopy images of a ML1 sample obtained from the XtalController experiment shown in Figure 2-5 B.

The sample is negative stained with uranyl acetate and shows amorphous aggregates of the protein ML1.

From the XtalController experiments with ML1 also the sample with the complex radius distribution pattern (Figure 2-5 C) could be successfully stabilized by chemical crosslinking. In the transmission electron microscopy images shown in Figure 2-8 A, the protein clusters from the larger radius fractions are visible. Corresponding to the radius pattern determined by DLS, particles with the size of 200 nm to around 1 μm are visible. Most of the particles have an irregular spherical shape, comparable to macroscopic phase separation commonly seen in crystallization experiments. However, in the same sample also particles with a defined triangular shape are visible (Figure 2-8 B). A similar morphology was observed in an transmission electron microscopy image of a ML1 crystal produced by a crystallization experiment at the XtalController published by Meyer *et al.* (2012). Therefore, it can be concluded that the shaping structure in these particles are nuclei of ML1 crystals, which have formed

inside a protein dense liquid cluster. The images might demonstrate the first microscopic observation of the transition from a cluster with high protein concentration to a crystal with higher order, as postulated by the two-step nucleation theory by Vekilov in 2004 already. Additionally, the particles possessing a geometrical order are always smaller in size compared to the spherical particles. It can be hypothesized that the size of a clusters gets slightly reduced when a nucleation event occurs inside, because the crystal nuclei consumes the surrounding protein of the cluster over time, leading to a higher packing density of protein in an ordered lattice, compared to an amorphous cluster.

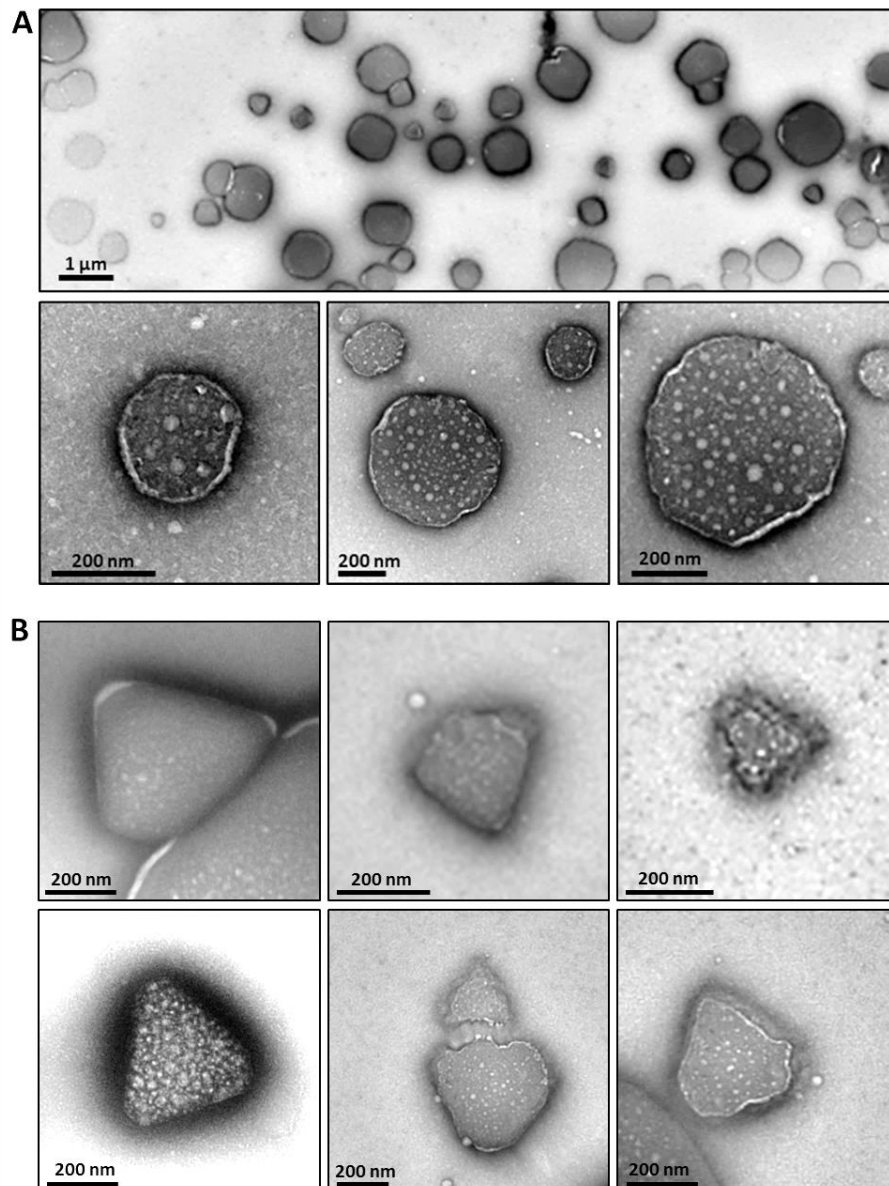


Figure 2-8: Transmission electron microscopy images of a ML1 sample obtained from the XtalController experiment shown in Figure 2-5 C.

[A] The sample is negative stained with uranyl acetate and shows protein dense liquid clusters with a size of 200 nm to 1 μm, as identified in the radius distribution pattern from the DLS measurements. The particles mostly possess an irregular spherical shape. [B] Additionally, geometrically ordered particles with triangular shape and surrounded by amorphous protein are visible. This provides additional indication that the nucleation occurs in protein dense-liquid clusters during the two-step mechanism of nucleation.

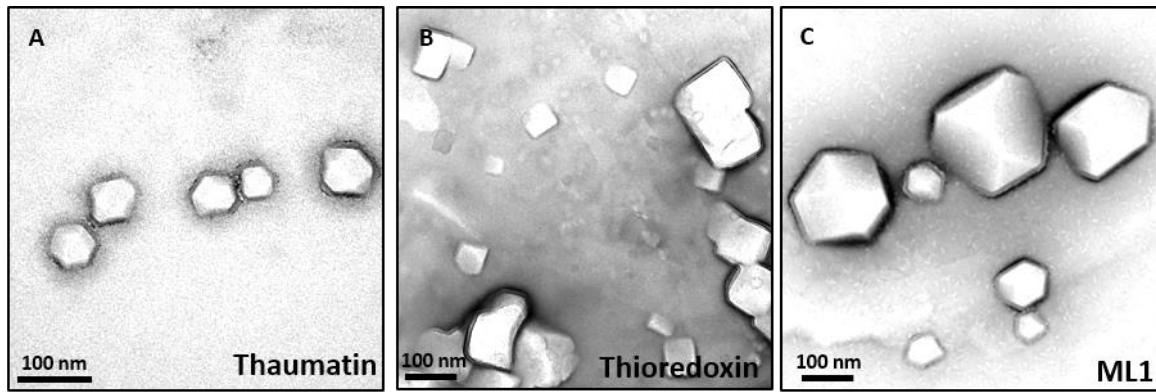


Figure 2-9: Transmission electron microscopy images of (A) thaumatin, (B) thioredoxin and (C) ML1 samples obtained from XtalController experiment.

The sample is negative stained with uranyl acetate and the images show crystalline particles with different shapes.

Because of the different chemical environments in the various crystallization conditions of the XtalController experiments the efficiency of stabilization has not been the same for all investigated proteins. Therefore, the larger clusters of the other investigated proteins could not be successfully stabilized for visualization using transmission electron microscopy (TEM). However, carbon grids with negative stained samples, produced in XtalController experiments with thaumatin, thioredoxin and ML1, showed clearly crystalline particles (Figure 2-9). The size of the crystals was very small and varied between 50 nm and 200 nm. Unfortunately, no crystal lattice similar to those demonstrated by other groups investigating protein nanocrystals by electron microscopy can be seen (Stevenson *et al.*, 2014b). Therefore, a determination of the unit cell size is not possible and consequently the crystals cannot be identified as protein crystals with absolute certainty.

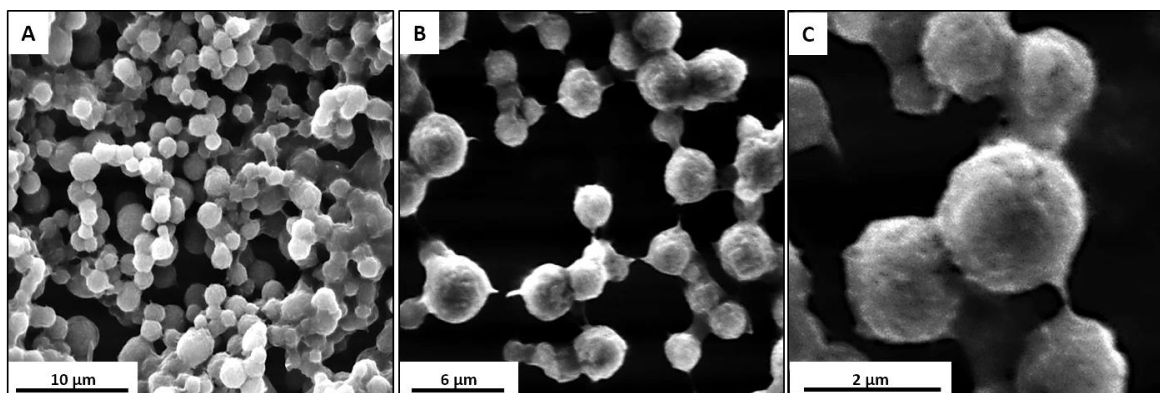


Figure 2-10: Scanning electron microscopy images of a thioredoxin sample obtained from the XtalController experiment shown in Figure 2-4 C.

The sample is sputtered with gold to enhance the contrast. The images show spherical particles with a size ranging from around 500 nm to 3 μm.

Samples produced in the XtalController experiment with thioredoxin, shown in Figure 2-4 C, were additionally analyzed by scanning electron microscopy, which benefits from a lower vacuum compared to TEM. The recorded images shown in Figure 2-10 reveal spherical particles with a size range between 500 nm and 3 μm . In this sample no geometrically ordered particles were found, indicating that the second step of the nucleation process, the transition to a higher order, might have not yet occurred in the sample.

2.1.4 Conclusion

The XtalController technology allows a feedback controlled navigation in the phase diagram and was applied to gain new information about the nucleation behavior of proteins during crystallization. It was demonstrated that DLS can be used to obtain valuable information about the early processes going along with nucleation events, which were initiated by injection of precipitant. After initial formation of particle clusters with a hydrodynamic radius of approximately 100 nm a complex radius distribution pattern evolved over time. The growth kinetics of the protein clusters, forming the different radius fractions, were analyzed. The data reveals that the rate of mass increase during cluster evolution is constant and provides evidence that the cluster aggregation is mainly diffusion-limited. Therefore, it can be hypothesized that the larger clusters grow on behalf of released protein from smaller clusters by Oswald ripening and the process is driven by a minimization of surface free energy. Further, it can be assumed that the particles of the second radius fraction represent the smallest stable nuclei size, called critical nuclei.

Characterization of the samples by scanning electron microscopy and transmission electron microscopy indicates that the observed radius distribution pattern is a result of the two-step mechanism of nucleation, proposed by Vekilov (2010). He assumed that liquid-liquid dense clusters form as stable intermediates in supersaturated protein solutions, which has been observed in the electron microscopy images of this study as well. Further, his postulation of crystal nucleation occurring within these clusters can be supported by the presence of geometrically ordered nuclei in the XtalController samples. Therefore, the presented results might demonstrate the first microscopic observation of the transition from a cluster with high protein concentration to a crystal with higher structural order.

2.2 Monitoring protein crystallization in microfluidic devices by dynamic light scattering

2.2.1 Introduction

Over the last 15 years, a lot of research was performed to transform a *wet laboratory* into a micro-sized device that is called lab-on-a-chip (Mitchell, 2001; Thorsen *et al.*, 2002). In most cases classical laboratory experiments are mimicked with the advantage of a greater control about the transport phenomena (Squires & Quake, 2005; Vilkner *et al.*, 2004; Stone *et al.*, 2004). For this, the microfluidic technology is used to manipulate small volumes of liquids in networks of micro-channels. In protein crystallography, where the preparation of a pure and monodisperse protein sample is required but laborious, a reduction of the used sample volume for the crystallization trials implies a great benefit. Therefore, methods have been developed to perform crystallization trials in microfluidic devices for high-throughput screening with only microliter sample consumption in free interface diffusion, microbatch and vapor diffusion approaches (Hansen *et al.*, 2002; Du *et al.*, 2009; Li & Ismagilov, 2010; Zheng *et al.*, 2005).

The free interface diffusion in a microscale format was the first application of microfluidics in protein crystallography (Hansen *et al.*, 2002). It benefits from the fact that convection is absent in the small volumes normally used by microfluidics. Therefore, after bringing protein in contact with precipitant, their exchange is solely based on diffusion. Precise tuning of the supersaturation was achieved by a combination of vapor diffusion and free interface diffusion (Hansen *et al.*, 2006). A different application of FID was developed in a system called SlipChip, where protein and precipitant are loaded in different chambers of a microfluidic chip. Subsequently, a connection between both chambers is established by slipping the connecting channels of the chip (Du *et al.*, 2009).

In the microbatch method protein and precipitant are mixed to form small droplets of 10 nL volume in microfluidic channels (Zheng *et al.*, 2004; Zheng *et al.*, 2005; Li *et al.*, 2006). By mixing various ratios of protein and precipitant, a broad area of the phase diagram can be covered. The individual droplets are separated from each other by chemically inert fluorocarbon oil, which is immiscible to the aqueous solution. The technique allows setting up thousands of individual crystallization trials, that can be stored in X-ray transparent capillaries. Crystals that have grown in the individual droplets can be analyzed by X-ray diffraction straight within the capillaries.

A similar approach is used in different vapor diffusion applications of microfluidic devices (Lau *et al.*, 2007; Zheng *et al.*, 2004). Contrary to the microbatch method, a water permeable carrier fluid is used which allows dehydration of the formed droplets containing a mixture of protein and precipitant. Dehydration and therewith supersaturation is achieved by placing the complete microfluidic device in

an osmotic bath. Alternatively, droplets containing solely protein can be dehydrated by adjacent precipitant droplets with higher salt concentration.

Despite the great advantage of very low sample consumption, these microfluidic approaches have the drawback that they rely on irreversible kinetic processes which cannot be controlled easily. In an effort to decouple nucleation and growth of protein crystals, a new microfluidic system has been developed and was named Phase Chip (Shim *et al.*, 2007). The aim of this design was to allow an optimization of the kinetic pathway of crystallization. In the Phase Chip all crystallization wells are separated from the reservoir by a thin (poly)dimethylsiloxane (PDMS) membrane, which is permeable to water and small non-polar molecules. The volume of the droplet in the crystallization well can be reversibly controlled by changing the concentration of the solutes in the reservoir. In a later enhancement, the PDMS membrane was exchanged by a regenerated cellulose membrane in order to obtain a membrane which is permeable to the precipitant as well (Michael Heymann, 2014). In this stage the Phase Chip allows navigating through the phase diagram in a variety of dynamic paths and thereby offers a comparable flexibility as achieved with the XtalController, presented in section 2.1. However, up to now the evaluation of the crystallization experiment in all microfluidic approaches is based on visual inspection of the droplets with a microscope. This leads to the fact that an occurring nucleation event or precipitation of the protein can only be observed with a significant time delay. In order to overcome this drawback of a response delay it is investigated, if Dynamic Light Scattering measurements can be performed in the nano-sized volumes of microfluidic devices. The aim is to get an earlier feedback information during crystallization experiments in microfluidic devices and the results are presented in this chapter.

2.2.2 Material and Methods

2.2.2.1 Mask Design

The photolithography masks, used for preparing silicon wafers, are designed by Dr. Michael Heymann (Center for Free Electron Laser Science, Hamburg) using the AutoCAD 2015 software (Autodesk, Inc., San Rafael, USA). The chip structure is imprinted on the silicon wafer in multiple layers of negative photoresist, while an individual mask is used for each layer. Vernier Caliper alignment marks allow the exact positioning of the layers with an error of around 10 μm (Heymann *et al.*, 2014). The CAD-designs are translated into foil masks by the company JD Photo Data (Hitchin, UK). Designed masks for the Phase Chip (2.2.2.4) approach are shown in Figure 2-11.

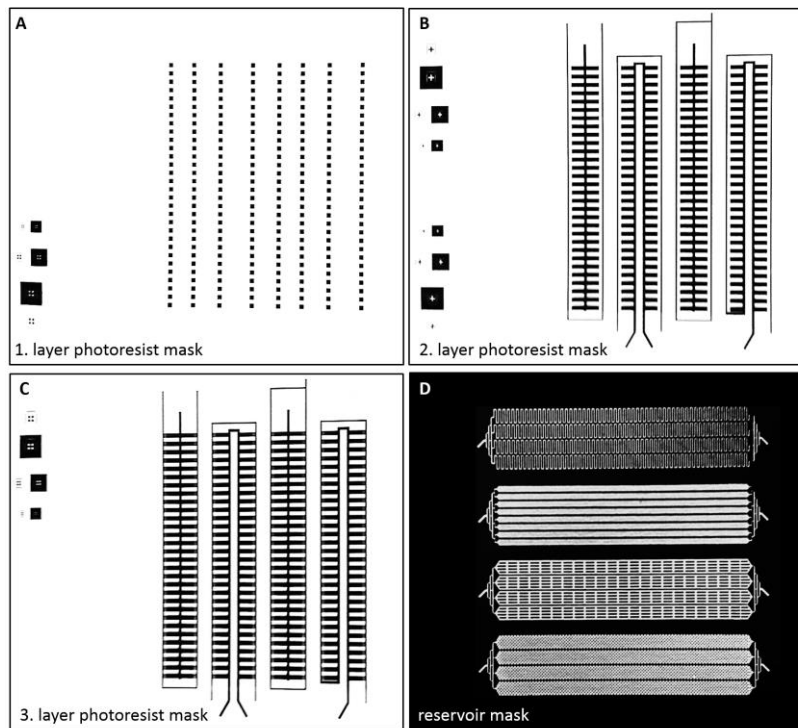


Figure 2-11: Photolithography masks used for preparing silicon wafers of the Phase Chip.

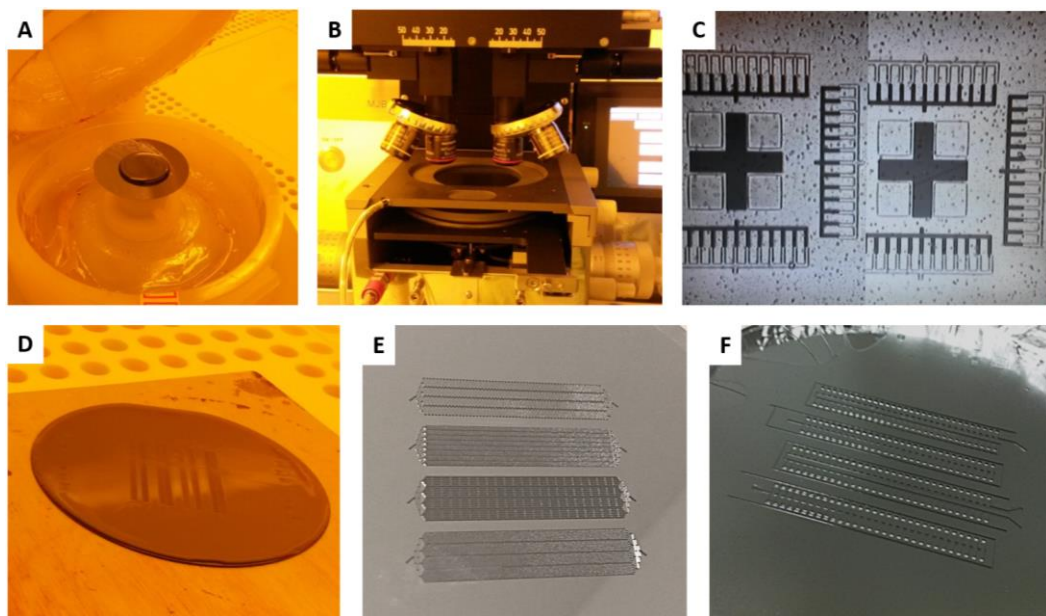
The masks are designed by Dr. Michael Heymann (Center for Free Electron Laser Science, Hamburg) using the AutoCAD 2015 software (Autodesk, Inc., San Rafael, USA). The silicon wafer for the crystallization-well structure of the Phase Chip is made by three layers ([A], [B] and [C]) and the reservoir wafer by one [D].

2.2.2.2 Photolithography

The silicon wafer was either imprinted with the positive or the negative features of the microfluidic chip by using photolithography. A negative master was used for structures directly casted in (poly)dimethylsiloxane (PDMS) (Figure 2-12 D) and a positive master was used for epoxy structures, where an intermediate negative PDMS replica was casted to print the final epoxy pattern (Figure 2-12 F). For this, the negative photoresist SU-8 (MicroChem, Westborough, USA) was spincoated on a 3-inch sized silicon wafer (Figure 2-12 A) (University Wafer, Boston, USA). The thickness of the photoresist layer was controlled by tuning the spinning speed and duration according to the manual and is shown in **Table 2**. Prior UV-light exposure, a soft bake was performed by heating to 65 °C and 95 °C in order to reduce the solvent concentration and to improve the photoresist adhesion to the silicon wafer. The wafer and the corresponding photoresist mask (Figure 2-11) were aligned using a mask aligner (Figure 2-12 B and C) (MJB4, SÜSS MicroTec). The photoreaction was initiated by exposing the photoresist to UV-light in the mask aligner and the reaction was catalytically completed by a subsequent hard bake at 65 °C and 95 °C (Figure 2-12 D). Exposure and baking durations are listed in **Table 2**. Finally, the photoresist, which have been shielded from UV-exposure by the photolithography masks, was washed off by using propylene glycol methyl ether acetate (PGMEA). The described protocol was repeated for each consecutive photoresist layer.

Table 2: Protocol for the preparation of a multilayer photoresist on a silicon wafer by photolithography.

Desired thickness	Photoresist	Spincoating	Soft bake	UV exposure	Hard bake
5 μm	SU-8 3005	1: 500 rpm, 5 s	1: 1 min, 65 °C	9 s	1: 1 min, 65 °C
		2: 3000 rpm, 30 s	2: 3 min, 95 °C		2: 3 min, 95 °C
40 μm	SU-8 3025	1: 500 rpm, 5 s	1: 1 min, 65 °C	11.5 s	1: 1 min, 65 °C
		2: 1800 rpm, 30 s	2: 15 min, 95 °C		2: 5 min, 95 °C
50 μm	SU-8 3025	1: 500 rpm, 5 s	1: 15 min, 95 °C	12.5 s	1: 1 min, 65 °C
		2: 1300 rpm, 30 s			2: 5 min, 95 °C

**Figure 2-12: Silicon wafer preparation by photolithography.**

[A] SU-8 photoresist is spincoated on a silicon wafer. [B] The wafer and the corresponding photoresist mask were aligned using a mask aligner (MJB4, SÜSS MicroTec). [C] Consecutive layers are aligned using Vernier Caliper alignment marks (Heymann et al. 2014). [D] Wafer with positive structures for the crystallization wells. [E] Wafer with negative features of the reservoir structure for direct casting in PDMS. [F] Casting of an intermediate negative PDMS replica used for printing the final epoxy pattern as described in section 2.2.2.3.

2.2.2.3 PDMS mold

The PDMS mold was casted in a petri dish. For this, the petri dish was lined with aluminum foil to facilitate the removal of the cured PDMS from the petri dish. The PDMS, consisting of a mixture of silicone base with 10 % (w/w) curing agent (Sylgard® 184, Dow Corning), was thoroughly mixed (Thinky ARE-250). After placing the silicon wafer in the petri dish, 20 g PDMS were poured on the wafer and degassed in a vacuum desiccator for 5 min in order to avoid bubble formation in the PDMS. The PDMS was cured in an oven for 1 h at 70 °C and was subsequently peeled from the silicon master. Access holes for the fluid were punched through the PDMS with a 0.75 μm biopsy punch (UniCore, Harrison).

2.2.2.4 Chip assembly

PDMS chip

In order to enable dynamic light scattering measurements inside the individual wells of the microfluidic chip, the PDMS mold was bonded onto a glass slide (Corning). For this, the glass slide was thoroughly cleaned and both, the glass slide and the PDMS mold, were plasma activated by 0.4 mbar O₂ plasma (Zepto, Diener electronic) for 30 s. The microfluidic channels in the PDMS structure were carefully orienting parallel to the edges of the glass slide and both were shortly pressed together for bonding. A vertical section scheme of the individual steps of the PDMS chip preparation is shown in Figure 2-13 A. A detailed illustration of the microfluidic structure of the PDMS chip is shown in Figure 2-13 B.

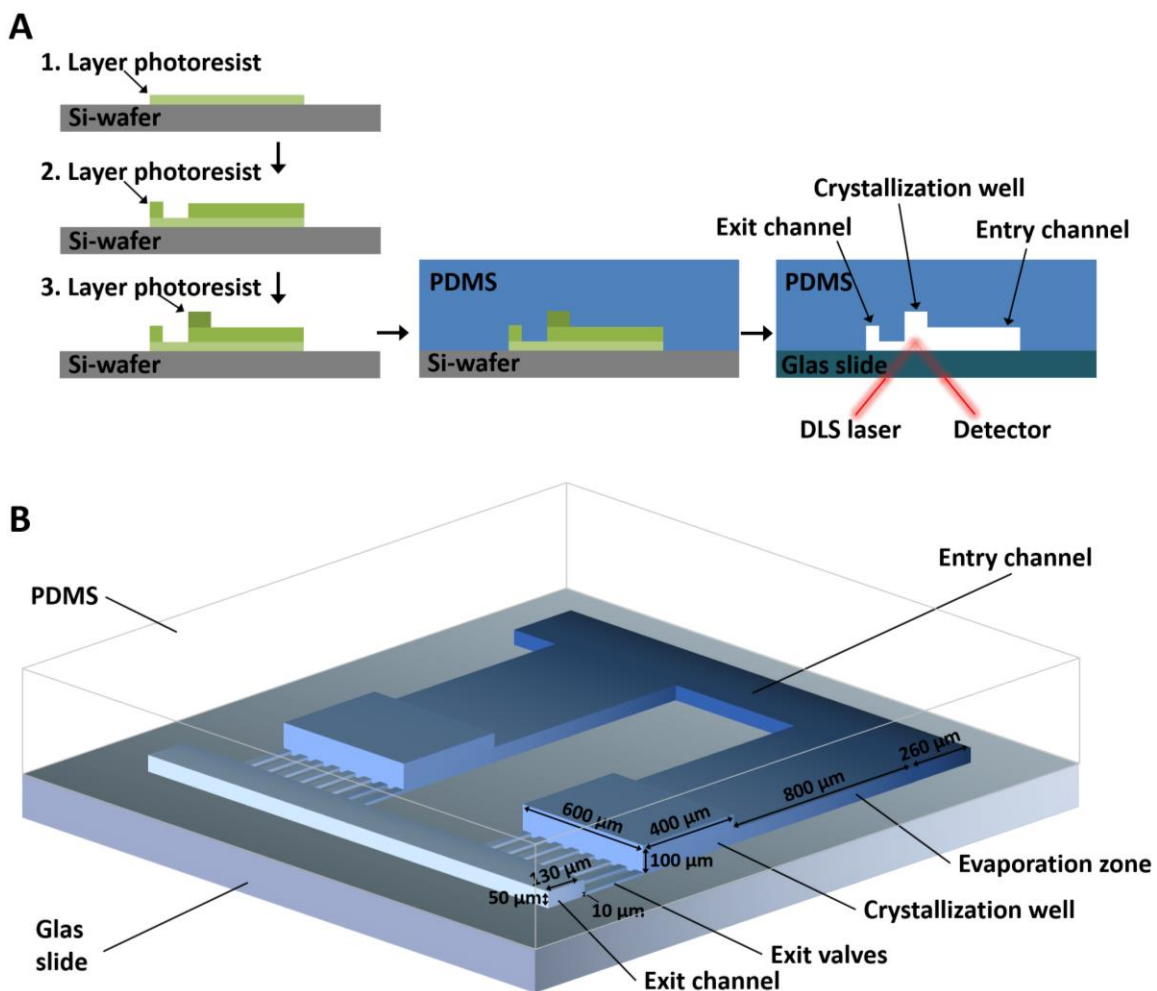


Figure 2-13: Schematic presentation of the PDMS chip.

[A] A vertical cross-section of the PDMS demonstrates how three layers of photoresist are build up on the silicon wafer. PDMS is casted on the structured wafer and is finally bonded on a glass slide. [B] Three-dimensional presentation of the PDMS chip shows the architecture and dimensions of the microfluidic structures.

Phase chip

The phase chip consists of three components: 1) the crystallization wells and fluidic channels, 2) the PDMS membrane and 3) the reservoir. In order to enable dynamic light scattering measurements comparable to those in the PDMS chip, the layer containing the crystallization wells has to point towards a glass slide. To achieve this, the crystallization well structure was imprinted in epoxy glue (UHU Plus Schnellfest 5 min, UHU GmbH Co. KG, DE). The viscosity of the two component glue was reduced by separate dilution with ethanol in an epoxy to ethanol ratio of 10:1. The PDMS mold, containing the negative structures casted from the positive silicon wafer, was degassed in a vacuum desiccator for 30 min. By this, the PDMS mold can absorb small bubbles from the epoxy resin during the molding step. Both components of the epoxy glue were thoroughly mixed and a small droplet was applied in the middle of a clean glass slide. The PDMS mold was pressed on the glass slide and weighted with metal weights for 1 h, until the epoxy resin was cured (Figure 2-14 A).



Figure 2-14: Photographic images of the three components of the Phase chip.

[A] Weighting the PDMS mold during epoxy structure imprinting of crystallization well structures. [B] Casting a PDMS mold of the positive reservoir structures. [C] Oxygen plasma activation (Zepto, Diener electronic) of the PDMS membrane, which separates the crystallization wells and the reservoir structure.

For the second layer, a 10 μm thick PDMS membrane was prepared by spincoating PDMS on the backside of a petri dish. The PDMS, consisting of a mixture of silicone base with 10 % (w/w) curing agent (Sylgard[®] 184, Dow Corning), was thoroughly mixed (Thinky ARE-250). Spincoating was performed using a rotation speed of 500 rpm for 5 s, followed by 3000 rpm for 30 s. The PDMS membrane was cured for 30 minutes at 70 °C.

The third layer contained the reservoir structure and was prepared by a PDMS mold from a silicon wafer containing the positive structure features (Figure 2-14 B). Bonding of the PDMS membrane to the third layer was achieved by pressing together both pieces after plasma activation with 0.4 mbar O₂ plasma (Zepto, Diener electronic) for 30 s (Figure 2-14 C).

The bonded structure of the PDMS membrane and the PDMS reservoir mold was finally bonded to the epoxy structure on the glass slide by (3-Glycidyloxypropyl)trimethoxysilane (GPTS) / (3-Aminopropyl)trimethoxysilane (APTS) chemistry. For this, an aqueous solution of APTS (1 % v/v) and GPTS (1 % v/v) was prepared separately. The glass slide with the epoxy structure and the PDMS membrane/reservoir mold was plasma activated at 0.4 mbar O₂ plasma (Zepto, Diener electronic) for 30 s. One part (e.g. the glass slide with epoxy structures) was incubated in the APTS solution for 5 min, while the other (e.g. the PDMS membrane and reservoir) was incubated in the GPTS solution for 5 min. Both were subsequently dried and pressed together, resulting in the completely assembled phase chip. A vertical section scheme of the individual steps of the phase chip preparation is shown in Figure 2-15.

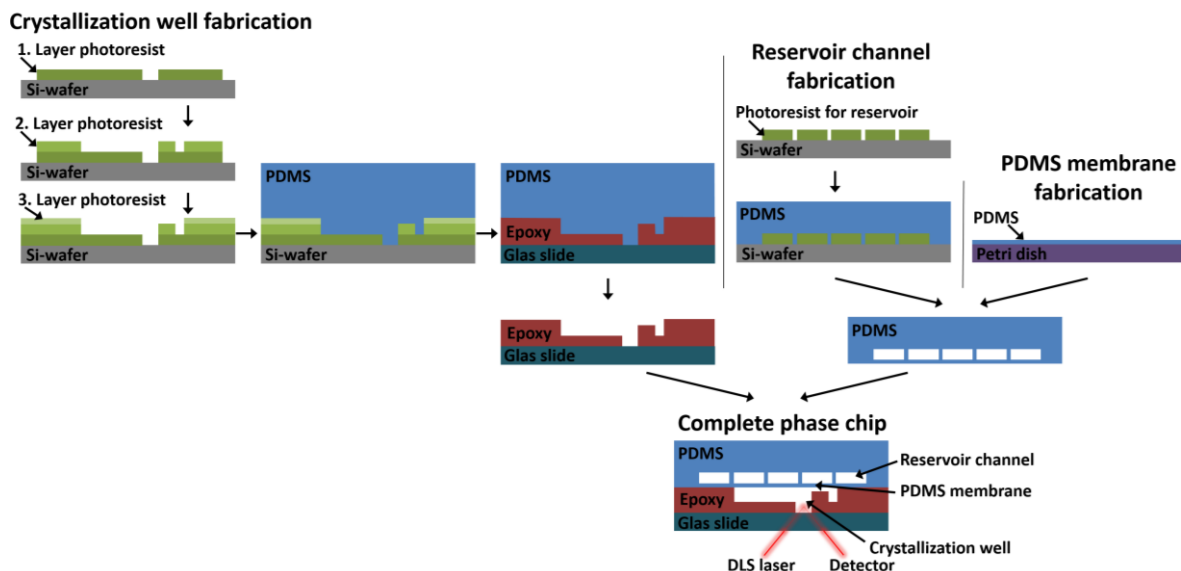


Figure 2-15: Vertical cross-section of the individual steps during Phase chip preparation.

The three components of the Phase chip are prepared separately before they are assembled to form the complete chip. The crystallization wells build up on the silicon wafer by three layers of photoresist. PDMS is casted on the structured wafer and subsequently used to imprint the crystallization well structure in epoxy on a glass slide. In parallel, the reservoir structure is made of a PDMS mold which is casted on a second silicon wafer. Both components are separated by a thin PDMS membrane, spincoated on a petri dish. Final assembly is performed by plasma activation bonding and APTS/GPTS chemistry.

2.2.2.5 Chip surface treatment and handling

Prior filling the chips with protein or reservoir solution, the surface was coated with a hydrophobic reactant. Thus, an interaction of the aqueous protein solution with the surface as well as an emerging of the fluid through the capillary valves into the exit channel can be avoided. For the coating, a solution of 9 % (w/w) CTX-109AE (AGC Chemicals, Exton, USA) in CT-Solv 100 (AGC Chemicals, USA) was used and injected into the chip. In order to allow the solvent to evaporate, the chip was placed on a 190 °C heating plate for 5 min.

The chip was loaded through the access holes using tubing with a diameter matching the access holes for optimal sealing. A protein solution, containing an initially low amount of precipitant, was injected by using a Hamilton syringe (Hamilton, Bonaduz, Switzerland). During chip filling, the exit holes of the main channel were closed to force the protein solution into the crystallization wells, while the air could escape through the exit valves. Proper filling of all crystallization wells was controlled using a binocular. Subsequent to the protein injection, the exit hole was opened and the main channel was rinsed with fluorinated oil (HFE-7500, 3M, USA) in order to separate the individual crystallization wells from each other. Finally, all access and exit holes were sealed after chip filling was completed.

2.2.2.6 Sample preparation

The sample thioredoxin (*W. bancrofti*) was prepared as described in section 1.2.1. The thaumatin (*T. daniellii*) protein solution was prepared as described in section 2.1.2.1. For both proteins the final protein concentration was determined using a Nanodrop ND-2000 (Thermo-Scientific, Erlangen, Germany). The protein solution was filtered through a 0.2 μm centrifugal filter (VWR, Darmstadt, Germany) and was centrifuged for 15 minutes at 16100 x g prior injection in microfluidic devices. Protein concentrations, buffer compositions as well as used precipitant compositions are listed in Table 3.

Table 3: Conditions for crystallization experiments in microfluidic chips. Protein and Precipitant were mixed in one to one ratio.

Protein	Protein concentration	Protein buffer	Precipitant	Experiment shown in Figure
Thioredoxin (<i>W. bancrofti</i>)	30 mg · mL ⁻¹	20 mM Tris-HCl, 5 mM EDTA, 150 mM NaCl, pH 8.0	27.5 % PEG1500, 100 mM SPG buffer, pH 6.3	2-16
Thaumatin (<i>T. daniellii</i>)	34 mg · mL ⁻¹	50 mM Bis-Tris, pH 6.5	0.5 M sodium tartrate, 50 mM Tris, pH 6.8	2-17
Thaumatin (<i>T. daniellii</i>)	20 mg · mL ⁻¹	50 mM Bis-Tris, pH 6.5	0.3 M sodium tartrate, 50 mM Tris, pH 6.8	2-18

2.2.2.7 DLS measurements

Dynamic light scattering measurements were performed using a SpectroLight 600 *in situ* plate reader (XtalConcepts, Hamburg, Germany). The laser has an output power of 100 mW, a wavelength of 660 nm and the scattered light was detected at a scattering angle of 142°. Because all investigated sample solutions were aqueous the refractive index of water ($n = 1.33$) was used for all calculations. Samples were measured at 293 K and each measurement was performed for 30 s. The autocorrelator

(XtalConcepts) of the instrument covers a sample time range from 0.4 μs to 30 s. The decay time constants of the scattering signal are derived from the autocorrelation function by using the CONTIN algorithm (Provencher, 1982). From this, the translational diffusion constant D_t as well as the particle radius can be derived by using the Stokes–Einstein equation (equation 2).

A calibration file was written to find the position of each individual crystallization well in the microfluidic chip and to allow automated DLS measurements over time. When inserting a new chip into the instrument, the measurement position in each well can be screened automatically. For this, five measurement positions were tested in the xy-plane and at each position five z-planes were tested. In case a reliable DLS measurement position was identified, which is defined by an autocorrelation curve with a high intercept and a smooth tail towards large correlation times, the coordinates were saved for later measurements. The calibration file, as well as the search pattern can be found in the Appendix.

2.2.3 Results and Discussion

2.2.3.1 Establishing DLS measurements in microfluidic chips

First attempts to perform DLS measurements in small compartments of a microfluidic chip were performed in a chip provided by Dr. Michael Heymann (Center for Free-Electron Laser Science, Hamburg). The chip consisted of a PDMS mold bonded on a glass slide in order to provide an optically transparent entry side for the DLS laser. The microfluidic chip had a serial design of circular crystallization wells with a diameter of 500 μm and a height of 50 μm . The chip was filled with a premixed solution of thioredoxin (*W. bancrofti*) and corresponding precipitant (Table 3).

For the first DLS experiments the laser was manually aligned in a single crystallization well. Due to the small height of the wells an automated positioning of the laser in different wells was not successful. The ACF of the DLS measurement showed a high intercept of approximately 1.8 and no oscillation in the tail of the curve. This demonstrated that a DLS measurement in a PDMS chip bonded to a glass slide can be successfully performed. The radius distribution of the protein solution in a single crystallization well was monitored over 20 hours (Figure 2-16 B). Already in the beginning of the experiment a second radius fraction with a size around 200 nm is visible. This can be explained by the fact that protein and precipitant have already been mixed before both were loaded into the chip, comparable to microbatch crystallization trials under oil. Protein crystals become macroscopically visible 12 hours after mixing of protein and precipitant (Figure 2-16 A). Interestingly, a strong increase in the DLS signal intensity can be observed after 10 hours, corresponding to larger crystal nuclei in solution (Figure 2-16 C). The volume of the droplet in the crystallization well of the microfluidic chip

shrinks due to slow evaporation of water through the semipermeable PDMS mold over time. On the one hand this leads to the intended effect of solute concentration in the droplet like in other vapor diffusion experiments, on the other hand this is problematic when conducting long-term DLS measurements to follow the nucleation process. Over time the droplet size might shrink to an extent that the DLS measurements are not performed in the shrunk droplet anymore, as can be seen in the image series in Figure 2-16 A.

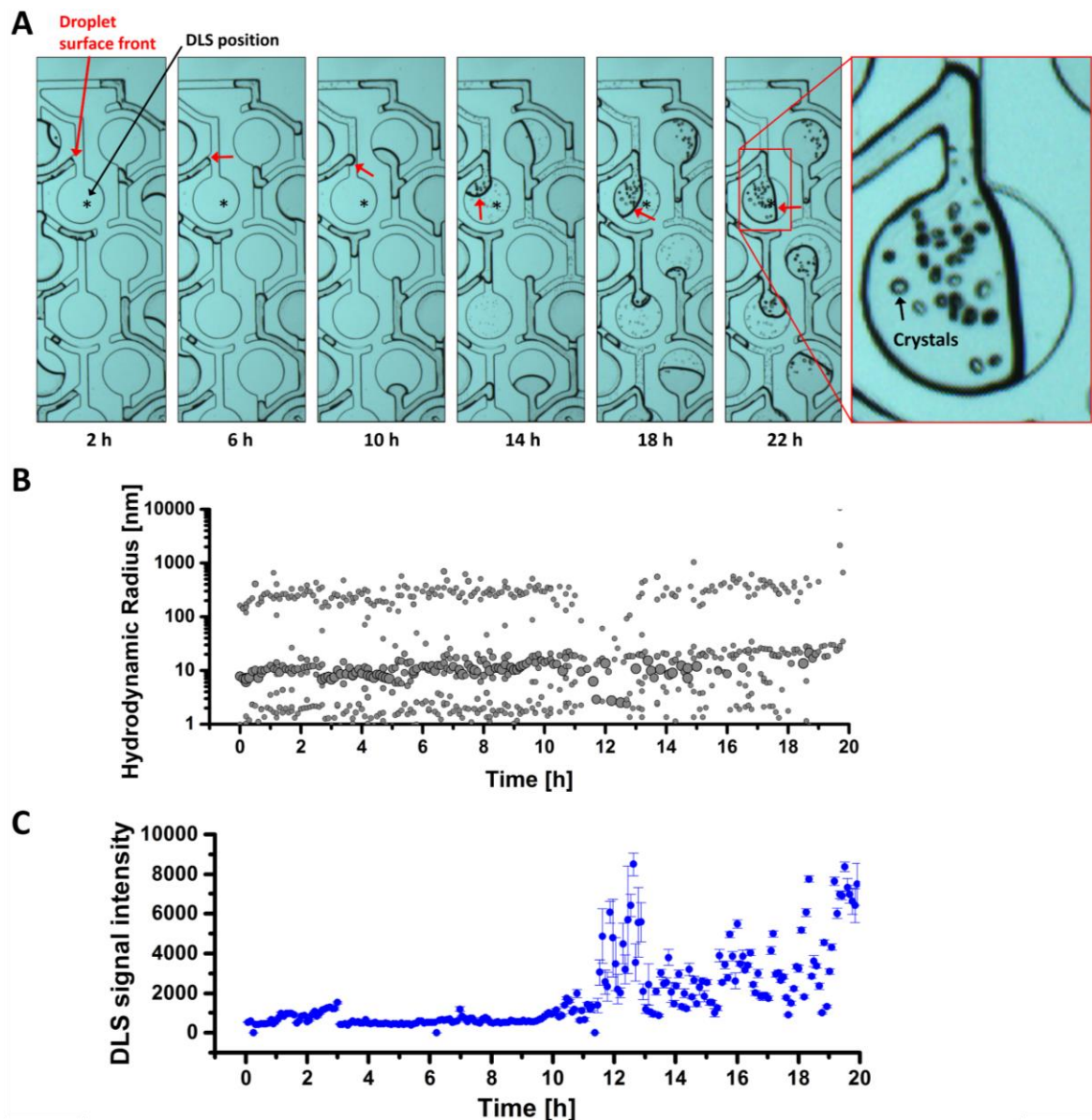


Figure 2-16: Following the crystallization process of thioredoxin by DLS measurements in a PDMS chip.

[A] Microscopic image series to follow changes in the crystallization droplets within the PDMS chip. Shrinking of the droplet volume can be observed over time due to slow water evaporation through the PDMS (Droplet surface front indicated by red arrow). The diameter of one crystallization well is $500\ \mu\text{m}$. [B] Radius distribution pattern over time, obtained from DLS measurements in a single well of the PDMS chip. [C] An increase in the DLS signal intensity after approximately 10 hours indicates initial nucleation events before microcrystals can be seen in the image series (diameter of crystallization well = $500\ \mu\text{m}$).

2.2.3.2 Optimizing Chip design for dynamic light scattering measurements

Based on the findings of the initial experiment, the microfluidic chip geometry was optimized for DLS measurements. In a new and improved parallel chip design an evaporation zone was included on both sides of the crystallization well (Figure 2-17 A). By this, the crystallization well, where the DLS measurement is performed, is not immediately affected by shrinking of the fluid volume in the compartment upon evaporation. Additionally, the thickness of the crystallization well is increased from 50 μm to 100 μm to allow an automated search of the DLS measurement position. In order to test the new design, a PDMS chip bonded on a glass slide (Figure 2-13) is filled with a one-to-one ratio of thaumatin ($34 \text{ mg} \cdot \text{mL}^{-1}$) and sodium tartrate (0.5 M) (Table 3). The evaporation is followed over 18 hours (Figure 2-17 B) and reveals, that the volume reduction upon solvent evaporation starts from the main channel and does not affect the crystallization well throughout the experiment.

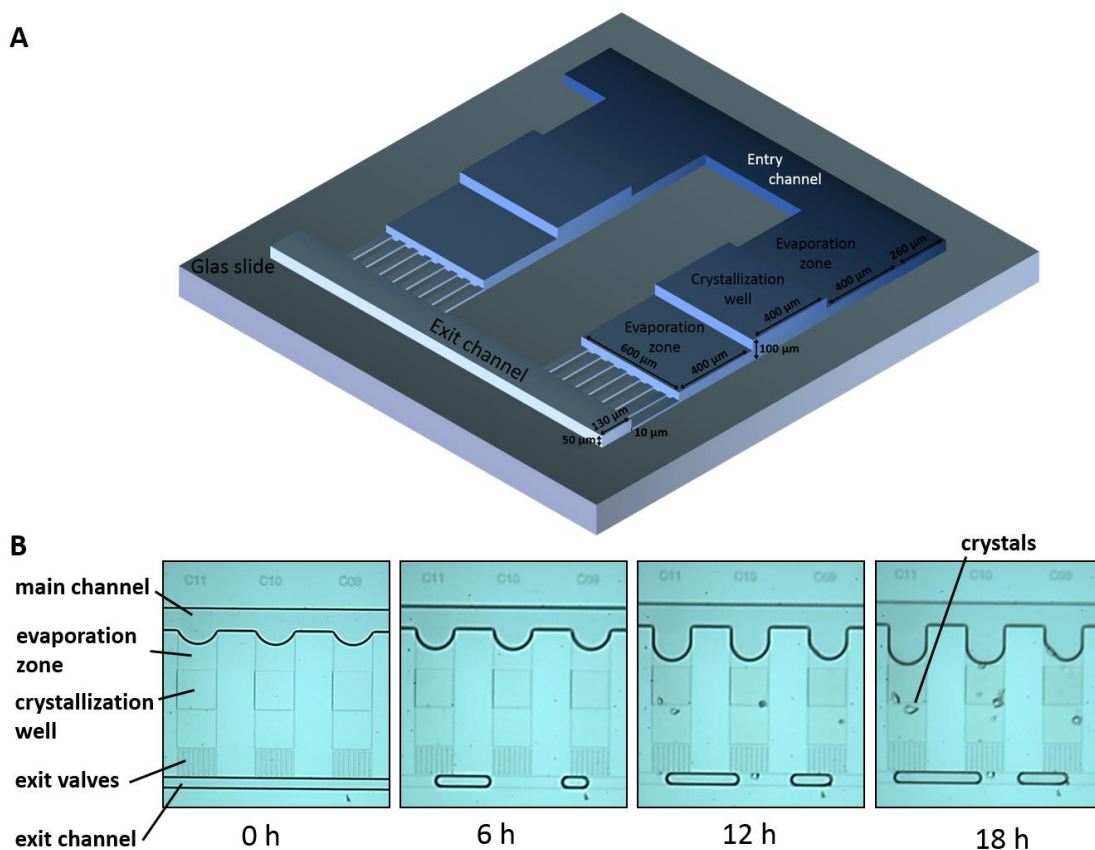


Figure 2-17: Observation of solvent evaporation in an optimized PDMS chip filled with a thaumatin protein solution.

[A] A schematic presentation of the new PDMS chip design reveals the architecture and dimensions of the microfluidic structures. Evaporation zones on both sides of the crystallization well are added in order to allow solvent evaporation without affecting the crystallization well where the DLS measurements are performed. [B] The image series of the evaporation process reveals that the droplet shrinks from the side of the main channel and not from the exit channel. The crystallization well remains unaffected from evaporation until larger Thaumatin crystals have grown.

However, no shrinking from the side of the exit valves is observed. Consequently, the position of the crystallization well can be relocated towards the side of the exit valves, in order to maximize the use of the evaporation zone. The large evaporation zone and stronger volume shrinking allows a significant shift towards supersaturation in the phase diagram. Therefore, the PDMS chip can be filled with an initially lower protein and precipitant concentration and the oligomeric state of the protein in the under-saturated zone of the phase diagram can be monitored. This enhances the possibility to observe nucleation and crystal growth by DLS in microfluidic devices.

Based on the initial results, a PDMS chip was designed with crystallization wells located next to the exit valves. The new chip (Figure 2-13) was filled with a lower protein and precipitant concentration in a one-to-one ratio of thaumatin ($20 \text{ mg} \cdot \text{mL}^{-1}$) and sodium tartrate (0.3 M) (Table 3). The automated search of the DLS measurement position in each well of the complete PDMS chip was successful. The recorded ACFs showed reliable DLS measurements with an intercept around 1.8 and a smooth tail in the beginning of the experiment (Figure 2-18 C). Exemplarily, the evolution of the size distribution as a function of time of the thaumatin particles in a single crystallization well is shown in Figure 2-18 B together with the corresponding recorded camera images (Figure 2-18 A). As expected, it can be seen that the shrinking of the volume starts from the main channel and keeps the crystallization compartment unaffected throughout the experiment. Due to the lower initial precipitant concentration in the beginning of the crystallization experiment the hydrodynamic radius of thaumatin can be followed while the protein is still undersaturated and before nucleation starts. After approximately two hours a second radius fraction becomes visible and more distinct over time (Figure 2-18 B). This demonstrates that the nucleation can be observed far before macroscopic crystals are observed in the camera image (after 4 hours). The results provide evidence that automated DLS measurements can be performed inside individual compartments of a microfluidic chip in a volume as small as 24 nL and allows to follow the nucleation process during protein crystallization.

2.2.3.3 Towards a Phase Chip for controlled navigation in phase diagram

The results demonstrate that the nucleation of protein crystals can be observed by DLS in the PDMS chip. However, the used PDMS design does not provide a high degree of flexibility in controlled positioning the protein solution in the phase diagram. The solution in the chip undergoes a typical path in the phase diagram, as known from other vapor diffusion approaches. In order to enable controlled navigation in the phase diagram by using a microfluidic device, like it can be done with the XtalController (2.1), a more complex chip design has to be used. By introducing a permeable membrane into the chip which separates the crystallization compartment from a reservoir, a reversible concentration and dilution of the crystallization condition becomes possible by changing the

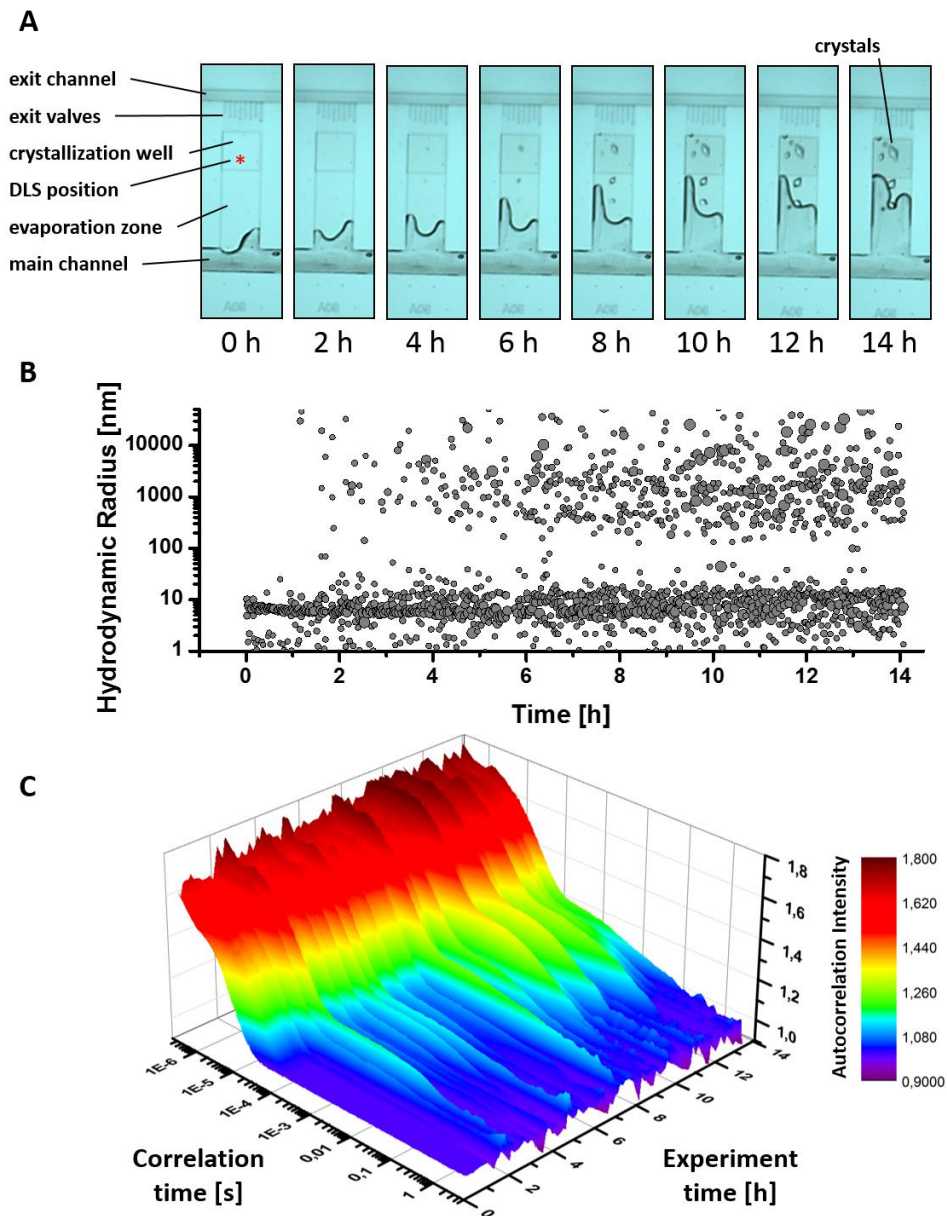


Figure 2-18: Automated DLS measurements in a microfluidic PDMS chip with optimized design.

[A] Microscopic images of the crystallization process and the concentration of the solution over time. Initial microcrystals can be observed after 4 hours. [B] Hydrodynamic radius distribution over time of the Thaumatin particles during the crystallization process. The formation of a second radius fraction, indicating initial nucleation events can be seen after approximately 2 hours. [C] Surface presentation of the recorded ACF of the DLS measurements over time.

Concentration of the reservoir solution (Figure 2-15) (Shim *et al.*, 2007). Thus, immediately after entering the nucleation zone in the phase diagram the supersaturation can be reduced to keep the solution in the meta-phase and thereby to facilitate crystal growth. The water flux through a PDMS membrane with a thickness of 15 μm to dry air is about 2 nL per hour in a 100 μm by 100 μm surface area of PDMS membrane (Shim *et al.*, 2007). To allow this mass exchange rate, the established chip design permitting for DLS measurements was extended to a phase chip approach (for preparation see

section 2.2.2.4). In order to preserve the good optical properties for the DLS laser, the chip needs to be bonded on a glass slide. Therefore, the structures of the crystallization compartments are stamped in a thin epoxy film directly on the glass slide. For the reservoir structure a PDMS mold is casted and the reservoir side is sealed with the thin permeable PDMS membrane. Finally, both parts are combined to assemble the complete phase chip. A photographic documentation of the individual steps is shown in Figure 2-19.

A critical parameter for the stability of the chip is the design of the reservoir structures. Support structures have to be embedded inside the reservoir, in order to support the thin PDMS membrane. If these are not present, pressure fluctuations during loading of the chip can easily disrupt the membrane. Four different types of reservoir structures have been tested and preliminary experience from the manufacturing process suggest that the design number 3 in Figure 2-19 is most suitable. The architecture combines a large reservoir surface, needed for rapid exchange between crystallization wells and reservoir, with sufficiently large support structures for the PDMS membrane.

Instead of using several separated reservoir channels also a microfluidic gradient structure could be used to induce a concentration gradient over the chip area. The usability of the Phase Chip has to be further elucidated with precise microfluidic pumps that are needed for chip filling and continuous and controlled exchange of the reservoir condition during the crystallization experiment.

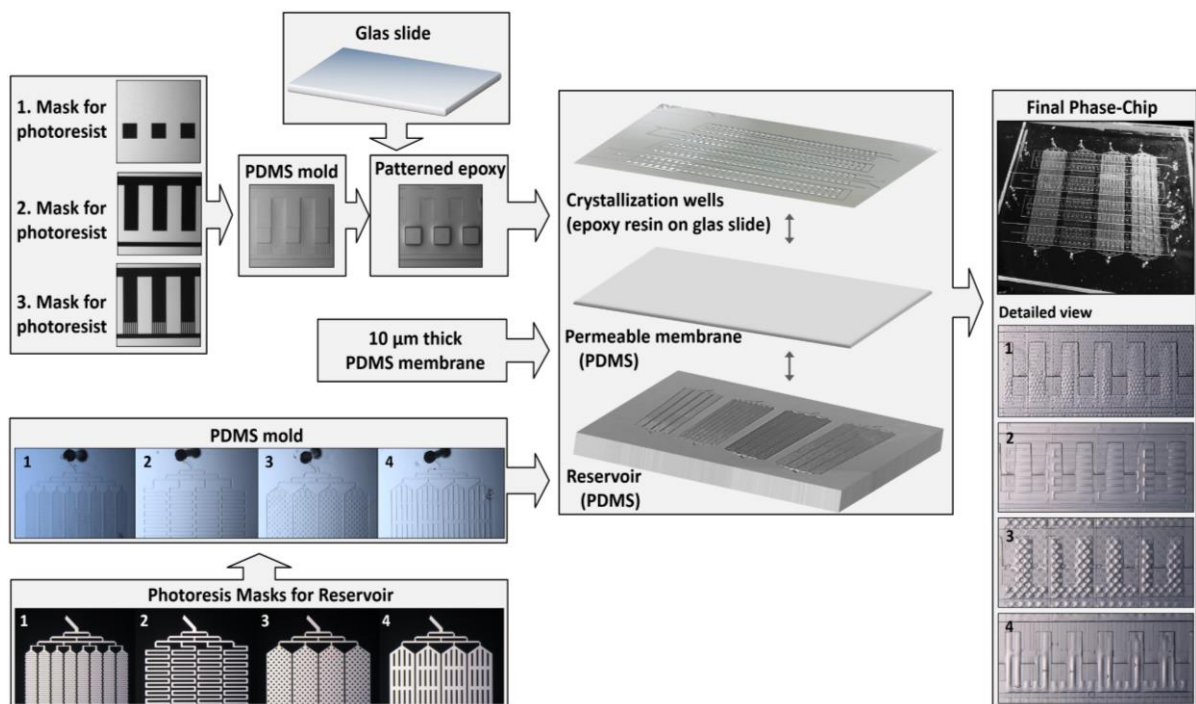


Figure 2-19: Photographic presentation of the individual steps of Phase Chip preparation.

The chip contains three components, the reservoir structure casted as a PDMS mold, the crystallization wells imprinted in epoxy on a glass slide and a thin PDMS membrane between both to allow for water exchange. The final Phase Chip facilitates in-chip DLS measurements to get feedback information about the crystallization processes during controlled navigation in the phase diagram.

2.2.4 Conclusion

It could be shown that DLS measurements can be successfully performed inside a microfluidic device in individual wells with a volume of 24 nL. Furthermore, an optimized chip design facilitates automated measurements in over hundred different crystallization wells, which allows for simultaneous monitoring of the crystallization processes in multiple buffer conditions while keeping the sample consumption low. The integration of an evaporation zone facilitates long term measurements without disturbing the DLS measurement itself. However, determining the concentration of protein and precipitant during the crystallization experiment is not as straight forward as with the XtalController, where the required information about changes in the droplet are obtained from the microbalance. Measuring the volume of the droplet in the microfluidic chip during shrinking, based on an automated evaluation of the microscope images using software like ImageJ, can possibly circumvent this limitation in the future.

In general, up to now the qualitative and quantitative evaluation of the crystallization process in microfluidic device is solely based on visual inspection with a microscope. By measuring DLS in microfluidic devices highly valuable feedback information can be obtained. In combination with the presented microfluidic Phase-Chip, it results in a high degree of flexibility when charting a course through the phase diagram. After this first proof-of-principle measurements, this method can be further extended by exchanging the PDMS membrane with a regenerated cellulose dialysis membrane. This would allow for a change of the precipitant composition, addition of cryo-protectant after crystal formation or introduction of ligands for crystal soaking experiments.

CHAPTER 3

3. RELIABLY DISTINGUISHING PROTEIN NANOCRYSTALS FROM AMORPHOUS PRECIPITATE BY DEPOLARIZED DYNAMIC LIGHT SCATTERING

3.1 Introduction

The interest in protein nano- and microcrystals for protein structure determination did substantially increase over the last years. This is particularly related to the invention of a revolutionary new method called serial femtosecond X-ray crystallography (SFX) (Chapman *et al.*, 2011; Schlichting, 2015; Martin-Garcia *et al.*, 2016). For SFX ultrashort X-ray pulses of very high brilliance produced by X-ray free electron lasers (XFELs) are focused on protein micro- or nanocrystals. From each exposed crystal in random orientation only one single diffraction image can be recorded. Because all atoms inside the crystal are fully ionized by the transferred electromagnetic energy of the FEL X-ray pulse, the crystal is destructed by a coulomb burst. However, the exposure time to record a diffraction pattern is short enough to record a single image before the atoms have significantly moved (Chapman *et al.*, 2011; Neutze *et al.*, 2000). Consequently, several thousand crystals have to be exposed by X-rays in random orientation and all single diffraction pattern have to be merged in order to obtain a complete dataset (Boutet *et al.*, 2012; Liu *et al.*, 2013; White *et al.*, 2012). Because of this, the conventional goal in protein crystallization to produce one single large protein crystal is shifted to the production of thousands of nano- or microcrystals with homogeneous size, when SFX experiments are performed. Additionally, a careful sample characterization and verification is essential in order to use XFEL beam time most effectively. So far, quality assessment of sample suspensions used for SFX data collection relies on time and labor intensive interpretation of electron-microscopy images or powder diffraction patterns.

Therefore, the development of novel, fast and reliable methods for nanocrystal preparation and quality control are of great demand. Crucial properties in the characterization of nanocrystal suspensions are the size distribution of the crystals, the total amount and concentration of the crystals in the suspension and the quality in terms of internal order. For the preparation of protein nanocrystals several methods have been developed including batch methods (Wu *et al.*, 2015), crushing of larger crystals (Stevenson *et al.*, 2014b; Stevenson *et al.*, 2014a), free interface diffusion (Kupitz *et al.*, 2014)

and manipulative techniques using vapor diffusion as described in section (2.1). Additionally, *in vivo* crystallization in SF9 insect cells has been successfully used for SFX experiments (Koopmann *et al.*, 2012; Redecke *et al.*, 2013), although the application of *in vivo* crystallization to a variety of proteins still needs to be evaluated.

Up to now, methods for identification and characterization of nano- or microcrystals are mainly limited to ultraviolet fluorescence (Dierks *et al.*, 2010), second harmonic generation (SHG) (Wampler *et al.*, 2008), X ray powder diffraction (Dreele, 2007) and electron microscopy (Stevenson *et al.*, 2014b; Falkner *et al.*, 2005). All these methods have a great potential, but also suffer from some fundamental limitations. So far only crystals with low symmetry and considerable size produce a sufficiently intense second harmonic (SHG) signal that can be detected (Kissick *et al.*, 2011). For ultraviolet fluorescence the recorded intensity greatly depends on the number of disulfide bonds or aromatic residues within the macromolecule, and for electron microscopy a labor-intensive sample preparation involving chemical crosslinking is required. Therefore, X-ray powder diffraction is still the most powerful method for sample characterization, because it provides qualitative information about the protein crystals. However, it is an invasive method which requires a rather large sample volume and a readily available X-ray source.

In this chapter, an alternative novel and non-invasive method is presented which is called depolarized dynamic light scattering (DDLS). Its potential to identify the presence of nanocrystals already in early stages of the crystallization process is tested. The detection method is based on optical properties like birefringence that leads to the ability of crystalline material to depolarize laser light. Birefringence can be defined as a variation in refractive index, sensitive to direction in a geometrically ordered material. The detected depolarized signal in the DDLS instrument is a combination of form birefringence and intrinsic birefringence (Oldenbourg & Ruiz, 1989; Bragg & Pippard, 1953). The first, form birefringence, is a result of the crystal morphology itself, while the latter, intrinsic birefringence, is based on the anisotropy of the individual macromolecules in the crystal lattice (Owen & Garman, 2005). In the presented DDLS method a crystallization experiment is monitored online and the number of depolarized and polarized photons from the scattered light is quantitatively analyzed. By this, it becomes possible to distinguish between the initial growth of ordered crystal and amorphous precipitation in solution. Additionally, the obtained results can give further information about the suggested theory of a two-step nucleation mechanism with a transition to a higher concentration prior to a transition to a higher order (Vekilov, 2004). This becomes possible, because the DLS signal reports about a formation of protein-dense liquid clusters, while the detected depolarized DLS signal specifically reports about the transition to a higher order within these clusters.

3.2 Material and Methods

3.2.1 Sample preparations

Crystallization trials with various proteins as well as a set of measurements with different reference samples have been performed with the newly constructed DDLS instrument (in collaboration with XtalConcepts, Hamburg, Germany) in order to investigate the capabilities of the instrument to monitor the nucleation and growth of protein nanocrystals.

Adjusting the DDLS setup was performed by using anisotropic gold nanoparticles (A12-25-600 and A12-40-750), in the following referred as Au-600 and Au-750, which have been obtained from the company Nanopartz (Loveland, USA). The particle solutions have been diluted with ultrapure water to a concentration of approximately 2.1×10^{10} particles mL^{-1} and were sonicated (ultrasonic bath, Branson, Danbury, USA) for 10 min before use for shape determination experiments by DDLS.

The isotropic particle counter standards (3020A, 3K-400, 3K-600, 3K-1000 and 4K-02) have been purchased from Sigma-Aldrich (Taufkirchen, Germany). The initial particle concentration of 1×10^9 particles mL^{-1} has been sequentially diluted after each measurement with ultrapure water, until a DLS signal intensity below 100 kHz was reached.

The proteins lysozyme (*Gallus gallus*), thaumatin (*T. daniellii*) (both Sigma-Aldrich, Taufkirchen, Germany) as well as glucose isomerase (*Streptomyces rubiginosus*) (Hampton Research, Aliso Viejo, USA) have been purchased. The protocol for the production and purification of the protein thioredoxin (*W. bancrofti*) has been described in section 1.2.1. All final protein concentrations are verified photometrically using a Nanodrop ND-2000 (Thermo-Scientific, Erlangen, Germany) and are listed conjointly with all used buffers in Table 4.

3.2.2 Batch crystallization in a DDLS cuvette

For online monitoring of nucleation and crystals growth via DDLS, the protein crystals were grown within a small cuvette (101.015-QS, Hellma Analytics, Müllheim, Germany). By siliconizing the cuvette, capillary effects at the inner edges of the cuvette have been avoided. For the siliconization the cuvette was incubated for 1 min in an isopropanol solution containing silicone (Serva Electrophoresis, Heidelberg, Germany). Consequently, the surface of the solution can be considered to be equal to the base area of the cuvette, which is 9 mm^2 , and thereby extensive evaporation is prevented. After removing the cuvette remaining isopropanol was evaporated, the cuvette was washed with ultrapure water and dried prior usage. For the crystallization experiments all protein solutions have been centrifuged for 15 min at $16100 \times g$ at $20 \text{ }^\circ\text{C}$. After this, $20 \text{ }\mu\text{L}$ of the buffered protein solution were pipetted into the cuvette, the cuvette was placed in the holder of the DDLS instrument and the initial

hydrodynamic radius of the investigated protein was determined. To induce supersaturation of the protein solution, the corresponding precipitant was pipetted into the cuvette and the solution was thoroughly mixed. For all proteins the individual precipitant conditions as well as the used volumes are listed in Table 4. All utilized solutions were prepared using ultrapure water and have been filtered through a 0.2 μm filter (Sartorius, Göttingen, Germany) before use. The DLS and DDLS measurements have been performed continuously at 20 °C with a duration of 30 s and a time interval of 30 s between consecutive measurements.

Table 4: Batch crystallization conditions of all investigated proteins with space groups of the resulting crystals.

Protein	Protein concentration	Protein buffer	precipitant	Precipitant volume added	Space group and PDB code
Lysozyme (Hen egg white lysozyme, <i>Gallus gallus</i>)	100 mg · mL ⁻¹	100 mM sodium acetate, pH 4.3	0.9 M sodium chloride, 1 % PEG8000, 0.1 M sodium acetate, pH 3	20 μL	P4 ₃ 2 ₁ 2
Thioredoxin (<i>Wuchereria bancrofti</i>)	30 mg · mL ⁻¹	20 mM Tris-HCl, 5 mM EDTA, 150 mM NaCl, pH 8.0	27.5 % PEG1500, 100 mM SPG buffer, pH 6.3	20 μL	P4 ₁ 2 ₁ 2
Thaumatococcos (<i>Thaumatococcus daniellii</i>)	34 mg · mL ⁻¹	50 mM Bis-Tris, pH 6.5	0.5 M sodium tartrate, 50 mM Tris, pH 6.8	20 μL	I4 ₂ 22
Glucose isomerase (<i>Streptomyces rubiginosus</i>)	28 mg · mL ⁻¹	10 mM HEPES, 1 mM MgCl ₂ , pH 7.0	100 mM Bis-Tris, 2.7 M ammonium sulfate, pH 5.7	35 μL	I222
Glucose isomerase (<i>Streptomyces rubiginosus</i>)	28 mg · mL ⁻¹	10 mM HEPES, 1 mM MgCl ₂ , pH 7.0	100 mM Bis-Tris, 1.35 M ammonium sulfate, pH 5.7	30 μL	I222

3.2.3 Setup of the depolarized dynamic light scattering instrument

The DDLS instrument has been developed in collaboration with the company XtalConcepts (Hamburg, Germany). A schematic as well as photographic representation of the instrument is shown in Figure 3-1. For the DLS and DDLS measurements a sapphire laser with a wavelength of 532 nm and an output power of 100 mW (Coherent, Dieburg, Germany) has been used. The laser is deflected by a mirror (Cage Cube-Mounted Protected Aluminum Turning Mirror, Thorlabs, Dachau, Germany) and the incident light is vertically polarized (Thorlabs, Dachau, Germany).

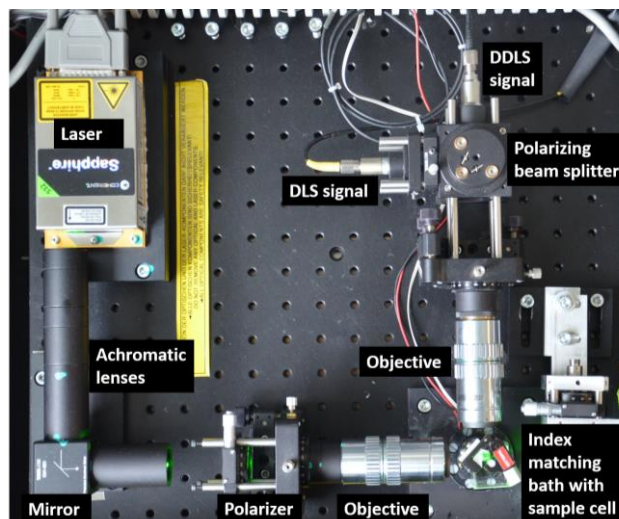
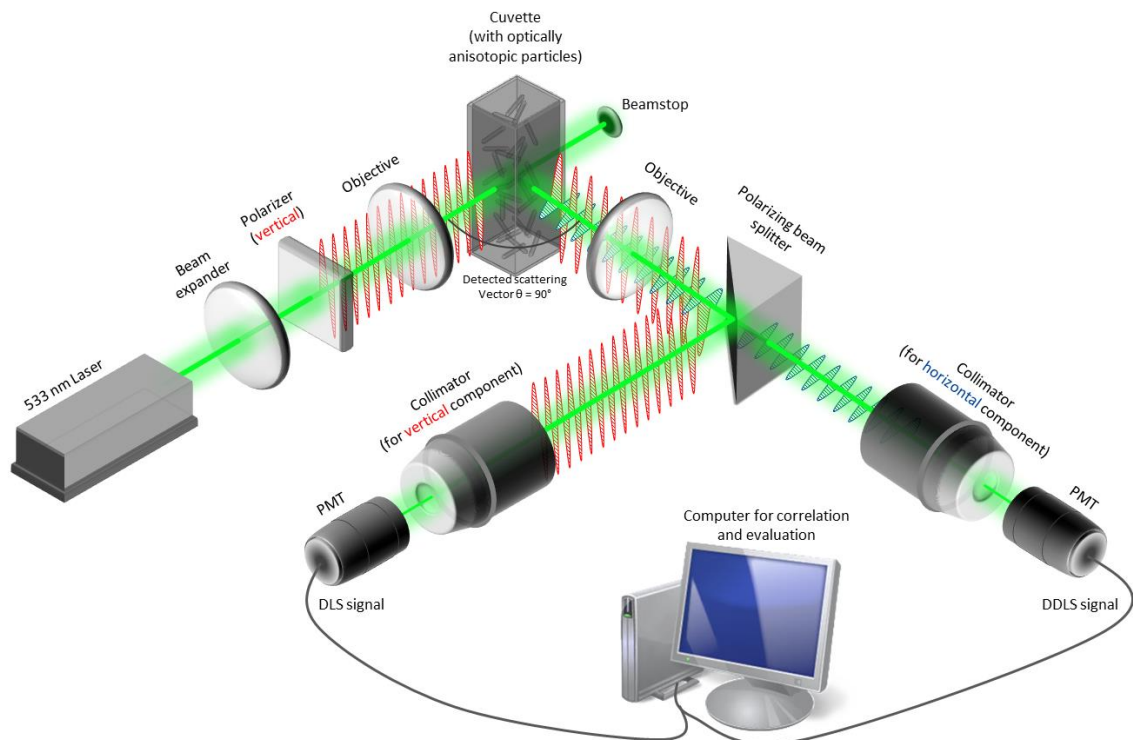


Figure 3-1: Depolarized dynamic light scattering (DDLS) instrument.

Schematic presentation (upper part) of the assembly of the optical components of the DDLS device and photographic top view of the instrument (lower part).

After expanding the beam by a factor of two, using two achromatic lenses, it is focused into the sample cell by an objective (Plan APO ELWD 20x 0.42 WD=20) in order to obtain a small DLS measurement volume. The sample cuvette (3 x 3 x 21 mm) was placed in an index matching bath with plane parallel walls (thickness 1 mm) and a size of 5 mm around the focal point, which was filled with prefiltered (0.2 μm Filter, Sartorius, Göttingen, Germany) ultrapure water. The focal spot of the laser and detector channel have been aligned by two tilt adjusters. A scattering angle of 90° was used and the scattered light was collected by an objective (Plan APO ELWD 20x 0.42 WD=20), resulting in a scattering vector q of $2.22 \times 10^7 \cdot \text{m}^{-1}$ or $4.5 \cdot 10^8 \text{ m}^{-1}$ for a wavelength of 532 nm and a refractive index of 1.33. The collected scattered light was separated by a polarizing beam splitter (Qioptic Photonics, Göttingen, Germany) into the horizontally and vertically polarized components providing the depolarized (DDLS) and polarized (DLS) signal, respectively. The light was then guided from the beam splitter to the photomultiplier tubes (Hamamatsu, Herrsching am Ammersee, Germany) by fiber cables. The autocorrelators of the DDLS instrument have been manufactured by XtalConcepts (Hamburg, Germany) and cover a sample time range from 0.4 μs to 30 s.

3.2.4 Evaluation of the depolarized dynamic light scattering data

For the evaluation of the DLS measurements the refractive index of water (1.33) was used, because all investigated sample solutions were aqueous. From the autocorrelation functions (ACF) of the DLS and DDLS signal the decay time constants of the translational diffusion and rotational diffusion are derived by using the CONTIN algorithm (Provencher, 1982), respectively. From this, the translational diffusion constant D_t is derived by the Stokes–Einstein equation,

$$D_t = \frac{k_B T}{6\pi\eta r}. \quad (2)$$

The rotational diffusion constant D_r can be determined from the rotational decay time constant by the Stokes-Einstein-Debye equation,

$$D_r = \frac{k_B T}{8\pi\eta r^3}. \quad (3)$$

For both equations k_B is the Boltzmann constant, η is the viscosity, T is the temperature and r is the particle radius. Consequently, both diffusion constants, D_r and D_t , were measured independently by this method. Because of this, DDLS can be used to obtain shape information (e.g. of gold nanoparticles) in solution by approximating the particles as rotational ellipsoids. The particle radius (r) is replaced by two minor half-axes (a_1 and a_2) and one major half-axis (b) as shown in Figure 3-2. The values can be calculated by an iterative procedure applying Perrin's equation that has been previously described in detail (Chayen *et al.*, 2004).

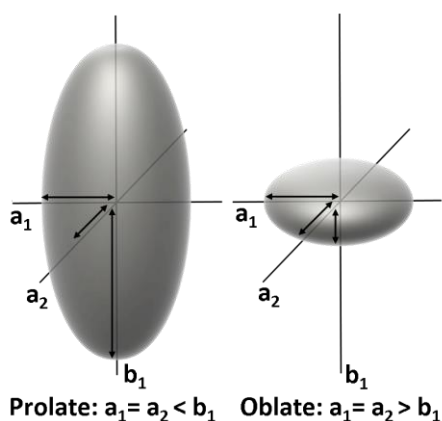


Figure 3-2: Approximating particles as rotational ellipsoids.

Two minor half-axes (a_1 and a_2) and one major half-axis (b) are introduced to distinguish between prolate and oblate particle shapes.

3.2.5 Second harmonic generation and ultraviolet two-photon excited fluorescence

Second harmonic generation is a specific signal that only occurs if laser light passes a chiral crystalline material. Testing the batch crystallization samples from the DDLS experiments on the presence of crystalline material has been performed using the SONICC instrument (Formulatrix, Bedford, Germany). For this, 400 nL of each individual sample were pipetted onto a Lipid Cubic Phase Sandwich Set (Hampton Research, Aliso Viejo, USA) and the individual wells have been sealed with siliconized cover slips. Images were recorded in bright field (exposure time: 15 ms), ultraviolet two-photon excited fluorescence (UVTPEF) (laser intensity: 37 mW, exposure time: 1.789 s) and SHG mode (laser intensity: 195 mW, exposure time: 1.789 s) with a gain of 1.

3.2.6 X-Ray diffraction analysis

The DDLS samples have also been analyzed by X-ray powder diffraction to analyze and verify crystallinity. For this, 20 μ L of each sample suspension from an DDLS experiment were transferred from the cuvette to a quartz capillary tube with a diameter of 0.3 μ m (HR6-108, Hampton Research, Aliso Viejo, USA) and solid components of the sample were pelletized by centrifugation (20 min, 3600 \times g). After cutting the capillaries to appropriate length by a capillary stone (Hampton Research, Aliso Viejo, USA) they were sealed with wax (Harvard Dental International). Diffraction images were recorded after mounting the capillary onto a 3-axis goniometer and aligning the sample pellet in the X-ray beam. A MAR image plate detector in combination with a Rigaku RU 200 X-ray generator ($\text{Cu K}\alpha = 1.54 \text{ \AA}$) was used to record powder diffraction pattern at room-temperature. Each sample was exposed to X-rays for 20 min and oscillated for 2 degrees during exposure. The sample to detector distance was 250 mm.

3.2.7 Scanning electron microscopy

For evaluating the sample content of the DDLS experiments by scanning electron microscopy the sample needs to be stabilized by chemical cross-linking. For this, 15 μL of each solution were transferred into a 1.5 mL Eppendorf tube and centrifuged for 5 min at 2600 \times g. After discarding the supernatant 1 mL of the sample buffer, containing the final precipitant concentration supplemented with 2.5 % (w/v) glutaraldehyde, were added to the tube and the solution was mixed thoroughly. The samples were incubated for 48 hours at room-temperature and have been centrifuged for 5 min at 2600 \times g, subsequently. The supernatant was replaced by ultrapure water and the washing process was repeated two times. The washed crystal pellet was resuspended in 50 μL ultrapure water. For preparing the microscopy specimens, 5 μL of the aqueous crystal solution was pipetted and dried onto round glass cover slips (10 mm diameter). The cover slips were fixed on SEM specimen mount stubs (Electron Microscopy Sciences, Hatfield, USA) and the sample has been sputtered with a thin film of gold by using a Q150T Sputter coater (Quorum Technologies, Laughton, UK) in order to reduce charging during electron microscopy. Scanning electron microscopy images were recorded using a FEI XL-30 Environmental Scanning Electron Microscope which was operated at 15 kV with a specimen distance of 6 mm.

3.3 Results and Discussion

3.3.1 Characterizing size and shape of nanoparticles

The functionality of the experimental setup was verified by using anisotropic gold nanoparticles (section 3.2.1). These particles are a good reference control, because their dielectric constant leads to a strong depolarized component of the scattered light. The recorded autocorrelation functions reveal that the dominant decay time constant of the DLS autocorrelation function (ACF) is $183.9 \pm 26.5 \mu\text{s}$ and $112.6 \pm 36.3 \mu\text{s}$, for Au-600 and Au-750 respectively. Thereby, for Au-600 it is $97.8 \mu\text{s}$ and for Au-750 it is $144.6 \mu\text{sec}$ slower in comparison to the DDLS ACF (14.8 ± 4.5 for Au-600 and $39.3 \pm 8.6 \mu\text{s}$ for Au-750) (Table 5). The mean signal intensity from 10 measurements of the Au-600 sample was 16327 ± 594 photons per second in the DLS channel and 3088 ± 164 photons per second in the DDLS channel. Similar values were obtained for the Au-750 sample (DLS: 12925 ± 495 photons \cdot s $^{-1}$; DDLS: 3950 ± 129 photons \cdot s $^{-1}$). Using the decay time constants of the gold nanoparticles, the shape of the particles can be calculated in an iterative procedure visualized in Figure 3-3. Several values for the semiaxis a are tested and a correct solution is defined when an intercept of semiaxis b is found with the same semiaxis a value for the translational and rotational diffusion constants.

Table 5: DDLS results of gold nanorods Au-600 and Au-750. Measurement parameters are DLS and DDLS signal intensities (count rates Γ) as well as translational and rotational time constants (τ). Calculated diameter and length of the particles in comparison to the values provided by the manufacturer (Nanopartz), shown in parentheses.

Sample	$\Gamma_{tr.}$ [kHz]	$\Gamma_{rot.}$ [kHz]	$\tau_{tr.}$ [μ s]	$\tau_{rot.}$ [μ s]	Semi axis a [nm]	Semi axis b [nm]	Aspect ratio
Au-600	16327 \pm 594	3088 \pm 164	112.6 \pm 36.3	14.8 \pm 4.5	17.6 \pm 8.5 (12.5)	44.1 \pm 1.7 (23.5)	2.5 (1.9)
Au-750	12925 \pm 495	3950 \pm 129	183.9 \pm 26.5	39.3 \pm 8.6	30.75 \pm 9.7 (20)	56.0 \pm 4.3 (69)	1.8 (3.5)

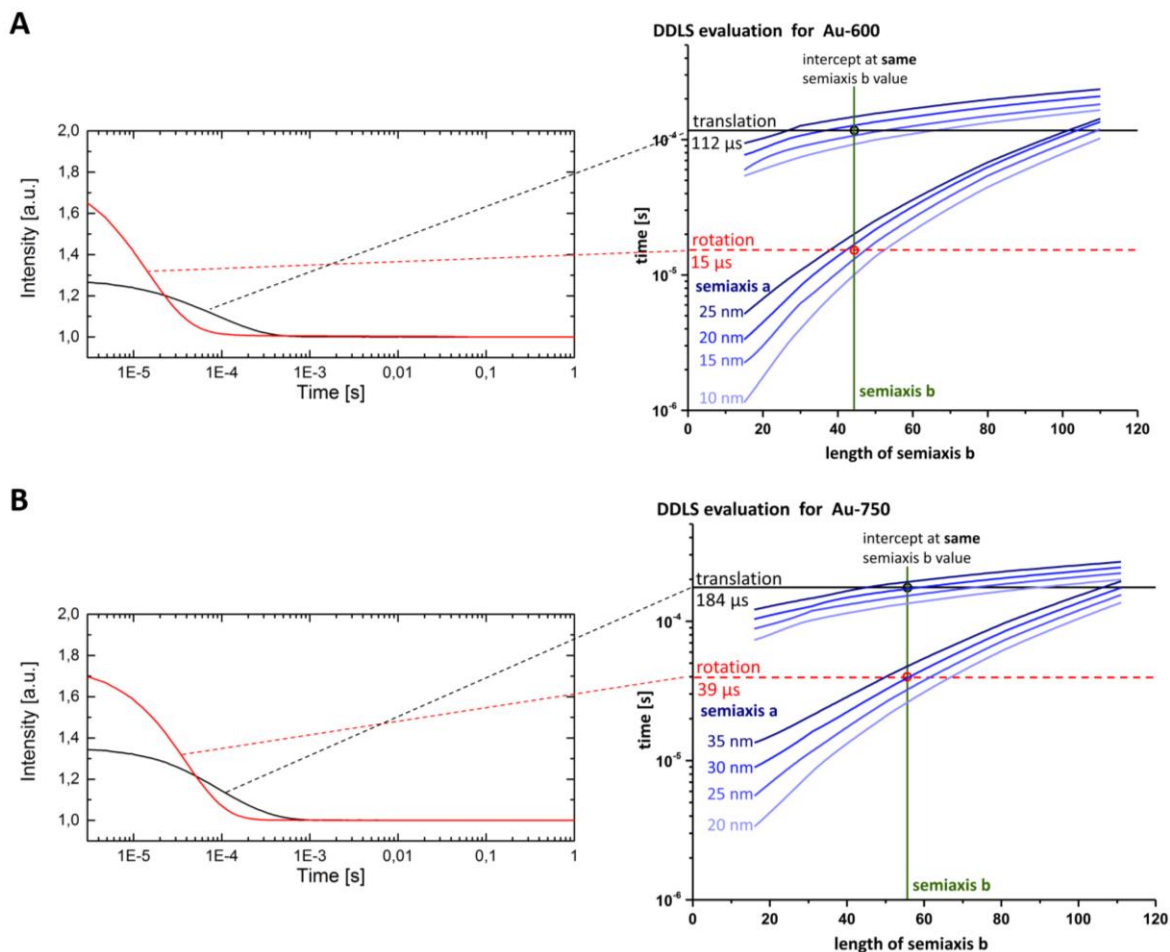


Figure 3-3: Size and shape determination based on the autocorrelation function (ACF) recorded by the DDLS instrument of the translational (black) and rotational (red) diffusion.

[A] The rotational (red) and translational (black) diffusion time constants of the Au-600 sample are taken for the iterative shape determination procedure by testing several values for the semiaxis a (in blue). A correct solution is defined when an intercept of semiaxis b (green line) is found with the same semiaxis a value (between 15 nm and 20 nm) for the translational and rotational diffusion constants. [B] Similar procedure as described in [A] for Au-750.

By this, for Au-600 the length of the minor half-axis was determined to be 17.6 nm \pm 8.5 nm and the length of the major half-axis was calculated to be 44.1 nm \pm 1.7 nm, as shown in Figure 3-3 A. For Au-750 rod shaped particles with a minor half-axis of 30.8 nm \pm 9.7 nm and a major half-axis of 56.0 nm \pm 17.4 nm was identified (Figure 3-3 B). The identified size dimensions are in acceptable agreement

with those provided by the manufacturer, determined with transmission electron microscopy (values are listed in Table 5). The measurements with both gold nanoparticles validate that the DDLS setup is adjusted correctly. Additionally, it demonstrates that DDLS could be used as a valuable method to determine the shape of biological particles like viruses or even protein monomers, after further optimization of the instrument for this approach.

3.3.2 Contribution of multiple scattering to depolarized signal

The detected DDLS signal intensity depends on the intensity of the incoming laser light, the radius and concentration of the sample and the ability of the sample to turn the polarization plane. At high sample concentrations multiple scattering might occur and can easily dominate the DDLS signal. Therefore, perfectly isotropic particles, which provide a very weak DDLS signal, are used to determine the contribution of multiple scattering to the intensity of the depolarized signal. The monodisperse isotropic particles are polystyrene spheres with well-defined size (Sample diameter: 20 nm, 400 nm, 600 nm, 1000 nm and 2000 nm). From each sample a serial dilution was prepared and the DLS as well as the DDLS signal intensities was measured from all concentrations. By plotting the fraction of the DDLS signal from the DLS signal against the particle concentration a strong dependence becomes apparent (Figure 3-4). The reason for this is, that multiple scattering occurs at higher particle concentrations and leads to an increase of the DDLS signal in respect to the DLS signal. Additionally, a disproportional dependency on the particle size becomes apparent for particle concentrations where multiple scattering dominates the depolarized signal. Because larger particles scatter more light, multiple scattering already occurs at lower particle concentrations. Consequently, the measured DLS signal intensity, which is proportional to the amount of scattered light, can be used to identify a threshold indicating when multiple scattering dominates the recorded depolarized signal. From the performed experiments with isotropic particles it can be seen, that the fraction of the DDLS signal remains constantly small as long as the DLS intensity remains below 5000 photons per second (kHz). This is represented as a roughly horizontal line connecting each measured concentration in Figure 3-4. In contrast, multiple scattering leads to a strong increase in the fraction of the DDLS signal, as observed in measurements of higher particle concentrations with DLS signal intensities above 5000 kHz, shown as empty squares in Figure 3-4. Because the refractive index of protein crystals (tetragonal lysozyme: 1.54-1.58 at 589 nm (Cervelle *et al.*, 1974)) and the used isotropic polystyrene spheres (polystyrene spheres: 1.59 at 589 nm) is in the same range, the identified DLS signal intensity threshold of 5000 kHz can be applied for all experiments of monitoring protein crystallization. Consequently, in the following measurements are only considered, when the DLS signal intensity stays well below 5000 kHz.

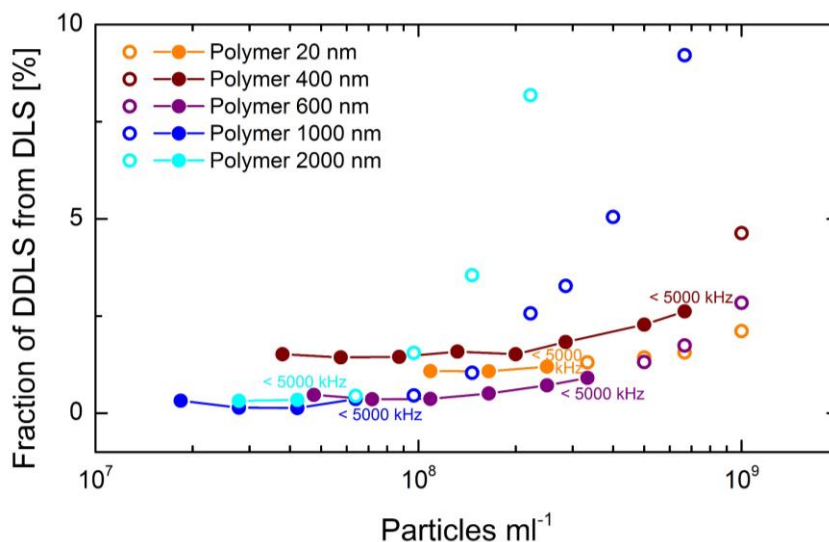


Figure 3-4: Contribution of multiple scattering to the intensity of the detected depolarized signal.

DDLS measurements are performed from a dilution series of spherical polystyrene particles of various sizes. The percentage of the DDLS signal from the DLS signal is plotted against the particle concentration. Empty circles represent measurements, where the DLS signal intensity exceeds 5000 kHz. For these high particle concentrations, multiple scattering leads to a strong increase in the percentage of the DDLS signal. For lower DLS signal intensities the contribution of the DDLS signal is concentration independent, resulting in a straight line with a small slope.

3.3.3 Monitoring crystal growth and distinguishing between protein nanocrystals and amorphous precipitate

The experiments to follow the nucleation and crystal growth by DDLS have been conducted with the proteins thioredoxin, thaumatin, lysozyme and glucose isomerase (Table 4). For this, supersaturation of the protein solution is induced in the cuvette of the DDLS instrument. The transition from a lower to a higher order within a protein cluster, as well as the early phase of crystal growth is monitored. Similar to the experiments using the XtalController (section 2.1) a second radial fraction with a size of approximately 100 nm appeared shortly after the addition of the corresponding precipitant. While the monomer signal stayed constant the second radius fraction continued to grow (Figure 3-5). Together with the appearance of the second radial fraction around 100 nm also an increase in the DLS signal intensity is detected. In contrast, the signal intensity in the DDLS channel did not increase directly after the occurrence of the second radius fraction. This indicates, that the detected particles at this stage are rather disordered cluster of higher protein concentration, than particles with a crystal lattice. In agreement with the obtained results from the XtalController experiments (section 2.1) and the theory of a two-step mechanism of nucleation, the signal intensity of the DDLS channel did increase with a significant time delay (Figure 3-5). The increase of the signal intensity indicates the transition to a higher order within these clusters and is a result of the ability of anisotropic crystals to change the polarization plane of the incoming laser light.

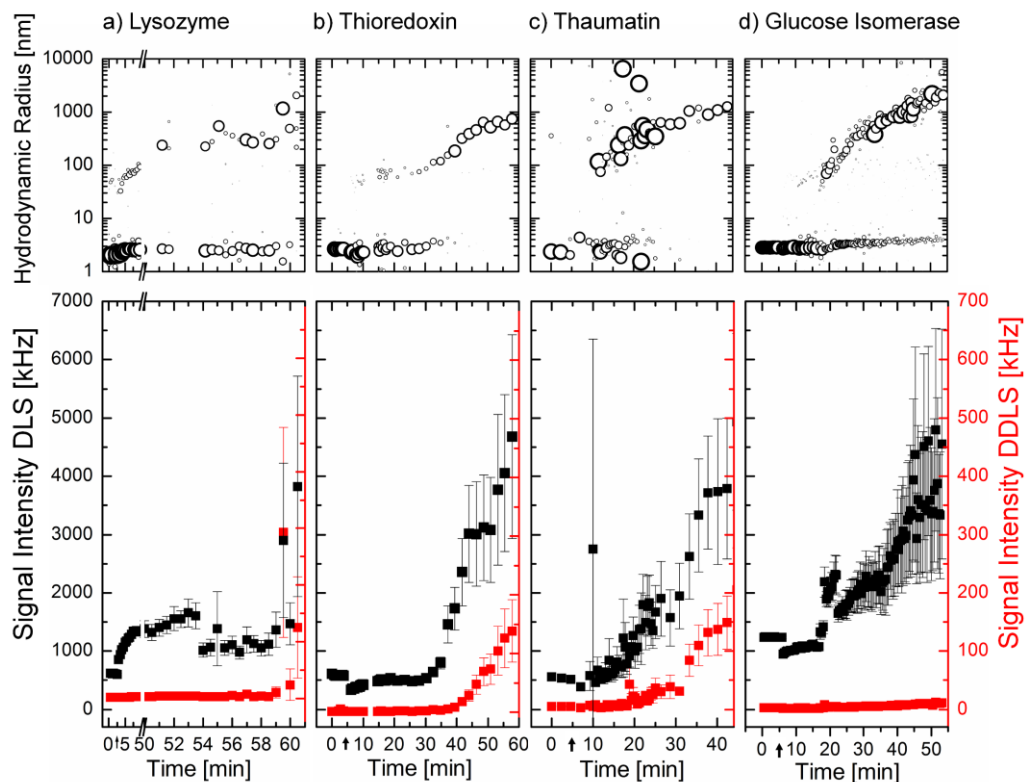


Figure 3-5: Radius distribution and signal intensity evolution for DLS and DDLS over time.

The upper graph shows the radius distribution of the proteins (a) thioredoxin, (b) thaumatin, (c), lysozyme and (d) glucose isomerase. The radius in the beginning of the experiment is representing the monomeric protein. A second radius fraction with a size of around 100 nm occurs after addition of the precipitant (black arrows) and was slowly increasing further. The corresponding signal intensities for the polarized (black) and depolarized (red) signal are shown in the lower graphs. An increase in the DDLS signal intensity can be detected for thioredoxin, thaumatin and lysozyme towards the end of the experiments, while the DLS signal intensity was still well below 5000 kHz. No increase in the DDLS signal intensity was detected for glucose isomerase. (reprinted with permission of the IUCr *Journal of Applied Crystallography* from Schubert *et al.*, 2015).

It is important to mention, that a contribution of multiple scattering to the DDLS signal intensity can be neglected because the DLS signal intensity remains well below the identified threshold of 5000 kHz. Additionally, a control experiment was conducted with glucose isomerase where a precipitant concentration was chosen that is known to produce amorphous precipitate instead of protein crystals (Echalier *et al.*, 2004). As expected no increase in the DDLS signal intensity was observed during the whole experiment. This demonstrates that no DDLS signal is detected from amorphous aggregates, whereas anisotropic crystals give a strong DDLS signal.

After performing the experiments in the cuvette of the DDLS instrument a small volume of each sample was sequentially diluted with the appropriate crystallization solution. By this, it was confirmed that the increase in the DDLS signal intensity is not attributed to multiple scattering. It can be seen that after diluting the sample back below a DLS signal intensity of 5000 kHz, the percentage fraction of the DDLS signal intensity from the DLS signal for the lysozyme sample was constantly around 2.5 % (Figure 3-6). In contrast, no significant DDLS signal was recorded after dilution of the glucose isomerase sample.

Additionally, the DDLS signal intensity of the strongly depolarizing gold nanorods is shown for comparison. After dilution of the Au-650 sample below a signal intensity of 5000 kHz the DDLS fraction of the DLS signal was around 7.5 % (Figure 3-6).

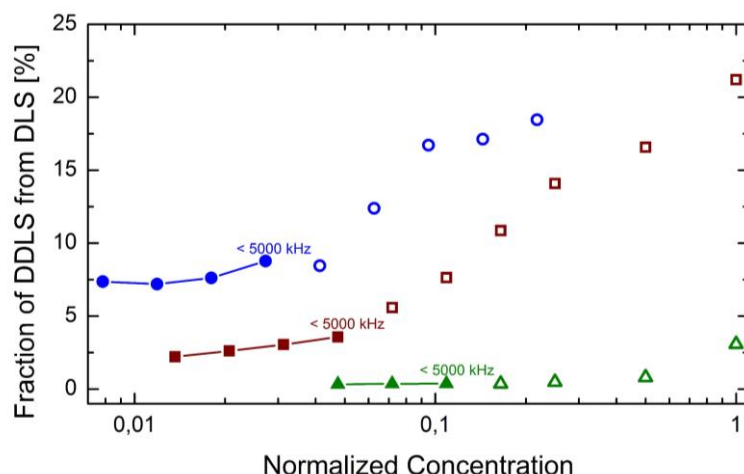


Figure 3-6: Evaluation of the contribution of multiple scattering to the DDLS signal intensity in the crystallization experiments.

A serial dilution was performed from the lysozyme (red) and glucose isomerase (green) sample after the experiments in the DDLS cuvette. Measurements with DLS signal intensities larger than 5000 kHz are displayed in empty symbols. For lysozyme a DDLS signal intensity of around 2.5 % was determined, while no significant DDLS signal was recorded for glucose isomerase after dilution below a DLS signal intensity of 5000 kHz. For comparison Au-650 (blue) is shown to provide a DDLS signal intensity of around 7.5 %.

3.3.4 Verification of DDLS results with complementary methods

Following the crystallization experiments in the DDLS instrument, aliquots of each sample were investigated by using X-ray powder diffraction, bright field imaging, second harmonic generation imaging, intrinsic fluorescence imaging, and scanning electron microscopy. Microscopy analysis in bright field mode revealed, that granular particles with a size of a few micrometers were found in the samples of thioredoxin, thaumatin and lysozyme (Figure 3-7 B). Additionally, intrinsic fluorescence was detected from these particles by ultraviolet two-photon excited fluorescence (Figure 3-7 D). In contrast, only some faint particles, which cannot be identified to be crystalline, are visible in the bright field image of glucose isomerase. Also the fluorescence signal was less defined compared to the other samples. The intensity of the recorded second harmonic generation (SHG) signal strongly depends on the symmetry as well as the orientation of the crystal. The intensity of a SHG signal decreases with increasing symmetry of the crystal. The crystals of thioredoxin, lysozyme and thaumatin have a tetragonal space group (Table 4) and consequently a very weak SHG signal is expected, in particular if the crystals are small. Only from glucose isomerase, which is expected to crystallize in an orthorhombic space group, a strong SHG signal can be seen in the control experiment (Figure 3-7 C). However, in all samples from the DDLS experiments no SHG signal is detected in the images recorded with the SONICC

instrument (Figure 3-7 C). This demonstrates the necessity of additional complementary methods like DDLS, because the SHG signal strongly depends on the symmetry of the crystal lattice. A more reliable confirmation about the sample content was obtained by environmental scanning electron microscopy (ESEM) and recording X-ray powder diffraction pattern of the pelletized samples. The ESEM images of the samples thioredoxin, thaumatin and lysozyme provide evidence that crystals of great size uniformity have grown during the DDLS experiment (Figure 3-7 E and F). Albeit their small size, the typical shape of the different crystals is already clearly visible. It was found that the glucose isomerase sample mainly contained amorphous aggregates and only a very limited number of microcrystals. Likewise, also no powder diffraction pattern could be recorded from glucose isomerase (Figure 3-7 A). Both methods confirm that the glucose isomerase sample contained no significant number of particles with a crystalline lattice, which is in agreement with the results from the DDLS experiment, where no increasing DDLS signal intensity was observed in this sample.

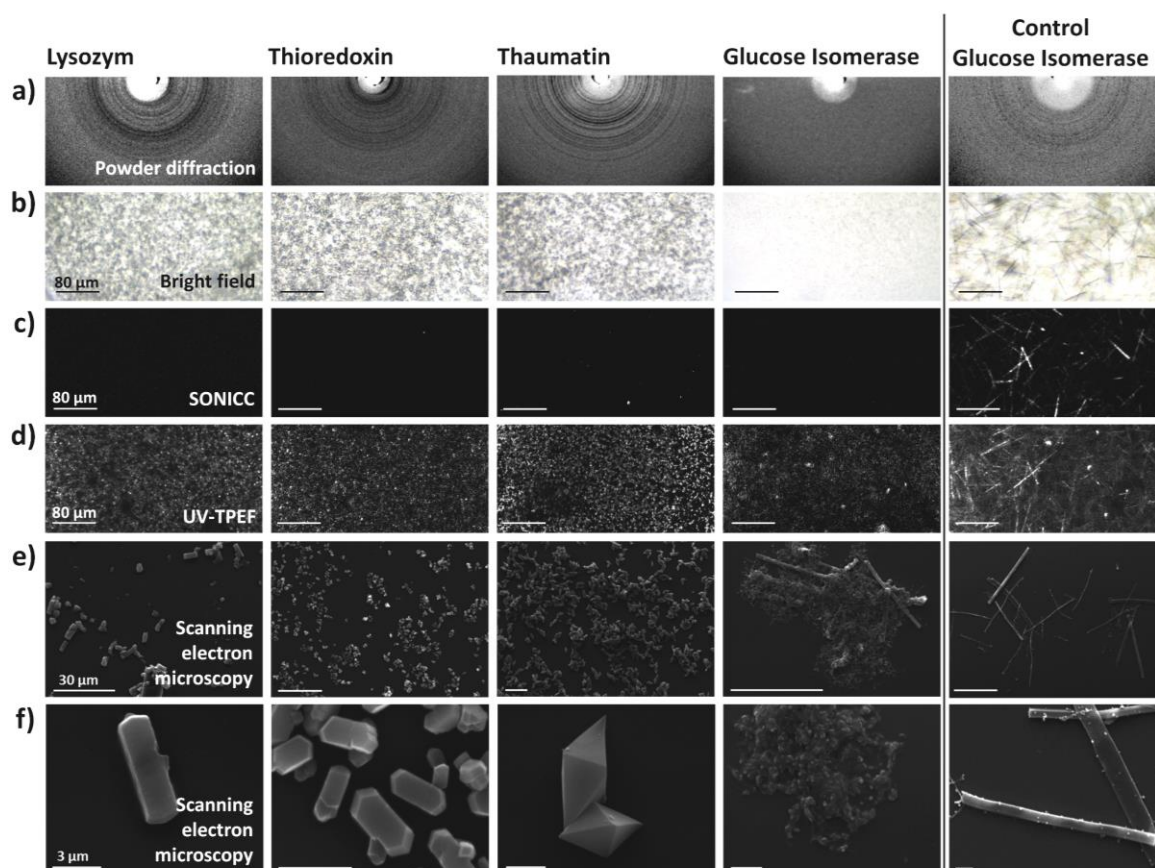


Figure 3-7: Verification of sample content after crystallization experiments with the DDLS instrument.

Samples were analyzed using (1) X-Ray powder diffraction and the SONICC instrument in (2) bright field, (2) SHG and (3) UV-TPEF mode. For [a] thioredoxin, [b] thaumatin and [c] lysozyme a powder pattern was recorded with diffraction up to 6 Å. Granular particles were observed in bright field and UV-TPEF mode. For [d] glucose isomerase no powder pattern was detected and the bright field and UV-TPEF images revealed less distinct particles. No additional information was obtained by using the SHG mode. Length of scale bars in the left column is valid for the entire row (reprinted with permission of the IUCr *Journal of Applied Crystallography* from Schubert *et al.*, 2015).

From the samples of thioredoxin, thaumatin and lysozyme, where an increase in the DDLS signal intensity was observed, a powder diffraction pattern could be recorded (Figure 3-7 A). Powder diffraction rings are visible up to a resolution of approximately 6 Å, which provide evidence that the samples contain well-ordered protein crystals.

An additional experiment has been performed to verify, that the formation of amorphous aggregates in the glucose isomerase sample is a consequence of the high precipitant concentration and not the protein preparation itself. For this a 50 % diluted precipitant solution was used and the outcome of the crystallization experiment demonstrates, that well-ordered needle-shaped protein crystals can be produced using the same protein batch (Figure 3-7).

3.4 Conclusion

The results obtained from experiments performed with the newly developed depolarized dynamic light scattering instrument demonstrate, that the translational and rotational decay time constants of gold nanoparticles can be measured and used to determine the size and shape of gold nanoparticles. Furthermore, by performing a set of measurements with isotropic polystyrene particles, the contribution of multiple scattering to the recorded depolarized signal was identified. A particle concentration dependent signal intensity threshold was determined and can be used to judge the bias of multiple scattering on the DDLS signal. By applying this threshold, several batch crystallization experiments could be performed and the formation of protein crystals could be followed. In particular, it could be shown that DDLS represents the first method which allows distinguishing between well-ordered crystalline particles and amorphous protein aggregates online and in solution. Additionally, the measurements are non-invasive and non-destructive. In comparison with other methods DDLS has a great potential in identifying and following the early stages of protein crystallization and the formation of nanocrystals in solution in real time.

CHAPTER 4

4. APPLICATIONS OF PROTEIN MICROCRYSTALS FOR SYNCHROTRON RADIATION

Although alternative methods like NMR and cryo-electron microscopy are available, X-ray crystallography remains the most extensively used method for structure determination of biological macromolecules. Over the last decades X-ray crystallography greatly helped to understand the chemical mechanisms underlying biological functions. The field has revolutionized within the last years upon the development of X-ray free electron lasers (FELs) and micro-focus crystallography beamlines at synchrotron radiation (SR) sources. Today, high-resolution diffraction patterns can be already obtained from well-ordered micro- and nanocrystals (Moukhametzianov *et al.*, 2008; Weckert, 2015; Neutze & Moffat, 2012; Spence *et al.*, 2012; Gruner & Lattman, 2015; Chapman *et al.*, 2011; Boutet *et al.*, 2012; Redecke *et al.*, 2013; Riekkel *et al.*, 2005; Smith *et al.*, 2012). In Chapter 2.1 and 2.2, new methods were presented that can be used to prepare protein nano- and microcrystals and to follow their nucleation and growth online. This chapter now presents potential applications of these microcrystalline samples for X-ray crystallography.

4.1 A multicrystal data collection approach for studying structural dynamics with millisecond temporal resolution

4.1.1 Introduction

Although the sample handling has been automated at many microfocus beamlines by using crystal mounting robots, mechanical stress is introduced to the crystals by sample transfer from the growth environment as well as buffer and temperature changes. Sample handling is especially difficult for fragile crystals and therefore several methods are proposed to minimize the extent of manual handling during this procedure (Cipriani *et al.*, 2012). Although diffraction data collection predominantly has been performed at cryogenic temperatures, cryo-cooling can hinder straightforward data collection at SR beamlines in some cases. Identification of the optimal composition of a cryo-protectant can be cumbersome and may have a detrimental effect on crystal quality and its diffraction properties (Axford *et al.*, 2012), but also diminished conformational diversity and different conformations were observed at cryogenic temperatures (Fraser *et al.*, 2011; Juers & Matthews, 2004; Rasmussen *et al.*, 1992; Tilton, JR *et al.*, 1992; Fraser *et al.*, 2009). These effects can be minimized by new data collection strategies at

room-temperature that additionally paved the road to follow biological reactions of proteins in a crystalline lattice by kinetic crystallography. To address this, new sample mounting systems for in-situ crystallography (McPherson, 2000) like microfluidic chips (Pinker *et al.*, 2013; Guha *et al.*, 2012; Perry *et al.*, 2013; Heymann *et al.*, 2014; Mueller *et al.*, 2015), low X-ray absorbing 96-well plates (Axford *et al.*, 2012; Kisselman *et al.*, 2011), capillaries (Stellato *et al.*, 2014) as well as other fixed targets (Coquelle *et al.*, 2015; Huang *et al.*, 2015) have been developed in order to record diffraction patterns from protein microcrystals at room-temperature.

Serial femtosecond crystallography (SFX) at free-electron laser radiation sources led to the development of a liquid jet technology to rapidly deliver microcrystals in suspension to the X-ray beam. However, this sample delivery approach may not be applicable for many crystalline samples, because of the relatively low hit rates as well as the high sample consumption (Redecke *et al.*, 2013; Schlichting, 2015; Martin-Garcia *et al.*, 2016). Therefore, a jet technology using viscous lipidic cubic phase (LCP) as sample delivery medium has been realized to reduce sample consumption (Weierstall *et al.*, 2014). In contrast to liquid jets, which usually have a diameter of 5 μm and smaller, viscous jets are much harder to focus and typically jet diameters of 25 μm and larger are used. Therefore, they result in an increased overall background to noise ratio, with additional background scattering from the media used to increase viscosity (Conrad *et al.*, 2015). In general, the experimental approaches aiming to perform serial crystallography with microcrystals at the more prevalent and readily accessible SR sources has been catalyzed upon the success of the serial femtosecond crystallography at FELs (Gati *et al.*, 2014; Stellato *et al.*, 2014; Botha *et al.*, 2015; Nogly *et al.*, 2015; Zander *et al.*, 2015; Roedig *et al.*, 2015; Roedig *et al.*, 2016).

Radiation damage can be either classified as specific or global and occurs at room-temperature to an even higher extent and thereby limits the number of diffraction patterns that can be recorded from one single protein crystal. Typically, the total X-ray dose is spread over the ensemble by collecting data from a large number of crystals. At a third generation SR source micro-focus beamline the X-ray flux, which is about $5 \cdot 10^{12}$ photons per second with an energy of 12 keV, is focused to an area of a few μm^2 . Consequently, the tolerated X-ray dose of each microcrystal at room-temperature is limited to a few milliseconds exposure time to avoid significant crystal damage. Therefore, the diffraction data from a succession of microcrystals is merged to acquire complete datasets. The success of the so far presented methods for room-temperature micro-crystallography is limited either by the crystal quality which suffers from the introduced mechanical stress or by the high sample consumption. In some of these methods an increased background signal reduces the signal to noise ratio (Panneels *et al.*, 2015; Liu *et al.*, 2013).

In this chapter a minimalistic fixed target approach and a corresponding data collection protocol is established that can be easily adapted at appropriate microfocus synchrotron beamlines. Additionally, the used protocol minimizes the crystal manipulation prior to data collection and extirpates the need for cryo-protectants, which in case no optimal cryo-protectant is found might reduce diffraction quality. For this purpose, a kapton foil sandwich for *in situ* crystallization is used which requires only one microliter of sample containing a few hundred microcrystals. The kapton sandwich is easily mounted onto a plastic frame and can be directly used for diffraction data collection from microcrystals at room-temperature. It is tested if high quality structural information and complete diffraction datasets can be recorded by this approach when merging diffraction data from multiple crystals within only a few minutes of beamtime. By choosing suitable X-ray beam attenuations or exposure times significant radiation damage can be avoided. Additionally, the analysis of the data collected as described here allows time-resolved observation of site specific radiation damage, structural changes and possibly enzymatic reactions. To address the question, thaumatin from *T. daniellii* containing eight intramolecular disulfide bonds is used as crystallization target, because it is a well characterized standard protein in radiation damage studies (Garman, 2010).

4.1.2 Material and Methods

4.1.2.1 Sample preparations

Lyophilized thaumatin (*T. daniellii*) (Sigma Aldrich) was purchased and used without further purification. It was dissolved to a final protein concentration of $34 \text{ mg} \cdot \text{mL}^{-1}$ in a buffer containing 50 mM Bis-Tris, pH 6.5. The obtained protein concentration was verified photometrically by using a Nanodrop (Thermo Scientific). For the precipitant and reservoir solution of the crystallization experiment 1.3 M sodium tartrate and 50 mM Tris, pH 6.8 was used. All solutions were prepared using ultrapure water, have been filtered through a $0.2 \mu\text{m}$ filter (Sartorius Stedim) and were centrifuged for 15 min at $16100 \times g$ before use.

4.1.2.2 Setup of the fixed target kapton sandwich

Thaumatin was crystallized in a vapor-diffusion hanging drop approach on a pre-greased Linbro plate. For the crystallization $2 \mu\text{L}$ reservoir solution and $2 \mu\text{L}$ protein solution were pipetted directly on an $8 \mu\text{m}$ thin kapton foil (American durafilm®) and the well was then sealed by a cover slip. To facilitate assembly, a small drop of water was placed on the glass lid to aid mounting of the foil. Since both Kapton foil and glass slide are hydrophilic the water droplet pulls foil and slide together through capillary force. Since the mounting droplet evaporates away over a few hours, separation of slide and

foil was trivial after crystallization. After a few hours multiple crystals with dimensions of 20 – 50 μm were grown. Directly at the synchrotron beamline the cover slip was lifted, excessive grease was removed and a second kapton foil layer was applied to seal the drop, resulting in a thin sample film between both kapton layers. The sample is automatically prevented from drying out by the remaining grease that seals the liquid between the kapton layers. The kapton-foil sandwich was either fixed on a frame in SBS format, in case a plate goniometer was used for data collection, or it was fixed on a small frame (1 cm x 1 cm) equipped with a base for an ordinary 3 axis goniometer by double sided adhesive tape. Both types of frames have been produced by using a 3D printer (Ultimaker). The design of the kapton foil sandwich and the process of sample mounting is illustrated in Figure 4-1.

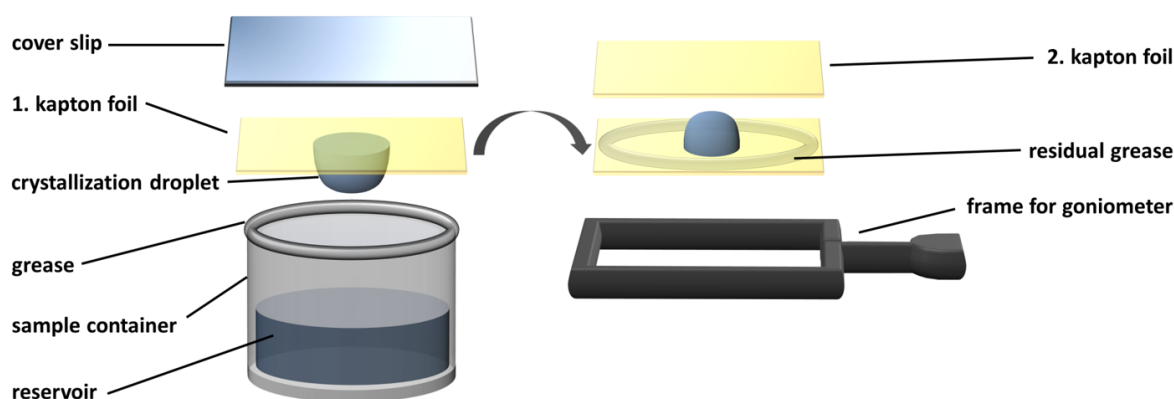


Figure 4-1: Schematic presentation of the experimental design of the kapton foil sandwich.

The thaumatin protein was crystallized in a hanging drop vapor diffusion approach directly on a kapton foil. After the crystals were grown the foil was lifted, sealed with a second kapton foil and mounted on a frame using a double-sided tape.

4.1.2.3 Data collection and evaluation

Diffraction data collection was performed on EMBL beamline P14 at the DESY storage ring PETRA III (Hamburg, Germany), using a micro focused X-ray beam with a size of 10 x 5 μm (FWHM of Gaussian profile) at 293 K. The energy of the X-rays was 12.8 keV and a flux density of $2.2 \cdot 10^{12}$ photons \cdot s $^{-1}$ in the non-attenuated beam were used. Diffraction pattern were recorded using a Pilatus 6M hybrid pixel detector and either a kappa goniometer or a plate goniometer were used to rotate the chip mounted on the frame. In each experiment 60 crystals of thaumatin were exposed to X-rays and 20 frames were recorded from each crystal within 800 ms in shutterless operation. An exposure time per image of 40 ms was used, limited by the maximum frame rate of the detector. The frame with the kapton foil was rotated by 1° during each exposure, resulting in a three-dimensional wedge rather than a thin slice of the reciprocal lattice. By this, the amount of crystals needed to record a complete data set was greatly reduced. Two separate data collections were performed from different set of crystals in order to determine the maximum tolerated X-ray dose. For the first data collection run a transmission of

50 % ($1.1 \cdot 10^{12}$ photons \cdot s⁻¹), while the transmission in the second run was further reduced to 5 % ($1.1 \cdot 10^{11}$ photons \cdot s⁻¹).

For the data evaluation each single diffraction pattern of thaumatin was individually processed using the program XDS (Kabsch, 2010). For each time interval (frame) individual HKL files from all crystals were created and scaled using the software XSCALE. The resulting correlation coefficients between datasets from the individual crystals during scaling were larger than 90 %, which indicates a high degree of isomorphism. The data processing was automated by using self-written bash scripts (Appendix). The phases for model building were obtained by Molecular Replacement (Vagin & Teplyakov, 2010) from the CCP4 suite (Winn *et al.*, 2011) using the 3D coordinates of the Protein Data Bank (PDB) entry 1LR2 (Charron *et al.*, 2002) as a search model. The structures were refined isotopically using Refmac5 (Murshudov *et al.*, 2011; Winn *et al.*, 2011), and COOT (Emsley *et al.*, 2010) for visual inspection of the final model. The highest resolution shell was determined by applying the conservative $\langle I/\sigma(I) \rangle > 2$ criteria. Solvent molecules were automatically added at the refinement process and checked to confirm chemically reasonable positions, where also difference electron density exceeded a 3σ level. All models were inspected for Ramachandran outliers. The coordinates for the structures, as well as the experimental diffraction amplitudes have been deposited at the Protein Databank (<http://www.rcsb.org>) with entry codes 5LH0, 5LH1 and 5LMI for the low dose run as well as 5LH3, 5LH5, 5LMH, 5LH6 and 5LH7 for the high dose run. The software RADDPOSE (Zeldin *et al.*, 2013) was used to calculate the applied X ray dose of each crystal at different time points.

4.1.2.4 Decay of diffraction power

The decay of diffraction power over time was determined by plotting the sum total of $I/\sigma(I)$ against time. For this, the intensity of all indexed reflections of a single time point, given by XDS (Kabsch, 2010), was taken from all exposed crystals. The diffraction power of each crystal was then normalized to the mean diffraction power of the first recorded image from all crystals (Owen *et al.*, 2014). By plotting the decay of diffraction power from all exposed crystals over time, a statistical distribution of the decay can be observed.

4.1.2.5 Crystal orientations

The distribution of the crystal lattice orientation in respect to the laboratory coordinate system was evaluated. For this the Euler angles were determined from the XDS orientation matrix, given in the XDS output file XPARM (Kabsch, 1988), using Matlab (2007a, The MathWorks). A detailed description of the calculation has been published by (Zarrine-Afsar *et al.*, 2012). The calculated Euler angles for the three rotation planes xy, xz and zy are grouped in classes of 10° and plotted in a histogram.

4.1.2.6 Site specific radiation damage

Structure-factor amplitude Fourier difference maps ($F_o - F_c$) between different time intervals of data sets from thaumatin were calculated as described (Coquelle *et al.*, 2015). For this, the final structural models of the first time point have been superimposed with later time points using the software package Phenix (Adams *et al.*, 2010). After superimposition difference maps were calculated in COOT (Emsley *et al.*, 2010) and displayed around all sulfur atoms. The difference density maps ($F_{O_{Frame\ x}} - F_{O_{Frame\ y}}$) were inspected at a contour level of 4σ to identify differences. (Schrödinger).

4.1.3 Results and Discussion

4.1.3.1 Diffraction data collection using the kapton foil sandwich approach

The aim of this study was to establish a protocol for X-ray diffraction data collection at room temperature with a millisecond temporal resolution. Great care was taken to design a reliable system as simple as possible, easy to fabricate, reproducible and compatible to be adapted to standard goniometers (Figure 4-2 A). Additionally, a plate goniometer can be used for rapid screening of multiple kapton foil sandwiches (Figure 4-2 B). The extent of crystal manipulation is minimized by crystallizing the protein crystals directly on the kapton foil in a hanging drop approach. Further, diffraction data collection at room-temperature does not require the addition of cryo-protectants and thereby helps to maintain the maximum intrinsic order in the crystal lattice. Additionally, measurements at room-temperature potentially allow for following dynamic processes and biological reactions.

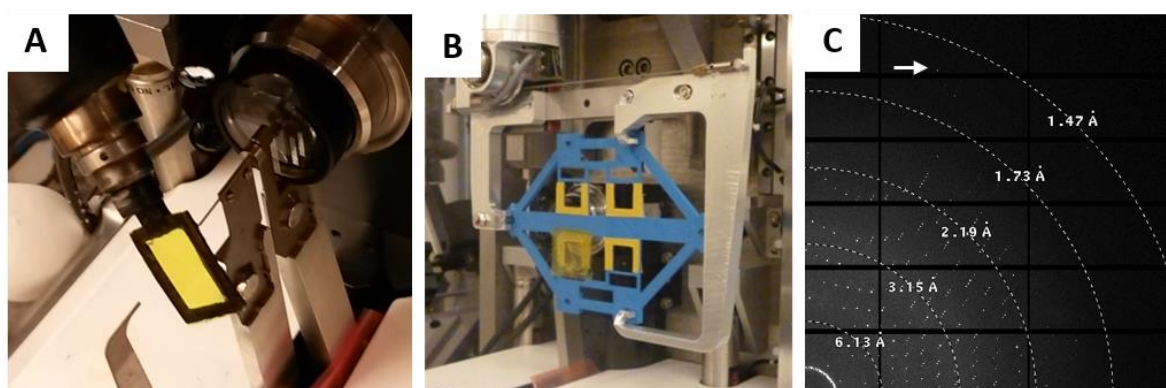


Figure 4-2: Diffraction data collection of thaumatin microcrystals in a kapton foil sandwich at a synchrotron X-ray radiation source.

[A] Individual kapton sandwiches can be mounted on a standard 3-axes goniometer at any synchrotron beamline or [B] on a plate goniometer for rapid screening of multiple kapton sandwiches. [C] Diffraction of thaumatin crystals in the kapton sandwich was recorded to a resolution of 1.6 \AA with a negligibly low background.

The exposed microcrystals of thaumatin in the kapton foil sandwich diffracted up to a resolution of 1.6 Å (Figure 4-2 C). It can be seen that the background contribution of the thin kapton double layer is minimal and mainly limited to a scattering at 33 Å ($2\theta \approx 1.7^\circ$) and at 11 Å ($2\theta \approx 5^\circ$) for a wavelength of 0.97 Å.

4.1.3.2 Data quality and statistics

In two separate experiments diffraction data was collected by exposing thaumatin crystals at low and at high X-ray photon flux, which corresponds to $1.1 \cdot 10^{12}$ photons \cdot s $^{-1}$ and $1.1 \cdot 10^{12}$ photons \cdot s $^{-1}$, respectively. In order to study possible radiation damage effects 20 consecutive exposures have been recorded from each crystal in the low-dose and high-dose run. Diffraction data from identical time intervals have been indexed and merged from 46 crystals, resulting in 20 complete data sets collected from 20 time intervals covering an exposure time range of 800 ms (Table 6 and Table 7). The total dose for the high dose and low dose runs after recording 20 consecutive diffraction patterns was calculated to be 2.32 MGy ($2.9 \text{ MGy} \cdot \text{s}^{-1}$) and 0.23 MGy ($0.29 \text{ MGy} \cdot \text{s}^{-1}$), respectively. For the low dose data only a minor decrease in the integrated high resolution Bragg reflection intensities have been observed. The maximum resolution decreased from 1.88 Å for the first data set (0 – 40 ms) to 1.96 Å for the last data set (760 – 800 ms). The statistics (Table 6) demonstrate that reliable and complete diffraction data sets without significant global radiation damage for each time interval have been recorded. In contrast, for the high dose experiments the comparison of the first (0-40 ms, total average dose of 0.12 MGy) to the last (760-800 ms, total average dose of 2.32 MGy) data set revealed, that the maximum resolution decreased from 1.65 Å to 2.28 Å, indicating significant global radiation damage (Table 7). Accordingly, also the $CC_{1/2}$ value dropped at lower resolution in the last time slice frame (760 – 800 ms) of the high dose experiment, compared to the first exposure (0 – 40 ms) (Figure 4-3).

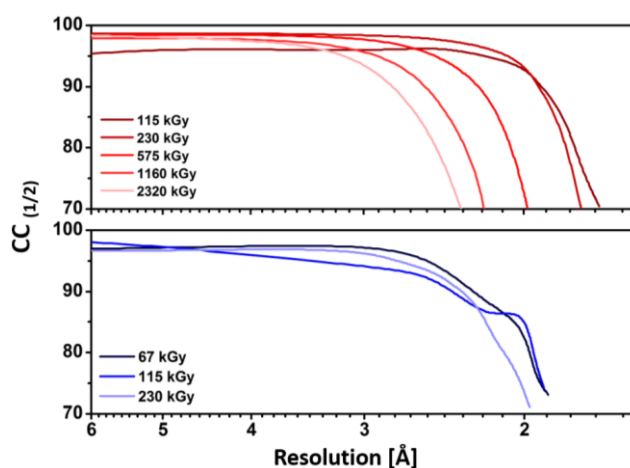


Figure 4-3: Data statistics from the room-temperature data collection of thaumatin microcrystals in the kapton foil sandwich.

$CC_{1/2}$ values (line plots) of the recorded diffraction data for low dose-rate (blue) and high dose-rate (red) experiment are plotted as a function of resolution.

Table 6: Data collection and refinement statistics for thaumatin with low dose X-ray photon flux at different time points

<i>Data collection statistics</i> ^a	1. Frame (0 – 40 ms)	10. Frame (360 – 400 ms)	20. Frame (760 – 800 ms)
Beamline	P14		
Wavelength [Å]	0.96863		
Space group	P4 ₁ 2 ₁ 2		
Unit cell: a = b, c [Å]	58.44, 151.58	58.43, 151.53	58.45, 151.59
Number of crystals	46		
Resolution [Å]	30 - 1.88 (1.95 – 1.88)	30 - 1.90 (1.97 – 1.90)	30 - 1.96 (2.02 – 1.95)
Total average dose [MGy]	0.01	0.12	0.23
Temperature [K]	296	296	296
R _{p.i.m.} ^b	9.0 (30.6)	8.8 (31.0)	8.3 (31.9)
Measured reflections	62822	63464	54468
Unique reflections	19955	19881	17759
Average I/σ(I)	5.3 (2.0)	6.3 (2.1)	6.0 (2.0)
Mn(I) half-set correlation CC _(1/2)	97.9 (71.5)	99.0 (78.2)	98.7 (72.9)
Completeness [%]	92.6 (93.6)	92.5 (93.0)	91.5 (92.8)
Redundancy	3.15	3.19	3.07
Refinement statistics			
Resolution range [Å]	30 - 1.88	30 - 1.90	30 - 1.96
R/ R _{free} [%]	18.8/23.9	18.1/22.8	18.9/22.1
Protein atoms	1550	1550	1550
Water molecules	51	44	33
Ligand molecules	20	20	20
Rms deviation			
Bond-length [Å]	0.020	0.021	0.021
Bond angle [°]	2.04	2.12	2.20
B factor [Å ²]			
Protein	22.6	25.0	28.1
Water	23.2	24.8	24.5
Ligand	20.4	47.1	59.2
Ramachandran plot analysis			
Most favored regions [%]	97.67	99.51	98.53
Allowed regions [%]	2.44	0.49	1.47
Generously allowed regions [%]	0.49	0.00	0.00
PDB entry	5LH0	5LH1	5LH2

a Values in parentheses are for the highest resolution shell.

$$b \text{ R p.i.m.} = \frac{\sum_{hkl} \sqrt{\frac{1}{n-1}} \sum_{i=1}^n |I_i(hkl) - \langle I(hkl) \rangle|}{\sum_{hkl} \sum_i I_i(hkl)}, \text{ where } I(hkl) \text{ is the mean intensity of the reflections } hkl, \sum_{hkl} \text{ is}$$

the sum over all reflections and \sum_i is the sum over i measurements of reflection hkl .

Table 7: Data collection and refinement statistics for thaumatin with high dose X-ray photon flux at different time points

	1. Frame (0 – 40 ms)	2. Frame (40 – 80 ms)	5. Frame (160 – 200 ms)	10. Frame (360 – 400 ms)	20. Frame (760 – 800 ms)
Data collection statistics^a					
Beamline	P14				
Wavelength [Å]	0.96863				
Space group	P4 ₁ 2 ₁ 2				
Unit cell: a = b, c [Å]	58.43, 151.58	58.42, 151.59	58.42, 151.59	58.49, 151.77	58.45, 151.62
Number of crystals:	46				
Resolution [Å]	30 - 1.65 (1.71 – 1.65)	30 – 1.69 (1.75 – 1.69)	30 – 1.96 (2.03 – 1.96)	30 - 2.15 (2.23 – 2.15)	30 - 2.28 (2.36 – 2.28)
Total average dose [MGy]	0.12	0.23	0.57	1.16	2.32
Temperature [K]	296	296	296	296	296
R p.i.m. ^b	8.2 (33.2)	6.8 (43.5)	8.5 (39.5)	10.2 (46.6)	11.6 (49.3)
Measured reflections	94713	90316	59357	41592	32153
Unique reflections	29947	28198	18364	13192	10726
Average I/σ(I)	5.6 (2.1)	7.1 (2.1)	5.8 (1.9)	6.1 (2.1)	5.9 (2.0)
Mn(I) half-set correlation CC _(1/2)	97.3 (70.7)	99.0 (71.2)	98.6 (65.0)	98.3 (66.9)	97.9 (61.7)
Completeness [%]	92.0 (92.0)	92.9 (93.8)	93.1 (93.4)	91.1 (90.6)	90.1 (90.1)
Redundancy	3.16	3.20	3.20	3.15	3.00
Refinement statistics					
Resolution range [Å]	30 - 1.65	30 – 1.69	30 – 1.96	30 - 2.15	30 - 2.28
R/ Rfree [%]	19.3/22.9	17.6/20.1	17.6/22.0	17.0/23.6	17.2/23.2
Protein atoms	1550	1550	1550	1550	1550
Water molecules	64	68	71	62	46
Ligand molecules	20	20	20	20	20
Rms deviation					
Bond-length [Å]	0.025	0.025	0.015	0.019	0.019
Bond angle [°]	2.29	2.63	1.68	2.08	2.07
B factor [Å ²]					
Protein	22.3	25.1	29.6	31.1	30.6
Water	26.0	21.3	50.2	35.2	34.3
Ligand	34.1	43.3	34.5	91.8	115.7
Ramachandran plot analysis					
Most favored regions [%]	98.53	98.53	97.07	97.56	97.07
Allowed regions [%]	1.47	1.47	2.44	2.44	2.93
Generously allowed regions [%]	0.00	0.00	0.49	0.00	0.00
PDB entry	5LH3	5LH5		5LH6	5LH7

a Values in parentheses are for the highest resolution shell.

$$b \text{ R p.i.m.} = \frac{\sum_{hkl} \sqrt{\frac{1}{n-1} \sum_{i=1}^n |I_i(hkl) - \langle I(hkl) \rangle|}}{\sum_{hkl} \sum_i I_i(hkl)}, \text{ where } I(hkl) \text{ is the mean intensity of the reflections } hkl, \sum_{hkl} \text{ is the sum over all reflections and } \sum_i \text{ is the sum over } i \text{ measurements of reflection } hkl.$$

4.1.3.3 Diffraction intensity decay

The intensity decay of the normalized diffraction power over time has been evaluated in order to visualize potential X-ray radiation damage during diffraction data collection. The total X-ray dose for the high dose-rate and low dose-rate runs after recording 20 consecutive diffraction pattern was calculated to be 2.32 MGy (dose-rate: 2.9 MGy s^{-1}) and 0.23 MGy (dose-rate: 0.29 MGy s^{-1}), respectively. The diffraction intensity decay for the high dose-rate and low dose-rate X-ray exposure experiments of thaumatin crystals is shown in Figure 4-4 A. The diffraction power in the high dose experiment already started to decrease after the first exposure and was below 50% after approximately 4 images (160 ms, $\approx 500 \text{ kGy dose}$).

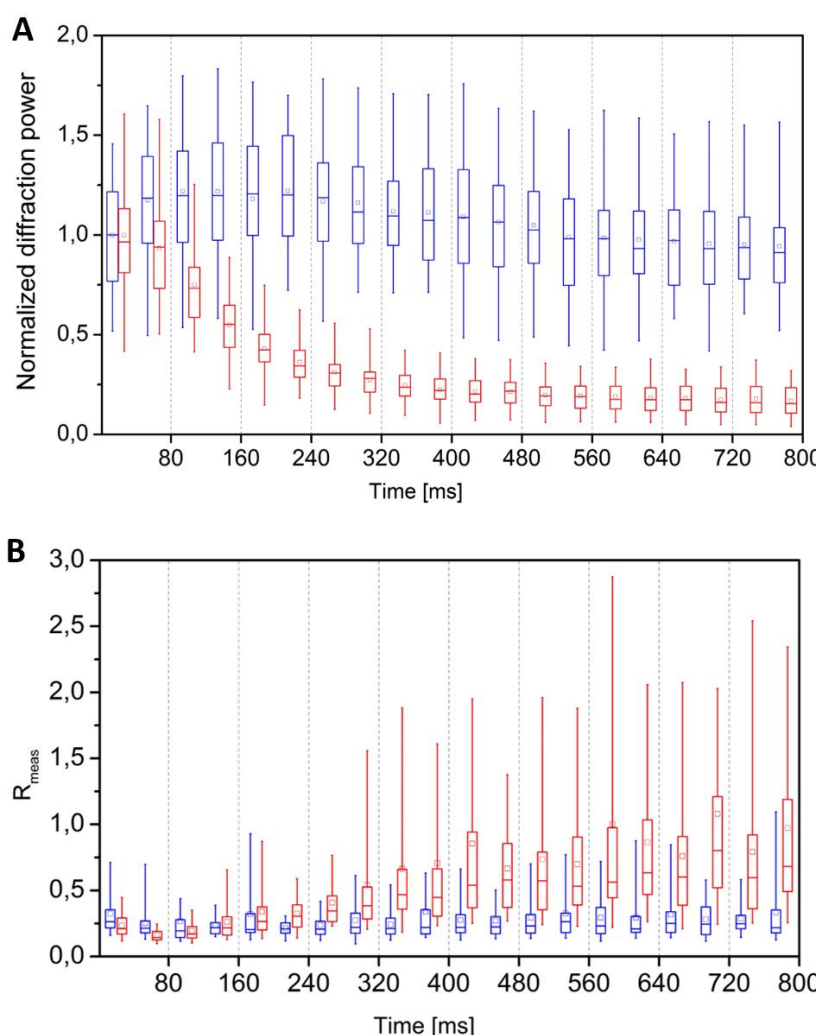


Figure 4-4: Effect of global X-ray radiation damage over time for the low dose-rate (blue) and high dose-rate (red) diffraction data.

[A] Normalized diffraction intensity decay of thaumatin microcrystals exposed to X-rays with low dose-rate (0.29 MGy s^{-1}) and high dose-rate (2.9 MGy s^{-1}) at room-temperature. [B] Evolution of the R_{meas} values of the individual crystals over time. The box plots in [A] and [B] with quartiles (mean, upper [75%], median [50%] and lower values [25%]) represent the decay of diffraction intensity and R_{meas} of all exposed crystals ($n = 46$).

In contrast, in the low dose experiment with a ten times attenuated X-ray beam, the diffraction power remained rather constant over the 20 recorded diffraction pattern within 800 ms. This is in good agreement with the expected maximum dose tolerance of 430 kGy for a single thaumatin crystal at room-temperature (Leal *et al.*, 2013), and also higher than the commonly assumed dose tolerance of 300 kGy for other protein crystals at room-temperature (Owen *et al.*, 2006; Nave & Garman, 2005). However, all refined models at selected time intervals presented in Table 6 and Table 7 reveal inconspicuous R factors/ R_{free} -values with constant R-values below 20 %. In general, no increase in the refinement R values is observed with respect to the X-ray dose absorbed by the crystals. The final electron density maps were of very good quality and all models have good stereochemistry.

4.1.3.4 Crystal orientations

In previously reported crystallography approaches on X-ray transparent fixed target setups, the orientation and arrangement of the protein crystals have been deliberately manipulated, in order to obtain a preferably random distribution of crystal orientations. To achieve this, in one example the hydrophobicity and roughness of a silicone mesh chip, covered with polyimide film, was increased by adding small glass beads to the sample (Zarrine-Afsar *et al.*, 2012). In the conducted experiments presented in this study no additional material was introduced between the kapton sandwich. Therefore, the unit cell orientation in respect to the laboratory coordinate system of all exposed crystals has been evaluated and the results demonstrate that a broad distribution of crystals orientations is obtained, regardless of the deliberate manipulation (Figure 4-5). It can be seen that for thaumatin crystals, which have a bipyramidal shape, no preferred orientation is observed in the xy-plane. Yet, the crystal orientation in the xy- and yz-planes is not fully unbiased from the kapton foil.

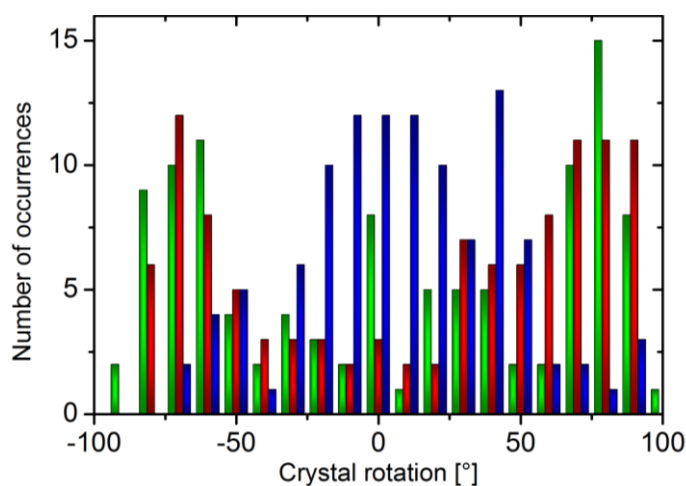


Figure 4-5: Distribution of crystal orientations of thaumatin in the kapton foil sandwich in respect to the laboratory coordinate system.

The bipyramidal thaumatin crystals were oriented in a broad range of rotations, covering nearly 180° in the xy-plane (green), xz-plane (red) and yz-plane (blue).

Nevertheless, a sufficiently good coverage of the reciprocal space is obtained from the broad range of crystal rotations. The recorded diffraction data resulted in complete datasets even if no care was taken while selecting exceptionally oriented crystals for X-ray exposure.

4.1.3.5 Time-resolved changes in electron density

The disulfide bridges in thaumatin are known to be sensitive to radiation damage (Garman, 2010; Yorke *et al.*, 2014). To visualize the effect of the site-specific component of the radiation damage on the electron density, structure-factor amplitude Fourier difference maps ($F_o - F_c$) have been calculated between datasets of the first recorded diffraction pattern and later time intervals. The temporal resolution in our experiment was limited to 40 ms, based on to the maximal frame rate of the detector. However, our experiment can potentially be combined by the additional use of Hadamard transform based X-ray probe-pulse sequences (Yorke *et al.*, 2014) easily. Thereby, the temporal resolution for tracking biological processes may be further reduced drastically to the low microsecond regime. The data statistics indicate that strong radiation damage has occurred in the high dose diffraction data sets, while only minor radiation damage has emerged in the low dose experiment. The site specific component of the radiation damage becomes visible by monitoring the difference density contoured at $\pm 4 \sigma$ in the proximity of all thaumatin sulfur atoms (Figure 4-6). Site specific damage was prominently observed for the sulfur atoms and a minor damage was observed for the oxygen atoms of some carboxyl groups.

As expected from the small decay of the diffraction intensity in the low dose run, no specific radiation damage was observed for the data set collected in the time interval between 360-400 ms (~ 0.12 MGy total average dose). Even for the data set, collected in the time interval between 760-800 ms (~ 0.23 MGy total average dose), only minor difference density could be detected around some of the disulfide bridges. This shows that the bonds between cysteines are still intact and only presumably start to become destabilized. This observation holds also true for data collected in the high dose run within the time interval of 40-80 ms exposure time, with the same total absorbed average dose of ~ 0.23 MGy. In contrast, more significant site specific damage could be observed already for the data set collected within 160-200 ms exposure time (~ 0.57 MGy total average dose) in the high dose experiment (Figure 4-6). All of the eight disulfide bonds reveal significant radiation damage. In contrast to our results, it was very recently reported, that for insulin no indications of site specific radiation damage up to the same absorbed dose of 0.57 MGy were observed (Roedig *et al.*, 2016). Roedig *et al.* concluded, that specific radiation damage – and here in particular cleavage of disulfide bridges – is less temperature dependent than global radiation damage and generally occurs only at higher doses. They assumed further, that disulfide bond breakage was not the preferred damage pathway at room

temperature, where global radiation damage to the lattice was clearly the dominating effect. However, our data do not support this hypothesis.

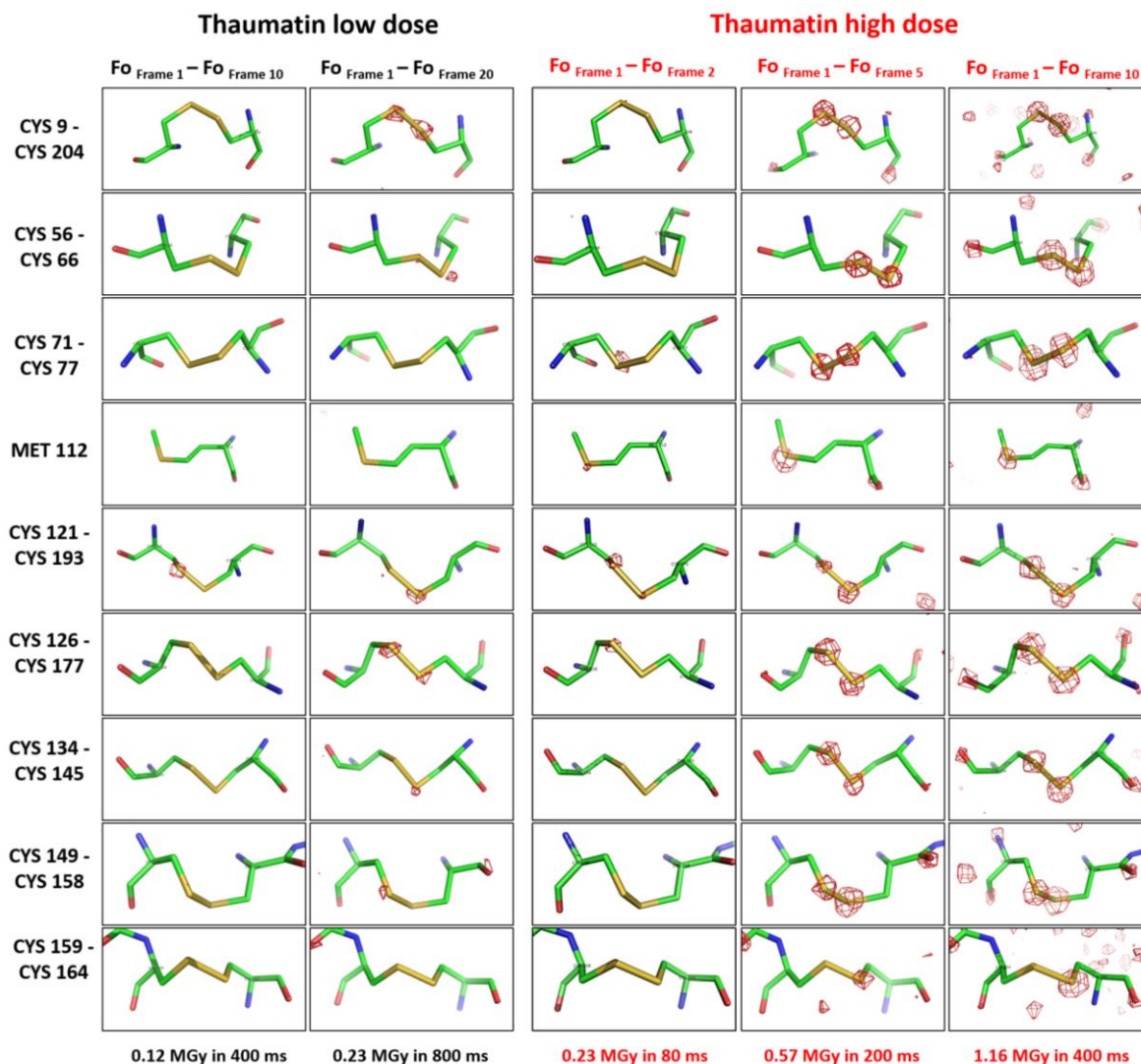


Figure 4-6: Time-resolved observation of specific radiation damage around all sulfur atoms of thaumatin over time.

Structure-factor amplitude Fourier difference ($F_o - F_o$) maps were calculated between different time points of X-ray exposure of the low dose (left side in black) and high dose (right side in red) experiments. The maps are displayed with red and green contours at 4σ indicating negative and positive density, respectively.

4.1.4 Conclusion

The data presented in this study demonstrate that complete diffraction datasets with a temporal resolution of 40 milliseconds can be recorded with the kapton foil approach at room-temperature by merging data from less than 50 protein microcrystals. Additionally, it was found that 20 diffraction datasets over a total X-ray exposure period of 800 milliseconds can be recorded with no significant site-specific or global radiation damage when using an attenuated X-ray beam, if the maximum dose

tolerance up to 400 kGy is considered. At doses higher than 550 kGy, beside the expected global radiation damage, we were able to observe dose-dependent site specific damage most prominently at the radiation sensitive disulfide bonds. The temporal resolution could be further reduced by using the newest generation of pixel detectors of the EIGER 4M series, where diffraction patterns can be recorded with a repetition rate of 750 Hz. In the resulting significantly shorter exposure time of 1.5 milliseconds the same number of photons (4.32×10^9) can be detected as in the presented low dose-rate experiments by using a non-attenuated X-ray beam. Thereby, the temporal resolution for tracing biological processes applying the presented kapton foil approach would be reduced to the low millisecond regime. Moreover, the protocol can be combined with the use of Hadamard transform based X-ray probe-pulse sequences (Yorke *et al.*, 2014). By this, the temporal resolution of diffraction experiments can be dramatically increased for cases when detectors with low frame rate or flux limited X-ray sources are available.

4.2 Multi-crystal radiation damage induced phasing

4.2.1 Introduction

A fundamental constraint in macromolecular crystallography is, that the phase information cannot be retrieved from the diffraction data mathematically - unless the diffraction is recorded to atomic resolution. To overcome this, the most commonly used method for obtaining phase information is called molecular replacement and requires the availability of already known highly homologue structures. For *de novo* phasing of diffraction data from proteins where no homolog is available, several different methods have been developed. In a method called isomorphous replacement (SIR: single isomorphous replacement; MIR: multiple isomorphous replacement), a small number of heavy atoms is introduced into the crystal artificially and two or more datasets are collected from the isomorphous *native* and *derivative* crystals. Typically selenomethionine is used to introduce atoms into the crystal which have a different scattering power than in the *native* crystal (Hendrickson *et al.*, 1990). Alternatively, in anomalous methods the wavelength of the X-rays is changed between the collection of different datasets and moved to the absorption edge of the introduced atoms (SAD: single-wavelength anomalous diffraction; MAD: multiple-wavelength anomalous diffraction) (Hendrickson & Teeter, 1981). In general, differences in the structure factors of both recorded datasets are used for the calculation of the phases. Over the last years, alternative methods have been developed to avoid the laborious derivatization of the *native* crystal. Among these are methods called free energy minimization (Castleden, 1992), iterated projections (Elser, 2003), three-beam X-ray diffraction (Weckert & Hümmel, 1997) and radiation damage induced phasing (RIP) (Ravelli *et al.*, 2003).

The fact that specific radiation damage can be used to phase diffraction data *de novo* has first been demonstrated by Ravelli *et al.* (2003). In many cases a combination of radiation damage and anomalous scattering has been used to obtain phase information (RIPAS) (Evans *et al.*, 2003; Banumathi *et al.*, 2004; Weiss *et al.*, 2004; Zwart *et al.*, 2004; Ravelli *et al.*, 2005). Different strategies for performing such experiments have been applied over the last years. In some studies, continuous data collection over a large oscillation range has been used for recording highly redundant data. Comparable with the SIR approach, the phase information is obtained by analyzing the intensity difference between a complete dataset merged from the first images and a complete dataset merged from the last images (Sanctis & Nanao, 2012; Schiltz *et al.*, 2004). In other cases, two low dose diffraction datasets are collected and interleaved with a high flux X-ray exposure to induce stronger radiation damage (Nanao *et al.*, 2005). In general, a labor-intensive derivatization of the isomorphous crystal in SIR experiments is rewarded by large differences in the structure factors between both datasets. In contrast, the intensity difference upon site specific radiation damage of X-ray susceptible

chemical groups in RIP experiments is small. Additionally, non-isomorphism is introduced in RIP experiments by global radiation damage, resulting in translation and rotation of molecules and minor changes of the unit cell parameters (Burmeister, 2000; Ravelli & McSweeney, 2000). This makes RIP significantly more difficult than SIR and requires a careful evaluation and improvement of the obtained substructures.

An alternative approach of inducing radiation damage for solving the phase problem of macromolecular diffraction data has been tested with UV-light and was called UV-RIP (Nanao & Ravelli, 2006). UV-light has the advantage that it does not ionize water molecules in the crystals and therefore does not induce reactive oxygen species, which are a major source of global radiation damage. Instead, UV-light mainly destabilizes or breaks disulfide and thioester bonds and affects the occupancy of bound heavy metal atoms in the protein (Sanctis *et al.*, 2011; Pereira *et al.*, 2013). Therefore, UV-light has some superior capacities for the introduction of site specific radiation damage compared to X-rays. Interestingly, it could be shown that UV-RIP experiments are also possible with the usage of high-power UV-LEDs, instead of using a sophisticated and cost intensive UV-laser setup (Sanctis *et al.*, 2016). In chapter 4.1 it has been shown, that the occurrence of specific radiation damage can be followed over time by evaluating data from multiple crystals which were exposed to X-rays at room-temperature. Up to now no experiment of radiation damage induced phasing from multi-crystal diffraction data has been published. One of the reasons is that the non-isomorphism is greatly increased when using multiple crystals, instead of evaluating the diffraction data from only one single crystal. Initial experiments on testing (UV)-RIP with a multi-crystal diffraction dataset have already been performed by Dr. Max Nanao (ESRF, France) and the results of continued experiments are presented in this chapter. Multiple microcrystals of thaumatin (*T. daniellii*) were exposed to X-rays as well as UV-light at cryogenic temperature in order to induce site-specific radiation damage which can be used for phasing.

4.2.2 Material and Methods

4.2.2.1 Sample preparation

The protein thaumatin from *T. daniellii* was purchased (Sigma-Aldrich, Germany). The lyophilized protein was dissolved in buffer containing 50 mM Bis-Tris pH 6.5 to a concentration of 40 mg · mL⁻¹, verified photometrically by using a Nanodrop (Thermo Scientific). Sodium tartrate was used as a precipitant with a concentration of 1.4 M. The protein and precipitant solutions were prepared using ultrapure water and have been filtered through a 0.2 µm filter (Sartorius Stedim). The thaumatin microcrystal samples were freshly prepared at the beamline a few hours before X-ray exposure. For the crystallization 2 µL protein solution were mixed with 2 µL precipitant in a hanging drop vapor

diffusion approach. Pure precipitant solution was used in the reservoir. In contrast to normal vapor diffusion experiments, the crystallization well was kept open to allow for rapid evaporation of water and a fast concentration of protein and precipitant in the crystallization droplet. By this, supersaturation is induced rapidly and many microcrystals start to grow. After the first microcrystals became visible the well was closed and sealed to avoid complete dehydration of the droplet.

4.2.2.2 Sample loading

A micro-patterned silicon chip mounted on a standard magnetic cap was used as a sample holder (Figure 4-7 A) as presented by Roedig *et al.* (Roedig *et al.*, 2015; Roedig *et al.*, 2016). The chip has a silicon membrane with dimensions of $1.5 \times 1.5 \text{ mm}^2$, a thickness of 10–30 μm and was provided by Dr. Anja Burkhardt (DESY, Germany). Prior sample loading, the crystallization well was opened and the droplet was supplemented with glycerol for cryoprotection to a final concentration of 25 % (v/v). 2 μL of the crystallization droplet containing crystals with a size around $5 \times 10 \times 5 \text{ }\mu\text{m}$ were then pipetted on the silicon chip. A wedge of filter paper was attached to the bottom side of the chip to soak off excessive mother liquor through the chip micro pores. This procedure was performed directly next to the goniometer and the chip was mounted in the cryostream immediately after removal of the liquid to avoid dehydration of the sample.

4.2.2.3 Data collection and evaluation

The radiation damage induced phasing experiments have been performed at the ID23-2 beamline at ESRF (Grenoble, France) in the framework of a collaborative project with Dr. Carolin Seuring (CFEL, Hamburg). For the RIP experiments, a mesh scan over a large area of the chip (approximately $250 \times 1100 \text{ }\mu\text{m}$, beam size $\approx 5 \times 10 \text{ }\mu\text{m}$) was performed in order to record diffraction data of a sufficient amount of randomly distributed thaumatin crystals for a complete diffraction dataset (Figure 4-7 B). At each scan position 100 diffraction patterns were recorded with an exposure time of 0.1 s and a chip rotation of 0.1 degrees per image at cryogenic temperature (100 K). The complete scan was performed for three times in the same grid position with an UV-light exposure between the second and third scan. This procedure allows assessing whether resulting radiation damage was induced by X-rays or by UV-light irradiation. By comparing X-ray radiation damage between the first and the second dataset (both before UV-light exposure) and the second and third dataset the contribution of X-ray damage to the total radiation damage after UV-light exposure can be evaluated. For the UV-light exposure, two high-power UV-LEDs with a wavelength of 245 nm were used and focused on a spot with a diameter of approximately 2 mm by ball lenses (Figure 4-7 C and D). The UV-light exposure unit is described and developed by Sanctis *et al.* (2016). The exposure time of the UV-light between the second and third recorded diffraction dataset was 25 minutes. XDS was used for indexing and processing of the 100

recorded images of each individual position of a thaumatin crystal hit (Kabsch, 2010). Process data from all crystals of each scan have been scaled using the software XSCALE. Further data processing and RIP phasing was performed with the help of Dr. Max Nanao (ESRF, France) and is described in detail in the result section (4.2.3).

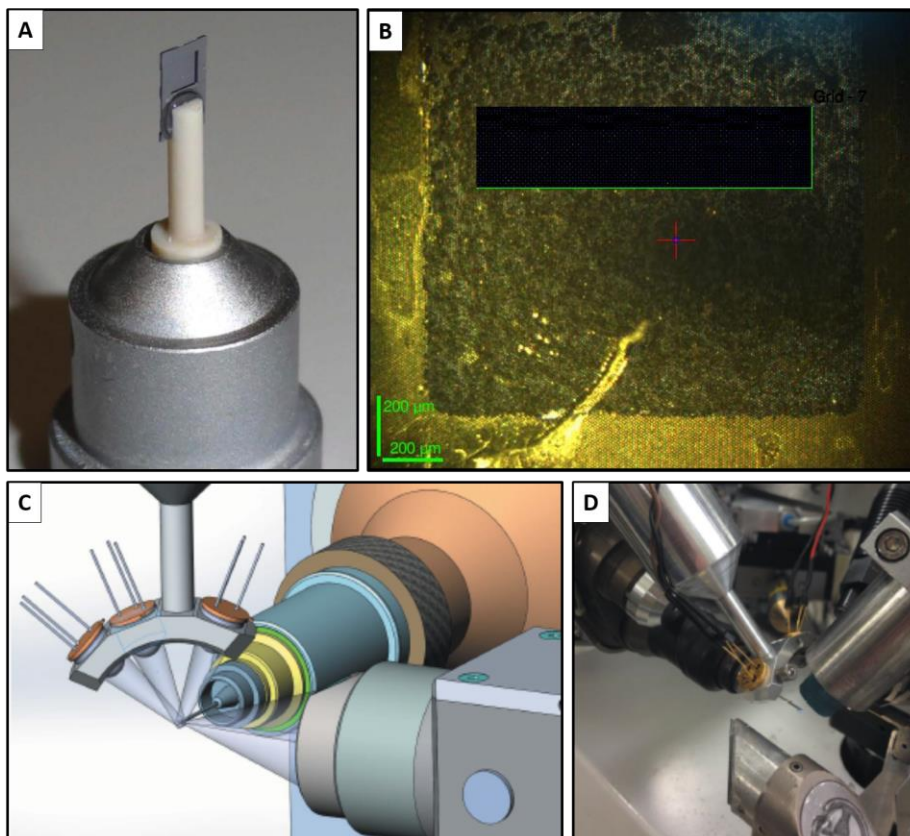


Figure 4-7: Sample mounting for UV-RIP experiments at ESRF beamline ID23-2.

[A] Micro-patterned silicon chip used for sample mounding. [B] Area of mesh scan on silicon chip loaded with thaumatin micro crystals. [C] Schematic presentation of the UV-exposure unit mounted next to the goniometer head. [D] Photographic presentation of the UV-exposure unit, the goniometer and cryo-stream. ([A] modified from Roedig *et al.*, 2015, [C] and [D] modified from Sanctis *et al.*, 2016).

4.2.3 Results and Discussion

4.2.3.1 Diffraction data collection and statistics

Up to now radiation damage induced phasing (RIP) has only been published for studies using diffraction data from a single protein crystal. The reason for this is, that the RIP signal is significantly reduced by non-isomorphism in multi-crystal diffraction datasets. It was now tested whether phase information can be obtained from small intensity differences induced by radiation damage in multi-crystal datasets of thaumatin microcrystals. For this, three mesh scans have been performed with a UV-light exposure between the second and third scan. The performed mesh scans on the silicon chip resulted in

diffraction data from 85 thaumatin crystals. The crystals had the space group $P4_12_12$ with unit cell parameters $a=b= 58.34$ and $c = 151.11$ Å and diffracted up to a resolution of 1.6 Å (Table 8).

By merging the data from all crystals of each scan, three complete diffraction datasets with high redundancy (>30) have been obtained. Data statistics from all three datasets are listed in Table 8. It can be seen that the I/σ value in the highest resolution shell did only drop slightly between the first dataset ($I/\sigma = 5.1$) and the second dataset ($I/\sigma = 4.6$), indicating only small global radiation damage by X-ray exposure. In contrast, a strong decrease in the I/σ value after UV-light exposure ($I/\sigma = 2.3$) is detected.

Table 8: Data collection statistics for the RIP diffraction data of thaumatin.

Data collection statistics^a			
Beamline	ID23-2		
Wavelength [Å]	0.873		
Space group	P41212		
Unit cell parameters: a = b, c [Å]	58.34, 151.11		
Resolution [Å]	54.5 - 1.6 (1.7 – 1.6)		
Photon flux [photons · s ⁻¹]	1.1 · 10 ¹²		
Beam size [µm]	5 x 10		
Temperature [K]	100		
Number of crystals	85		
Dataset	Before 1	Before 2	After-UV
R _{meas} ^b	31.3 (139.9)	18.8 (137.6)	25.2 (233.0)
Measured reflections	2153781	2149031	2153549
Unique reflections	65809	65807	65807
Average $I/\sigma(I)$	20.9 (5.1)	21.4 (4.6)	17.7 (2.3)
Mn(I) half-set correlation $CC_{(1/2)}$	99.9 (94.0)	99.9 (93.0)	99.9 (76.6)
Completeness [%]	100.0 (100.0)	100.0 (100.0)	100.0 (100.0)
Redundancy	32.7	32.6	32.7
X-ray dose [MGy]	2.36	4.72	7.09

a Values in parentheses are for the highest resolution shell.

b $R_{meas} = \frac{\sum_{hkl} \sqrt{\frac{n}{n-1}} \sum_{i=1}^n |I_i(hkl) - \langle I(hkl) \rangle|}{\sum_{hkl} \sum_i I_i(hkl)}$, where $I(hkl)$ is the mean intensity of the reflections hkl , \sum_{hkl} is the sum over all reflections and \sum_i is the sum over i measurements of reflection hkl .

4.2.4 Using radiation damage for phasing of a multi-crystal thaumatin dataset

Similar to the procedure in single isomorphous replacement (SIR), a scaling factor k needs to be applied to the second dataset after X-ray or UV-light induced radiation damage in order to put both onto a common scale. Consequently, the undamaged diffraction data corresponds to the *derivative* data and the damaged data to the *native* data according SIR terminology. Unfortunately, the k value has to be determined empirically and typically varies between 0.97 and 1.01. SHELXC was used for the preparation of the data for substructure determination and the calculation of the difference signal (ΔF) (Sheldrick, 2008). Both combinations have been tested, “before 1” - “before 2” for assessing the X-ray radiation damage, and “before 2” - “after-UV” for the UV-light induced radiation damage. Surprisingly, already between the first two datasets the model-phased $F_{\text{before 1}} - F_{\text{before 2}}$ map peak heights reached a maximum of 15σ , calculated by the software AnoDe (Thorn & Sheldrick, 2011). Therefore, SHELXD was used for substructure determination of the “before 1” - “before 2” data and the results are evaluated by plotting the correlation coefficient for all reflections (CC_{all}) against weak reflections (CC_{weak}) (Sheldrick, 2010). The presence of clusters with maximal CC_{all} versus CC_{weak} values gives a good estimate about correct solutions and is complemented with the best combined figure of merit (CFOM) value as described by Sanctis *et al.*, 2016. The results for various scaling factors (k) are comparatively shown in Figure 4-8. In general, several good solutions were found between scaling factors ranging from 0.98793 to 0.99897. One of the highest values is obtained for a scaling factor of 0.99207, as indicated by the black box in Figure 4-8. A detailed view of the CC_{all} vs CC_{weak} values of this scaling factor is shown in Figure 4-10 A and reveals, that the cluster is rather streaked out at high values than a well separated cluster is observed. In Figure 4-9, the obtained substructures are compared with the known substructures determined by peak-searching the model-phased $F_{\text{before 1}} - F_{\text{before 2}}$ map. Naturally, this can only be done because the thaumatin structure is already known. It is apparent, that for the structure factor 0.99207 the number of correct sites, representing S^Y atoms of some cysteines, which are present in the SHELXD solution and indicated by purple spheres, is maximal. It can be seen, that the substructures are incomplete because of negatively occupied sites (due to atom movements) and low-occupancy sites. To improve this, peak-searching, based on difference Fourier maps calculated from the initial substructures, and phase improvement is performed in five iterative rounds in SHELXE as introduced by (Nanao *et al.*, 2005). The difference in the obtained substructures between the first run and the last run is presented in Figure 4-10 B. Sites are indicated by the red arrows, which initially were not identified, but are present after the iterative optimization.

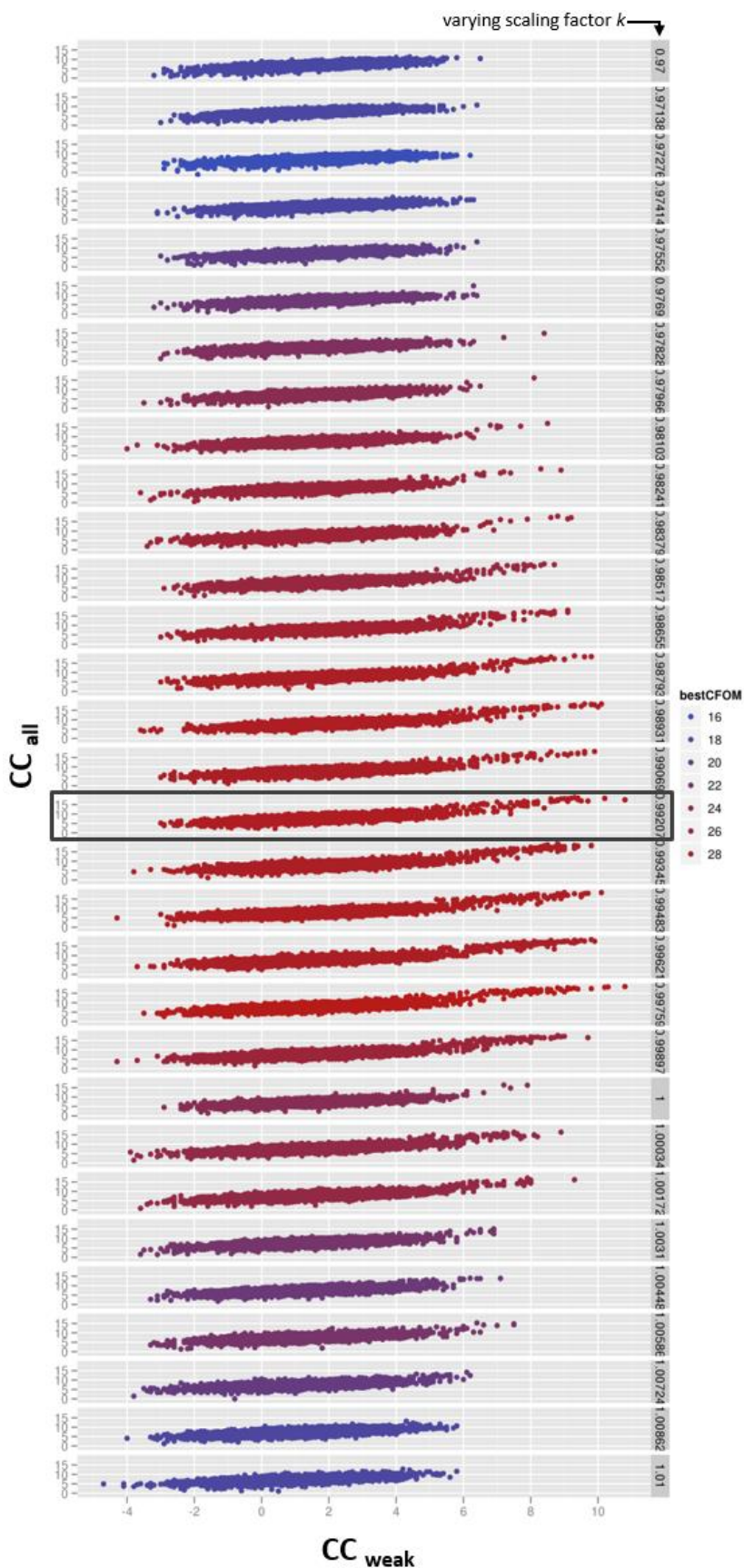


Figure 4-8: Results of substructure determination for various scaling factors by SHELXD.

[A] The correlation coefficient for all reflections (CC_{all}) is plotted against weak reflections (CC_{weak}) and additionally color coded by the best combined figure of merit (CFOM) to find the best substructures. The best results are obtained for a scaling factor of 0.99207 (black box).

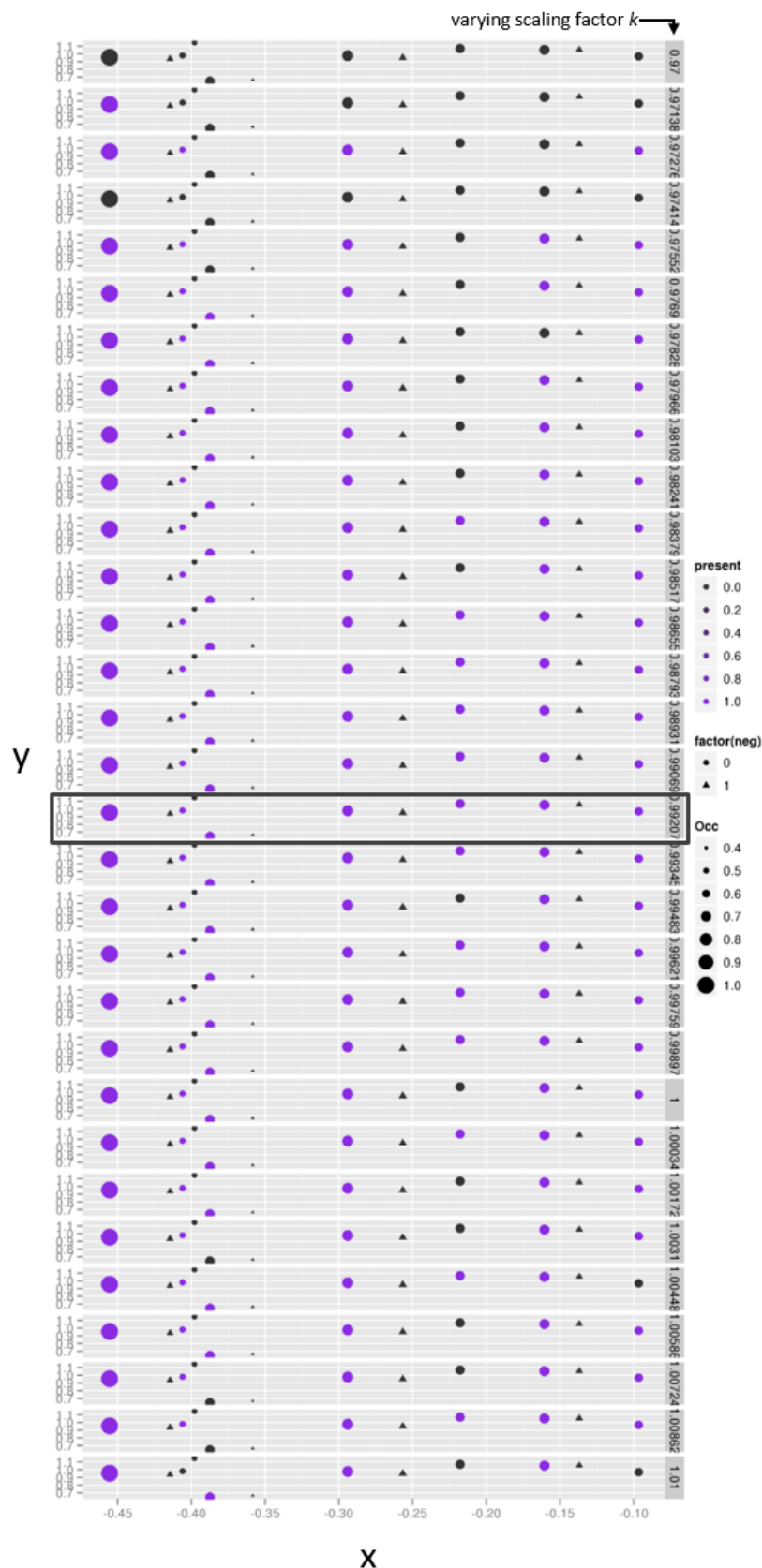


Figure 4-9: Comparison of the obtained substructures with known substructures from thaumatin data.
 [A] The Y and X position of the substructure in the unit cell is plotted and their intensity is shown by the size of the circle. Correctly found substructures by SHELXD are indicated by the purple color. Triangles present negative sites resulting in movement of atom positions upon X-ray exposure. The best results are obtained for a scaling factor of 0.99207 (black box).

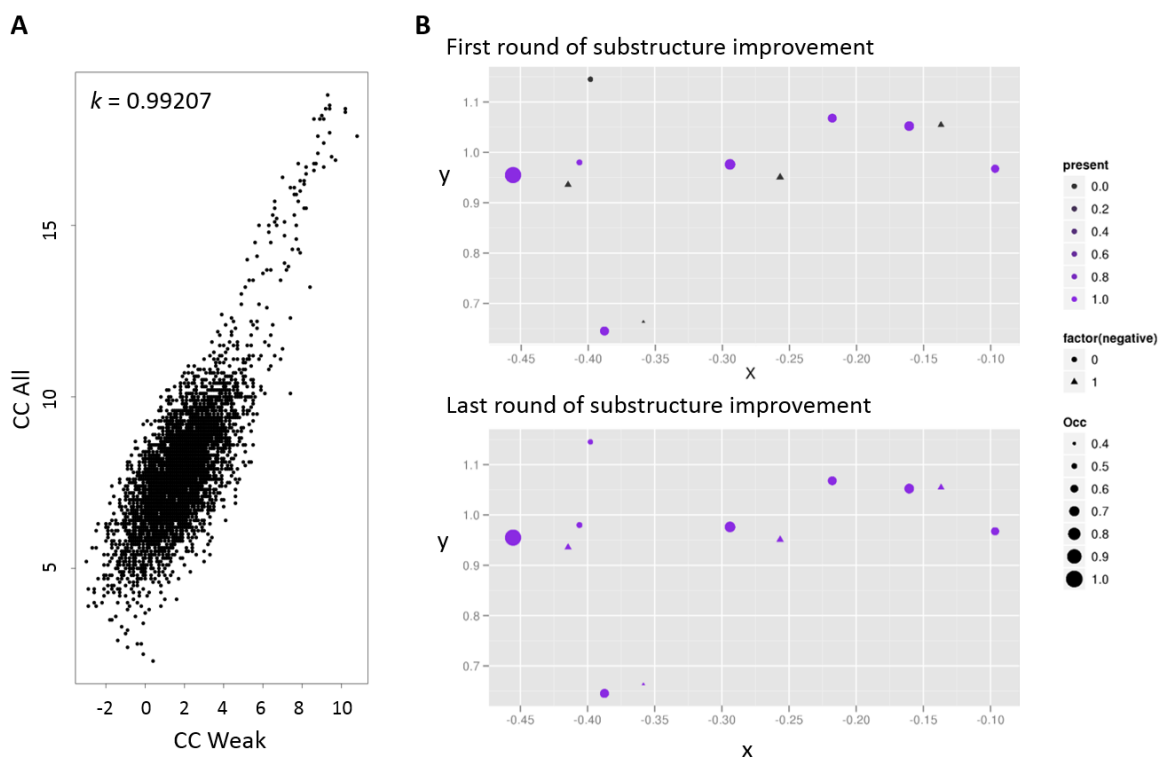


Figure 4-10: Substructure determination for best scaling factor.

[A] The best results are obtained for a scaling factor of 0.99207, as indicated by the pronounced cluster streaking towards high CC values. [B] The obtained substructures for the scaling factor 0.99207 are iteratively improved by SHELXE. Substructures, which have not been identified in the first round, but are present after the last round of improvement by difference Fourier analysis are indicated by the red arrows. Triangles present negative sites resulting in movement of atom positions upon X-ray exposure.

After substructure improvement, difference Fourier peaks are visually inspected by superimposing the reference thaumatin structure with the map. Difference density around all sulfur atoms of thaumatin contoured with 8σ is clearly visible and shown in Figure 4-11. Additionally, density is visible for other radiation sensitive sites as carboxyl groups or ordered waters.

Based on this, chain tracing and model building was performed using ARP/wARP, providing the thaumatin amino acid sequence as input (Langer *et al.*, 2008). Refinement of the obtained model was performed using REFMAC (Murshudov *et al.*, 2011) and COOT (Emsley *et al.*, 2010) and resulted in an R factor of 15.8 and R_{free} value of 19.0. Refinement statistics are summarized in Table 9 and demonstrate excellent geometry of the obtained structural model. The $F_o - F_c$ electron density map of a small region of the thaumatin structural model, obtained by X-ray radiation damage induced phasing of a multi-microcrystal dataset, is shown in Figure 4-12. A strong artificial contribution of the radiation damage in the structural model of thaumatin from the “before 1” dataset is possible by reducing the number of diffraction pattern included in the dataset for the final model. By merging the data of the first 10 diffraction pattern (representing a total oscillation range of 1 degree) from all 85 exposed microcrystals, a complete dataset with lower redundancy is obtained. The obtained structural model

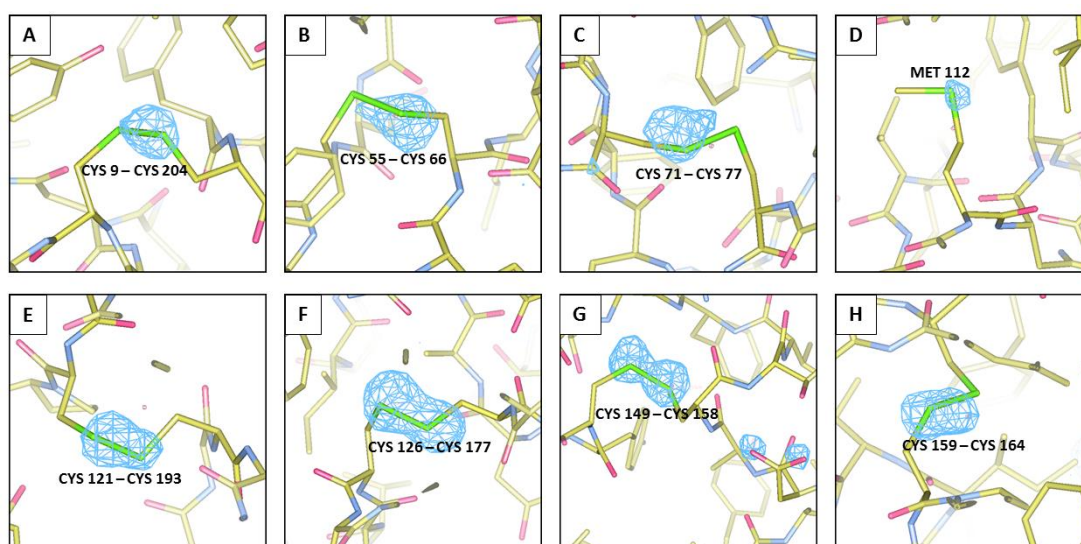


Figure 4-11: Difference Fourier peaks between before 1 and before 2 data around all sulfur atoms of thaumatin.

[A]-[H] Difference density is shown as blue meshes contoured at 8σ , after iterative phase improvement with SHELXE.

of thaumatin from the X-ray RIP phasing can now be used as a search model for molecular replacement. By this, a structural model of thaumatin is obtained from microcrystals which were exposed to a total X-ray dose of 236 kGy, according to RADDOSSE. The same radiation damage induced phasing approach could also be successfully used for the “before 2” – “after-UV” data. However, it is not possible to derive additional information from this, because the contribution of X-ray damage to the total induced radiation damage after UV-light exposure cannot be determined and separated.

Table 9: Refinement statistics of thaumatin RIP data.

Refinement statistics	
Resolution range [Å]	54.5 - 1.6
R/ R _{free} [%]	15.8/19.0
Protein atoms	2959
Water molecules	268
Rms deviation	
Bond-length [Å]	0.0317
Bond angle [°]	2.751
B factor [Å ²]	
Protein	15.03
Water	29.25
Ramachandran plot analysis	
Most favored regions [%]	99.02
Allowed regions [%]	0.98
Generously allowed regions [%]	0.0

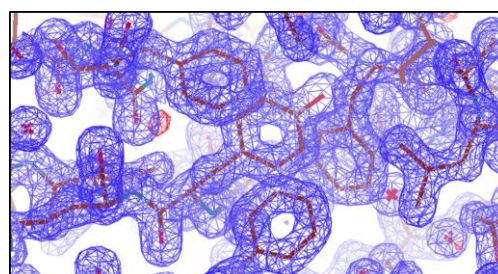


Figure 4-12: Fo-Fc electron density of the structural model of Thaumatin phased by X-ray RIP using multi-crystal diffraction data (contoured at 2 r.m.s.d).

Consequently, for phasing diffraction data by UV-light induced radiation damage rather than X-ray damage, a lower X-ray dose has to be used when exposing microcrystals. This can be done by reducing the exposure time, the photon flux, or by scanning a larger grid on the chip with fewer frames per crystal. It would also be possible to use a larger oscillation increment per frame to obtain the same high redundancy from fewer diffraction pattern.

4.2.5 Conclusions

The presented data clearly show that X-ray induced radiation damage can successfully be used for phasing of a multi-microcrystal diffraction dataset collected at cryogenic temperatures. This is particularly interesting, because it was not known if the non-isomorphism from multiple crystals would diminish the differences in structure factors induced by radiation damage. It turned out, that between the first two diffraction datasets the X-ray induced radiation damage was already sufficient for phasing. Thus, an evaluation of the UV-light induced radiation damage is not possible, because the contribution of X-ray damage cannot be determined and separated.

Additionally, it should be noted that also the multi-crystal diffraction data collected at room-temperature in the kapton sandwich, as presented in section 4.1, was tested by this approach. However, the RIP signal obtained from this data could not be used successfully for phasing. A probable explanation for this is, that radiation damage propagates rather quickly at room-temperature, resulting in increased global damage which cannot be used for phasing. It needs to further elucidated if UV-RIP experiments conducted at X-ray free electron lasers can overcome this limitation.

SECTION B

AMINOPEPTIDASE P FROM *P. FALCIPARUM*

5. STRUCTURAL CHARACTERIZATION OF *PLASMODIUM FALCIPARUM* APP

5.1 Introduction

Malaria remains a human disease of global burden with 214 million estimated new cases of human infections and 438 000 malaria deaths (estimations between 236 000–635 000) in 2015 (World Health Organization (WHO), 2015). The clinical manifestation of malaria is caused by replication of a protozoan parasite belonging to the genus *Plasmodium* within host erythrocytes. Five *Plasmodium* species are known, whereas the most severe form of malaria, malaria tropica, is caused by *P. falciparum* (Snow *et al.*, 2005). Although a range of antimalarial drugs are on the market, strains of *P. falciparum* that are resistant to drugs like chloroquine and Sulfadoxine-Pyrimethamine are widely distributed (Uhlemann & Krishna, 2005; Mugittu *et al.*, 2004; Mita & Tanabe, 2012; Marks *et al.*, 2005). Also for the drugs Malarone, which is a combination of Atovaquone and Proguanil, as well as Artemisinin resistant strains are emerging (Fivelman *et al.*, 2002; Witkowski *et al.*, 2013; Dondorp *et al.*, 2009) and consequently, new antimalarial drugs need to be discovered urgently.

In the asexual blood stage *P. falciparum* digests hemoglobin in the food vacuole and requires this for proliferation (Rosenthal *et al.*, 1988). The parasite takes up to 75 % of the host hemoglobin in the erythrocytes by endocytosis and catabolizes it in order to acquire a source of free amino acids for protein biosynthesis (Krugliak *et al.*, 2002; Loria *et al.*, 1999; Goldberg & Slater, 1992). The pathway of hemoglobin catabolism is essential for the replication of the parasite and thus of great interest in anti-malarial drug development. Hemoglobin is first cleaved by endopeptidases of various catalytic mechanisms and divers specificity (plasmepsin I, II, and IV; falcipain-2, -2b, and -3 and histoaspartic protease) before the globin peptides are cleaved to oligopeptides by the metalloprotease falcilysin (Gluzman *et al.*, 1994; Shenai *et al.*, 2000; Goldberg, 2005; Rosenthal, 2002; Eggleston *et al.*, 1999).

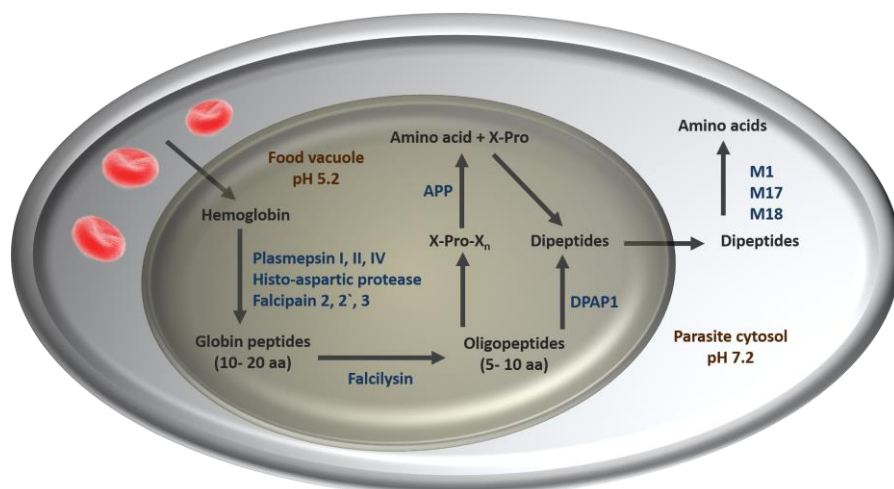


Figure 5-1: Simplified schematic of the hemoglobin degradation pathway in *P. falciparum*.

The oligopeptides are then hydrolyzed to dipeptides by a dipeptidyl Aminopeptidase (Klemba *et al.*, 2004) and subsequently the dipeptides are cleaved to individual amino acids by aminopeptidases M1 and M17 (Kolakovich *et al.*, 1997).

However, peptides containing a X-Pro sequence do not bind in the active sites of aminopeptidases with broad specificity, due to the cyclic structure of proline. Because human hemoglobin contains seven proline residues a third aminopeptidase, which is called Aminopeptidase P (APP), plays an important role in the hemoglobin degradation. APP possesses a high specificity for a substrate with proline in P1' position and appears to be the only enzyme of *Plasmodium* that is capable to hydrolyze an N-terminal amino acid from X-Pro-containing peptides (Cunningham & O'Connor, 1997; Ragheb *et al.*, 2009).

APP is a metallopeptidase whose activity is strongly dependent on manganese (Ragheb *et al.*, 2009). For human APP1 and *E. coli* APP structural studies have revealed a di-Mn²⁺-cluster (Graham *et al.*, 2004; Li *et al.*, 2008), while for *C. elegans* APP a di-Zn²⁺-cluster was identified (Iyer *et al.*, 2015). The structurally known homologues with the highest sequence identity to *P. falciparum* APP have a three-domain structure and form a dimer as catalytically active form. As a distinguishing feature, *P. falciparum* APP contains a non-conserved N-terminal extension of 128 amino acids. Based on protein isolations from parasite extracts it is speculated, that APP is translated and directed to the food vacuole as a full length variant and then processed to its mature form in this compartment (Ragheb *et al.*, 2009).

In this chapter it is intended to structurally characterize the key enzyme APP from *P. falciparum*. A protocol for the protein expression and purification is established and the protein is further analyzed by CD-spectroscopy, Dynamic Light Scattering and X-ray crystallography.

5.2 Material and Methods

5.2.1 Cloning and expression of APP

The sequence of the Aminopeptidase P (APP) from *Plasmodium falciparum* was obtained in a IBA3+ plasmid from Prof. Dr. Carsten Wrenger (University of Sao Paulo, Brazil). Based on information from nucleotide sequence homology (Blastn, Altschul *et al.*, 1990), structural homology modelling (ITASSER and PHYRE²) and crystallizability prediction (XtalPred-RF) a truncated version of the APP protein was designed. The APP was truncated by 128 amino acids (384 bp) N-terminally and by 6 amino acids (18 bp) C-terminally, resulting in a construct with 643 amino acids (1929 bp). Additionally, the presence of rare codons for *E. coli* in the APP coding nucleotide sequence was analyzed. The sequence has been optimized in order to avoid the occurrence of these rare codons and the gene was synthesized by the company GenScript (Piscataway, USA). The codon optimized sequence was C-terminally extended by

a 6x His tag followed by a TEV cleavage site (27 amino acids, 81 bp), to allow for protease cleavage of the affinity tag, and contained EcoR1 and BamH1 restriction sites. The synthesized gene sequence had a complete length of 2010 nucleotides (670 amino acids) and was obtained subcloned in a pUC57 bacterial expression vector. The protein sequence of full-length APP as well as an overview of the truncated regions is listed in the Appendix.

The APP gene was then recloned in a IBA3+ bacterial expression vector and transformed into *E. coli* BLR(DE3) cells from Novagen (Merck, Darmstadt, Germany). A single colony of the cells, grown on a LB-agar plate with tetracycline ($17 \mu\text{g} \cdot \text{mL}^{-1}$) and ampicillin ($100 \mu\text{g} \cdot \text{mL}^{-1}$) over night at 37°C , was used to inoculate a 20 ml preculture with LB-medium containing the same antibiotics. The preculture was grown for 16 hours at 37°C at 180 rpm and subsequently used to inoculate the expression culture (1L LB-medium at 37°C und 180 rpm, supplemented with the same antibiotics selection and 1 mM MnCl_2). Gene expression was induced at an OD_{600} of 0.6-0.8 by addition of 1 mM IPTG, the temperature was reduced to 20°C and the expression was conducted for 16 hours. The cells were harvested after 16 hours by centrifugation at $4000 \times g$ for 20 minutes at 4°C and the cell pellet was stored at -20°C until usage.

5.2.2 APP purification protocol

For the purification of APP the cell pellet was resuspended in lysis buffer (50 mM Tris, pH 8.0, 150 mM NaCl, 1 mM MnCl_2 and 1 mM PMSF), supplemented with a spatula tip lysozyme (*Gallus gallus*, Sigma Aldrich, Germany). The cells were disrupted by sonication on ice for three minutes each (30 % duty cycle) and the procedure was repeated three times. The lysate was centrifuged at 4°C at $17\,000 \times g$ for 40 minutes to remove cell debris and APP was obtained in the supernatant. Metal ion affinity chromatography using a Ni-NTA column with gravity flow was applied as a first purification step. The column was equilibrated with lysis buffer and the cleared lysate was incubated with the matrix for 30 to 60 minutes at 4°C . The flow-through was collected and the resin was washed three times with 20 ml lysis buffer supplemented with 20 mM imidazole, 1 mM ATP and 1 mM MgCl_2 to remove unspecifically bound protein. The protein was eluted in several steps with 10 ml elution buffer containing 50 mM Tris, pH 8.0, 150 mM NaCl, 100 mM Imidazole, 1 mM MnCl_2 . The elution fractions were analyzed by SDS-PAGE and suitable fractions were combined. The combined fraction was dialyzed over night against imidazole free elution buffer at 4°C . Subsequently, the sample was concentrated to a volume of 5 ml and a second purification step using a size exclusion chromatography (SEC) was applied and operated by an ÄKTA FPLC system (ÄKTA Purifier P-901; GE Healthcare, UK). For the SEC a Hi-Load 16/60 Superdex 200 (GE Healthcare, UK) column was used at 4°C and equilibrated with APP-buffer (50 mM Tris, pH 8.0, 150 mM NaCl and 1 mM MnCl_2). SEC was used to separate the catalytically active

APP dimer from larger oligomers and aggregates. Finally, the purified APP was concentrated using a Amicon centrifugal filter concentrator (Merck Millipore, Schwalbach, Germany) with an MWCO = 10 kDa. Native page was performed according to the manufacture protocol by using a kit containing precasted gradient gels and buffer solutions (#43204.01, SERVA Electrophoresis, Heidelberg, Germany)

5.2.3 DLS measurements

Dynamic light scattering measurements with a SpectroLight 300 cuvette instrument (XtalConcepts, Hamburg, Germany) were performed to determine the hydrodynamic radius of the APP protein in solution. The laser has an output power of 100 mW, a wavelength of 660 nm and the scattered light was detected at a scattering angle of 90°. The autocorrelator (XtalConcepts) of the instrument covers a sample time range from 0.4 μ s to 30 s. Samples were measured at 20 °C and each measurement was performed for 30 s and repeated 20 times in order to get highly reliable results. The refractive index of water ($n = 1.33$) and a viscosity of 1.016 cP were used for all calculations. The decay time constants of the scattering signal are derived from the autocorrelation function by using the CONTIN algorithm (Provencher, 1982). The hydrodynamic radius (R_H) of the particles in solution was calculated from the decay time constant. The molecular weight of the particles was approximated applying the formula

$$R_H = \left(\frac{3M \cdot (V_S + h)}{4\pi \cdot N_A} \right)^{\frac{1}{3}}, \quad (4)$$

with M being the molecular weight, V_S the specific particle volume, h the hydration volume and N_A the Avogadro constant.

5.2.4 CD spectroscopy

Circular Dichroism (CD) spectroscopy measurements were performed using a J-815 CD-Spectrometer (Jasco, Gross-Umstadt, Germany). Prior recording of far-UV spectra the APP sample was dialyzed against a buffer containing 10 mM Tris, pH 8.0. Subsequently, the sample was diluted 20 times with ultrapure water, resulting a protein concentration of 2 μ M. 100 μ L of this sample were filled into a quartz glass cuvette with 1 mm pathlength (Hellma-Analytiscs, Müllheim, Germany). 15 individual spectra were recorded and merged from a wavelength range of 190 – 260 nm with a data pitch of 0.1 nm a bandwidth of 1 nm and a scanning speed of 50 nm \cdot min⁻¹. The spectra were cut at a wavelength of 195 nm, because the absorption exceeded 3 at lower wavelength. The spectra were evaluated in the Software *Spectra Manager* from Jasco to estimate the secondary structure content of APP.

5.2.5 Crystallization

For the crystallization of the purified APP (5.2.2) the protein solution was concentrated to a range of 7 to 11 mg · mL⁻¹ by using a Amicon centrifugal filter concentrator (Merck Millipore, Schwalbach, Germany) with an MWCO =10 kDa. Before crystallization trials have been conducted the protein solution was centrifuged for 30 minutes at 16100 x g and DLS (5.2.3) was used to determine the particle size distribution of the particles in solution. Crystallization trials were performed as vapor diffusion method in a sitting drop approach and seeding experiments were set up in microbatch mode under oil.

For the vapor diffusion experiments 96-well SWISSCI MRC2 plates were used (Hampton Research, Aliso Viejo, USA) and pipetted by a Honeybee 961 pipetting robot (Genomic Solutions, Huntingdon, UK). 45 µL of precipitant were used in the reservoir well and 400 nl protein were mixed with 400 nl precipitant on the sitting shelf. The commercial crystallization screens PACT premier (MD1-36), JCSG-plus (MD1-40), Morpheus (MD1-47), Stura FootPrint (MD1-20) (all Molecular Dimensions, Suffolk, UK) and AmSO₄ (Quiagen) were tested. The plates were sealed, stored at 289 K and regularly inspected for crystal formation using a microscope.

The microbatch experiments have been set up by using the Oryx4 pipetting robot (Douglas Instruments, Hungerford, UK). Hydrophobic vapor batch plates (VBATCH 1/1 PHO, Douglas Instruments, Hungerford, UK) were set up using a 3-bore tip with 300 nl protein, 200 nl reservoir and 100 nl seed stock. The plate was flooded with Al's oil, which is a 50:50 (v/v) mixture of Paraffin Oil and Silicon Oil (Hampton Research, Aliso Viejo, USA), to allow for a slow solvent evaporation. Seed stocks have been prepared by using seed-beads (Jena Bioscience, Jena, Germany) according manufacturer protocol.

5.2.6 Data collection, evaluation, phasing and refinement

Before diffraction data collection the crystallization droplet was supplemented with 25 % glycerol for cryo protection. The crystals in nylon loops were mounted on the kappa-goniostat of the EMBL P14 beamline at the synchrotron source PETRA III in Hamburg, Germany. The protein crystals have been exposed to an X-ray beam with an approximate flux of $1.2 \cdot 10^{11}$ photons · s⁻¹. The beam size was 90 by 124 µm, adjusted to the crystal size in order to obtain an optimal signal to noise ratio. The exposure time of each diffraction pattern was 40 milliseconds and the crystal was rotated by 180 ° in 0.05° increments.

The diffraction data was integrated and processed by the programs XDS (Kabsch, 2010) and SCALA (Evans, 2006). Structure solution and refinement was done by using programs from the CCP4 suite (Winn *et al.*, 2011). Molecular replacement was performed with the PDB entry 3CTZ as a search model,

which has a sequence identity of 35 %, to obtain phase information by using the software MOLREP (Vagin & Teplyakov, 2010). Refinement was done with REFMAC5 (Murshudov *et al.*, 2011) and COOT (Emsley *et al.*, 2010) was used for visual inspection and improvement of the structural model. Figures were drawn by using the program PYMOL (DeLano Scientific, San Carlos, USA).

5.3 Results and Discussion

5.3.1 Recombinant expression, purification and characterization

A sequence homology analysis of *P. falciparum* APP with homologue proteins by using the Basic Local Alignment Search Tool (BLAST) (Altschul *et al.*, 1990) revealed, that the first 128 amino acids from the N-terminus are not conserved and absent in any homologue protein. The highest sequence identity of truncated APP to a protein with known structure was identified from *Homo sapiens* APP (35 %) (pdb code: 3CTZ) followed by APP from *Caenorhabditis elegans* (30 %), determined by the modeling and prediction server Phyre² (Kelley *et al.*, 2015). Additionally, a long disordered region was predicted at the N-terminus by the server XtalPred (Slabinski *et al.*, 2007), resulting in a rather poor predicted crystallizability. The N-terminal extension might be involved in signaling of the premature APP to the food vacuole, where it is further processed to its mature form.

Based on this, a truncated version of APP was designed by removing 128 amino acids on the N-terminus and six amino acids on the C-terminus (sequence listed in Appendix). However, expression of truncated APP resulted in a relatively low protein yield and the soluble fraction of APP was mainly aggregated after purification and could not be concentrated without inducing further aggregation. Because optimization of the purification protocol was not successful, a codon optimization of the gene was performed. The original APP gene from *P. falciparum* was analyzed for the presence of rare codons for *E. coli* and the codons were modified to obtain an improved codon usage without changing the amino acid sequence after translation of the mRNA. After codon optimization the truncated APP was expressed recombinantly in *E. coli* BLR pLysS cells for 16 hours and an expression profile before and after induction of expression is shown in Figure 5-2 A. The APP protein was purified from the cleared lysate by Ni-NTA affinity chromatography and the resulting eluate fractions contained around 90 % pure APP protein, as can be seen on the SDS-PAGE in Figure 5-2 B. No significant amount of APP is observed in the flow through (FT) and first washing step (W1). A small amount of APP is detected in the washing steps with buffer containing 1 mM ATP and MgCl₂ (W2 and W3). In the elution fractions (E1 and E2) a single band is visible, revealing that the APP sample contained a relatively low amount of impurities.

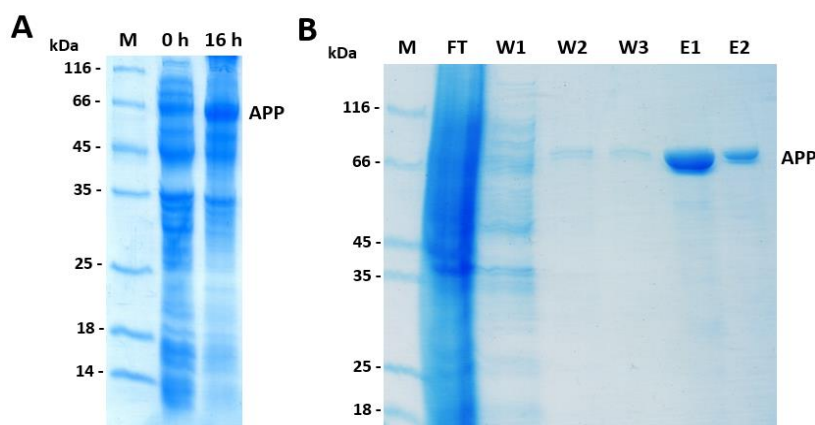


Figure 5-2: SDS-PAGE showing the expression of APP and fractions from its purification.

[A] Expression profile of APP in *E. coli* BLR pLysS cells before and 16 h after induction of expression by IPTG at 20 °C. A strong band corresponding to *P. falciparum* APP becomes visible in the sample after expression (M = molecular weight marker). [B] Elution fraction of the first purification step, the Ni-NTA affinity chromatography (M = molecular weight marker, FT = flow through, W = washing step, E = elution step).

Subsequently, a second purification step was performed by size exclusion chromatography in order to remove remaining impurities and to separate different oligomeric states of APP from each other. The resulting chromatogram is shown in Figure 5-3 A and revealed three distinct peaks. For comparison, a chromatogram before codon optimization is presented (blue curve), demonstrating a significantly reduced height of the void peak and the improved separation of latter peaks after codon optimization (red curve). In the chromatogram after codon optimization (red curve) the first peak (I) represents the void fraction containing aggregated APP as well as other impurities and the peaks II and III were further analyzed by native page (Figure 5-3 B). The native page of the elution fractions revealed, that the third fraction contained predominantly dimeric APP (155.6 kDa) and only trace amounts of monomeric (77.8 kDa) and tetrameric (311.2 kDa) APP (Figure 5-3 B). In the fraction of the second peak of the size exclusion chromatogram a mixture of dimeric and tetrameric APP was identified, together with higher oligomeric assemblies, presumably hexamers and octamers.

For structural characterization of APP, the central fractions under peak III were combined and further concentrated (typically five fractions with 10 mL volume in total). DLS was used to analyze the dispersity of the protein after concentration and a representative radius distribution pattern from a sample concentrated to $5.3 \text{ mg} \cdot \text{mL}^{-1}$ is shown in Figure 5-3 C. The determined hydrodynamic radius calculated from 20 measurements was 4.8 nm ($\approx 125 \text{ kDa}$) and showed a highly monodisperse solution (PDI = 18 %). The results demonstrate, that APP preferably forms a dimer in solution, which has already been reported to be the catalytically active form for other aminopeptidases (Li *et al.*, 2008; Iyer *et al.*, 2015). The recorded CD-spectrum shows two distinct minima at 220 nm and 208 nm, a zero crossing at 203 nm and a maximum towards 195 nm. Based on these curve characteristics it can be concluded that APP is well folded. By using a set of reference spectra and the algorithm developed by Venyaminov

et al. (1991), a secondary structure content of 40 % α -helices, 23 % β -sheets, 13 % turns and 24 % random coil was approximated.

An activity assay with APP was conducted by Jasmin Lindner (University Hamburg/University of Sao Paulo) and revealed that the protein is active (Data not shown). For this, a penta-peptide derived from human hemoglobin was used as a substrate containing a proline in P1' position. The substrate was incubated with APP and the amount of uncleaved peptide was identified by mass-spectrometry followed by taking aliquots over a period of 2 hours. A penta-peptide with glycine in P1' position instead of a proline was used as a control to verify the substrate specificity of the enzyme.

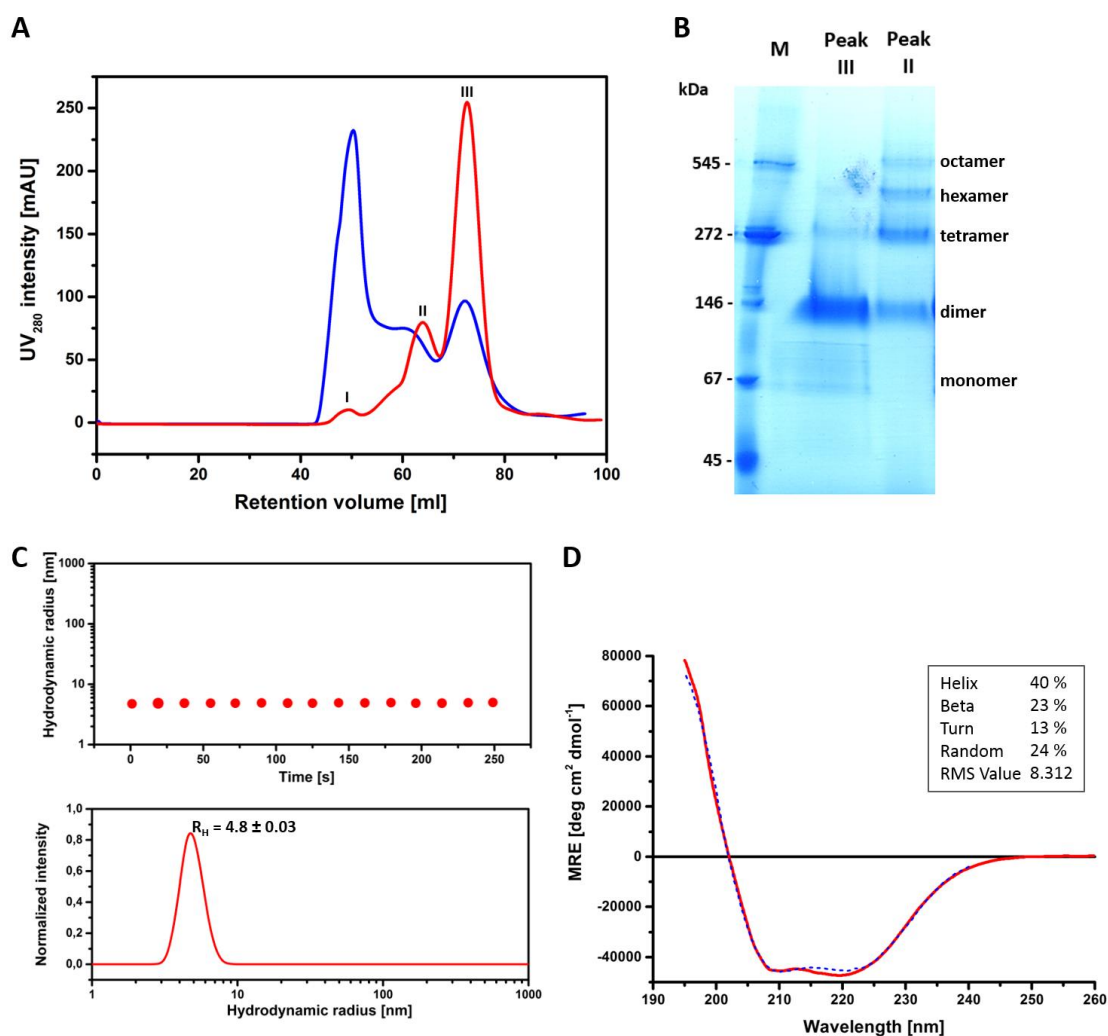


Figure 5-3: Second purification step of APP and biophysical characterization of elution fractions.

[A] Chromatogram of the size exclusion chromatography before (blue curve) and after (red curve) codon optimization. After codon optimization the void peak (I) was small and the protein mainly eluted in two major peaks at a retention volume of 64 ml (II) and 75 ml (III). [B] Native page revealed that the elution fractions from peak II contained APP in dimeric, tetrameric and presumably hexameric and octameric state, while in elution fractions from peak III mainly dimeric APP was identified. [C] Hydrodynamic radius distribution obtained by DLS measurements of an APP sample from fractions of peak III, which was concentrated up to $5.3 \text{ mg} \cdot \text{mL}^{-1}$. The solution was highly monodispers and a R_H value of $4.8 \pm 0.03 \text{ nm}$ was calculated. [D] CD-spectrum of APP shows typical characteristics for a well-folded protein and allows a secondary structure content approximation. The graphs are created with Origin (OriginPro 9.1, OriginLab, Northampton, USA).

The results showed, that after 30 minutes no significant amount of proline containing penta-peptide was identified, while the amount of glycine containing penta-peptide remained constant throughout the duration of two hours.

5.3.2 Crystallization, data collection and refinement

Crystallization trials were performed using commercially available crystallization screens according to the protocol described in section 5.2.5. APP protein crystals have formed after a few days in several crystallization conditions containing high molecular weight PEG (>1500), predominantly at pH values between 7 and 8 (theoretical isoelectric point of APP is 5.9). Successful crystal formation has been observed in crystallization experiments, which have been set up with a protein concentration ranging from 7.4 to 11.6 mg · mL⁻¹. APP crystals were colorless and possessed a rhombical shape with side dimensions up to 200 μm, while the thickness remained significantly smaller. Best diffracting crystals were obtained in a condition containing 0.2 M sodium fluoride, 0.1 M Bis-Tris propane pH 6.5 and 20% PEG 3350 with a protein concentration of 11.6 mg · mL⁻¹ (Figure 5-4 A).

For X-ray diffraction data collection, crystals were cryo-protected by supplementation of 26 % (v/v) glycerol, fished in a nylon loop, flash cooled in gaseous nitrogen at 100 K and mounted at the P14 EMBL beamline at the PETRA III synchrotron (Figure 5-4 B). Diffraction was recorded up to a resolution of 1.7 Å (Figure 5-4 C) and the data were cut at 1.89 Å resolution based on monitoring I/σ , R_{merge} and $CC_{1/2}$ after indexing, integration and scaling. The data collection statistics are shown in Table 10.

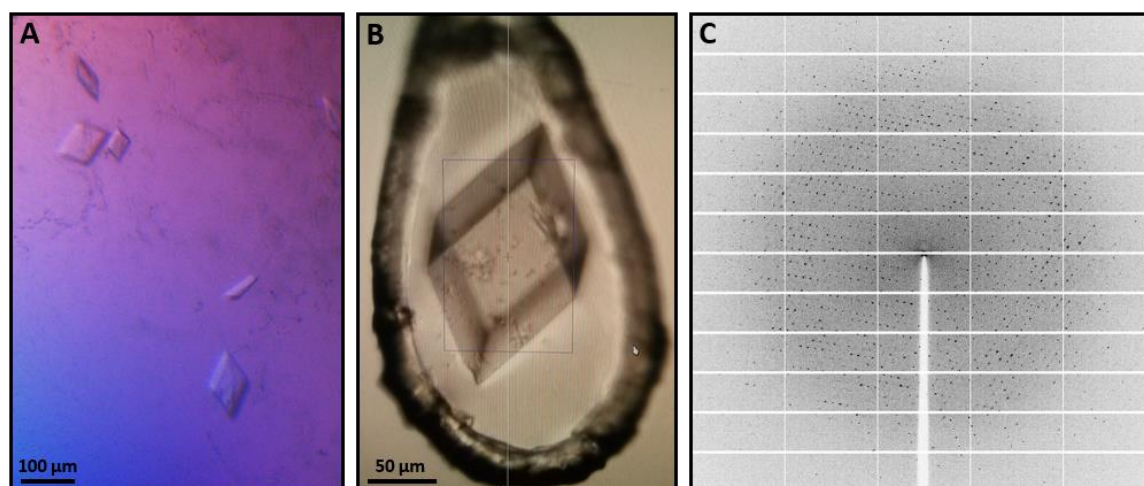


Figure 5-4: Protein crystal of *P. falciparum* APP used for X-ray diffraction data collection.

[A] APP crystals grown in 0.2 M sodium fluoride, 0.1 M Bis-Tris propane pH 6.5 and 20% PEG 3350 with a protein concentration of 11.6 mg · mL⁻¹ possessed a rhombical shape. [B] Crystals were fished with a nylon loop and flash frozen in gaseous nitrogen (100 K). [C] APP crystals diffracted up to a resolution of 1.7 Å, recorded at the P14 EMBL beamline at PETRA III.

Table 10: Data collection and refinement statistics for APP.

<i>Data collection statistics^a</i>	
Beamline	P14
Wavelength [Å]	0.96863
Space group	C2
Unit cell parameters: a, b, c [Å]	146.09, 93.86, 103.03
α, β, γ [°]	90.0, 105.33, 90.0
Resolution [Å]	30 - 1.89 (1.99 – 1.89)
Temperature [K]	100
R _{merge} ^b	6.5 (61.3)
R _{meas} ^c	7.8 (72.7)
Measured reflections	364885 (53166)
Unique reflections	106236 (15406)
Average I/σ(I)	13.1 (2.2)
Mn(I) half-set correlation CC(1/2)	99.9 (65.0)
Completeness [%]	99.2 (99.1)
Average mosaicity	0.10
Redundancy	3.4 (3.5)
<i>Refinement statistics</i>	
Resolution range [Å]	30 - 1.89
R/ R _{free} [%]	18.67 / 22.54
Protein atoms	9561
Water molecules	284
Ions	4
Ligands	4
Rms deviation	
Bond-length [Å]	0.0186
Bond angle [°]	1.8810
B factor [Å ²]	
Protein	34.7
Water	27.9
Ions	19.2
Ligands	37.3
<i>Ramachandran plot analysis</i>	
Most favored regions [%]	88.3
Allowed regions [%]	11.2
Generously allowed regions [%]	0.5

a: Values in parentheses are for the highest resolution shell.

$$b \text{ R}_{merge} = \frac{\sum_{hkl} \sum_i |I_{i(hkl)} - \langle I(hkl) \rangle|}{\sum_{hkl} \sum_i I_{i(hkl)}}$$

$$c \text{ R}_{meas} = \frac{\sum_{hkl} \sqrt{\frac{n}{n-1}} \sum_{i=1}^n |I_{i(hkl)} - \langle I(hkl) \rangle|}{\sum_{hkl} \sum_i I_{i(hkl)}}$$

where $I(hkl)$ is the mean intensity of the reflections hkl , \sum_{hkl} is the sum over all reflections and \sum_i is the sum over i measurements of reflection hkl .

The monoclinic space group C2 was identified for the crystal with unit cell dimensions of $a = 146.09 \text{ \AA}$, $b = 93.86 \text{ \AA}$, $c = 103.03 \text{ \AA}$ and $\beta = 105.30^\circ$. Based on the calculated Matthews coefficient of $2.19 \text{ \AA}^3\text{Da}^{-1}$ and a solvent content of 43.9 %, two molecules in the asymmetric unit were identified by using the software MATTPROB (Kantardjieff & Rupp, 2003; Weichenberger & Rupp, 2014). The phase problem was solved by molecular replacement using one monomer from human APP (PDB: 3CTZ) as a search model, resulting in a contrast value of 7.44, a correlation coefficient of 60 % and a R-factor of 44.5 % (Wisedchaisri & Gonen, 2013). Further refinement with isotropic B factors was done by REFMAC5 (Murshudov *et al.*, 2011), two TLS group were defined and the TLS contribution was included in the final structural model of APP. The R-factor of the final model is 18.7 % and the R_{free} -factor is 22.5 %. In chain A of the structural model amino acids 1-28, 101-102, 178-180, 199-205, 328-333 are not visible in the electron density and consequently excluded from the final model. Most of the missing loops are located in the N-terminal domain I, which also has a higher B-factor compared to domain II and domain III. In chain B the amino acids 1-53, 72-73, 97-135, 172-187, 195-202 and 332-333 are not visible in the electron density, including a large fraction of domain I. The larger fraction of missing amino acids compared to chain A can be explained by the fact, that chain A is stabilized by crystal contacts which are absent in chain B. The missing regions in both, chain A and B, are visualized in the amino acid sequence shown in the Appendix. The resulting model demonstrates excellent geometry and no Ramachandran outliers are identified using PROCHECK (Laskowski *et al.*, 1993). Processing and refinement statistics are summarized in Table 10.

5.3.3 Structural model interpretation

A sequence alignment of APP has been performed with known homologue structures by the server Clustal Omega (Sievers *et al.*, 2011) and was visualized by the ESPript server (Robert & Gouet, 2014) (Figure 5-5). For human APP, which has a sequence identity of 35 %, an $C\alpha$ RMSD value of 2.1 \AA has been calculated by superimposing the structure with the structural model of APP (PDBeFold, (Krissinel & Henrick, 2004)). The $C\alpha$ RMSD value from the structure comparison with *C. elegans* APP, which has a lower sequence identity (30 %), was calculated to be 1.7 \AA .

As expected from the data of the biophysical characterization, APP forms a homodimer in the crystal (Figure 5-7 A). The overall size of the dimer is approximately $85 \times 70 \times 55 \text{ \AA}^3$. The stabilization of the dimer is mostly based on hydrophobic interactions and four hydrogen bonds. The dimer interface consists of three hydrophobic patches, a large patch between the domains III of chain A and B and two small patches in domain I and domain II. The largest patch in domain III is build up by side chains of the residues I₅₁₂, F₅₁₃, Y₅₁₆, L₅₂₂, F₅₂₄, I₅₂₅, F₅₃₁, F₅₃₄, P₅₆₀, K₅₉₇ and Y₆₀₅, as shown in Figure 5-6. Additional hydrophobic patches are created by L₁₅₆, P₁₆₀, K₁₆₁ and K₁₆₃ of domain I in chain A, interacting with P₃₃₄

and F₃₃₆ of domain II in chain B and vice versa. Hydrogen bonds further stabilize the dimer interaction and are found between D₅₃₆ of chain A and Y₅₁₆ of chain B as well as for the symmetry equivalent (distance 2.5 Å) and additionally between E₅₂₈ of chain A/B and R₅₀₇ of chain B/A (distance 2.9 Å). As a result of these interactions, approximately 1580 Å² from each subunit are buried from the total solvent accessible surface area (28350 Å²) upon dimer formation.

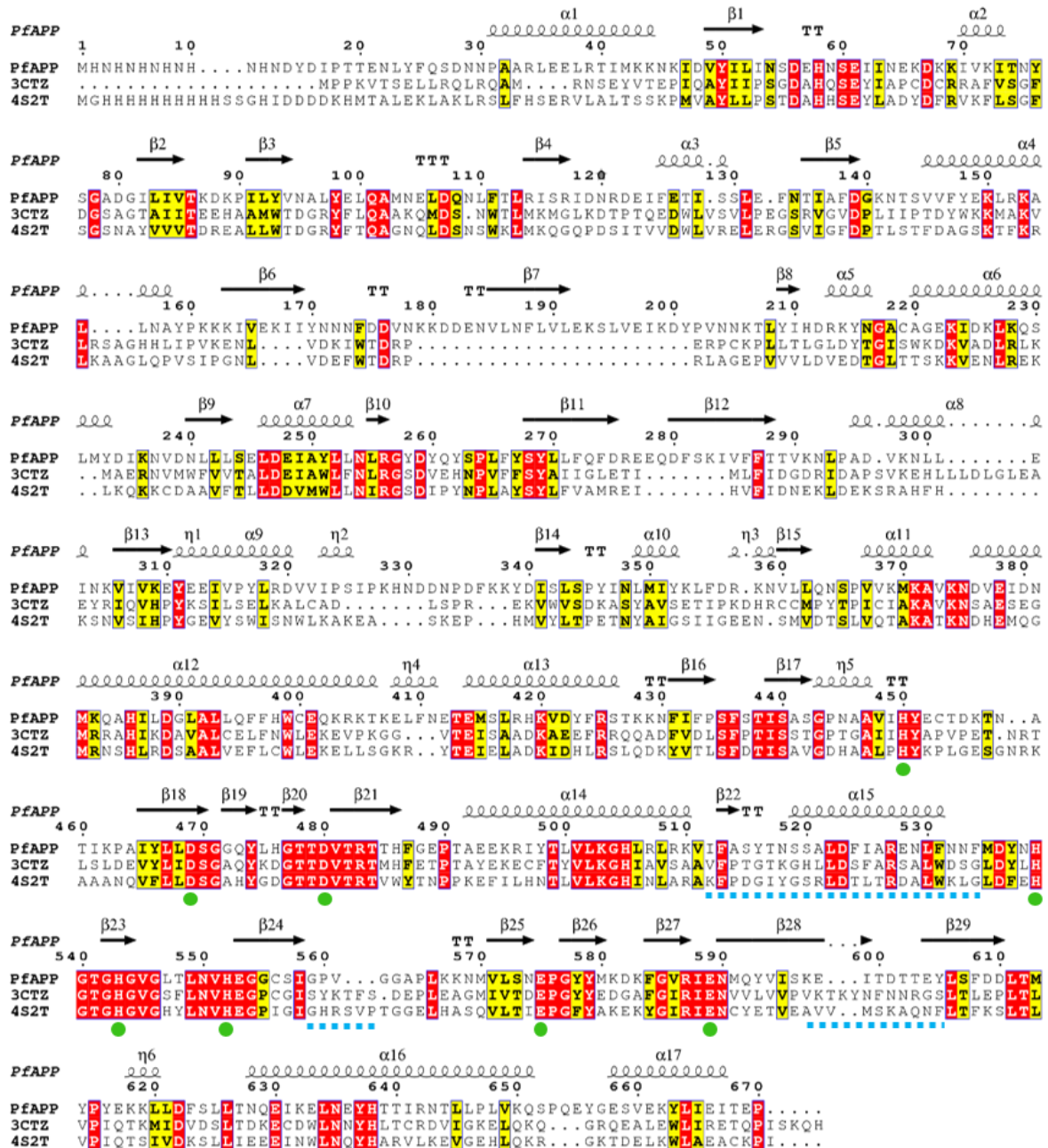


Figure 5-5: Multiple sequence alignment of *P. falciparum* APP with closest structurally known homologues. The multiple sequence alignment was performed with the web server Clustal Omega (Sievers *et al.*, 2011) and the graphical presentation was generated using the ESPript 3.0 server (Robert & Gouet, 2014). The secondary structure of APP is displayed above the alignment with α-helices (spirals), β-strands (arrows), turns (T) and 3₁₀ helices (μ). Identical residues are indicated by a red background and similar residues by yellow background. The residues contributing to the active site are highlighted by green circles (below) and a dashed blue line indicates amino acids located at the dimer interface.

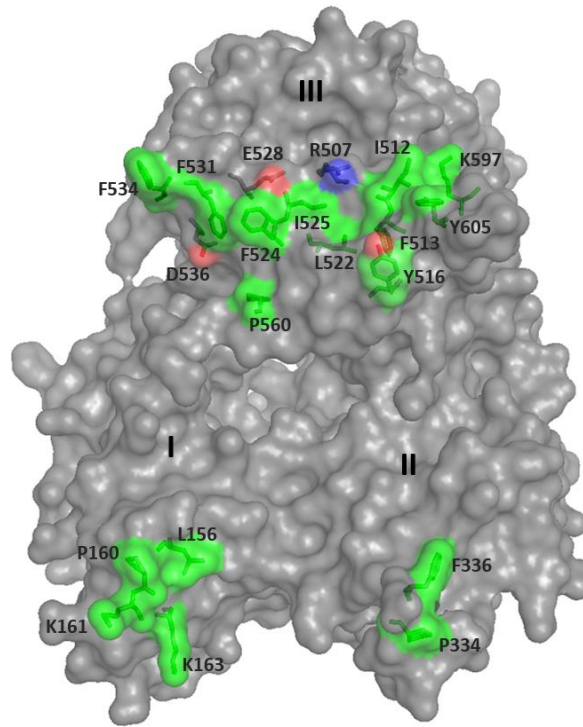


Figure 5-6: Surface illustration of the dimer interface of *P. falciparum* APP.

The overall surface of the three domains (I, II and III) is colored gray. The dimer interface consists of three hydrophobic patches (green) and 4 hydrogen bonds (red and blue). The figure was created with PyMOL (Schrödinger, LLC).

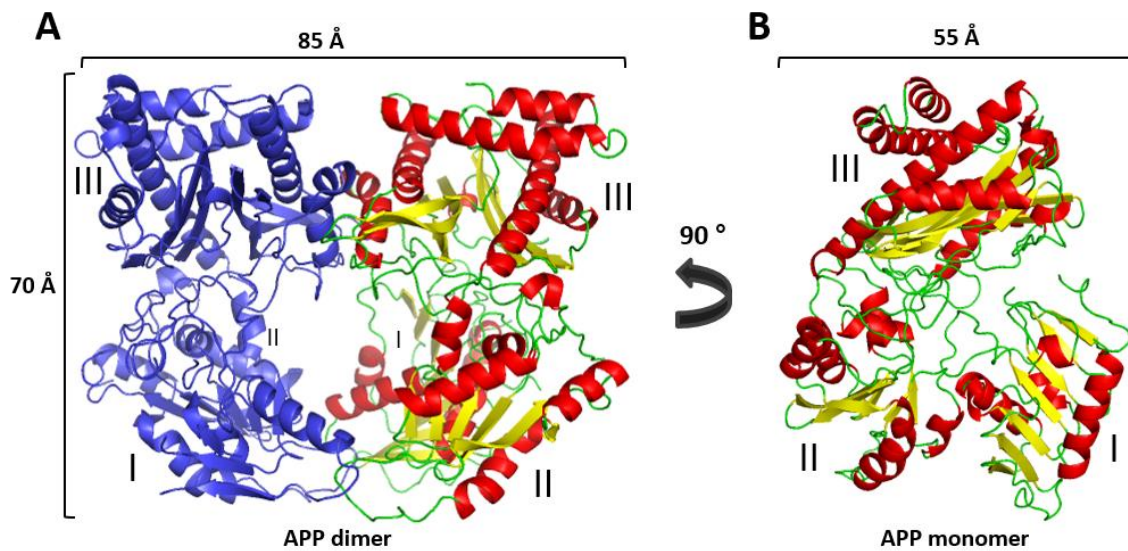


Figure 5-7: Cartoon representation of the structural model of *P. falciparum* APP.

[A] APP is found in a homodimer assembly in the crystal with dimensions 85 x 70 x 55 Å³. [B] One APP monomer consist of three domains, domain I from the N-terminus to residue 203, domain II from residue 204 to 374 and domain III from residue 375 to the C-terminus. In the cartoon representation β-strands are colored yellow, α-helices in red and green is used for turns and loops. The figure was created with PyMOL (Schrödinger, LLC).

Similar to human APP and *C. elegans* APP, each monomer of *P. falciparum* APP possesses a three domain architecture (Figure 5-7 B). The N-terminal domain (domain I) includes residues 1-203, the middle domain (domain II) consist of residues 204-374 and the C-terminal domain (domain III) spans from residue 375 to 670 (C-terminus). The general fold of domain I is composed of a central seven-stranded β -sheet in the topological order 4 3 2 1 5 7 6, with strand β_2 being antiparallel. The β -sheet is flanked by four α -helices, with α_3 and α_4 located on the concave side and α_1 and α_2 on the convex side. The arrangement of the secondary structure elements is visualized in Figure 5-8 A. The fold of domain II is similar to that of domain I with some small modifications. The central β -sheet contains five strands in the order 11 10 9 8 12 13 with β_9 pointing in the opposite direction. In addition, seven α -helices are present, α_9 and α_{10} on one side and α_5 , α_6 , α_7 , α_8 and α_{11} on the other side (Figure 5-8 B). An alignment of 101 amino acids from both domains (I & II) resulted in a RMSD value of 2.4 Å.

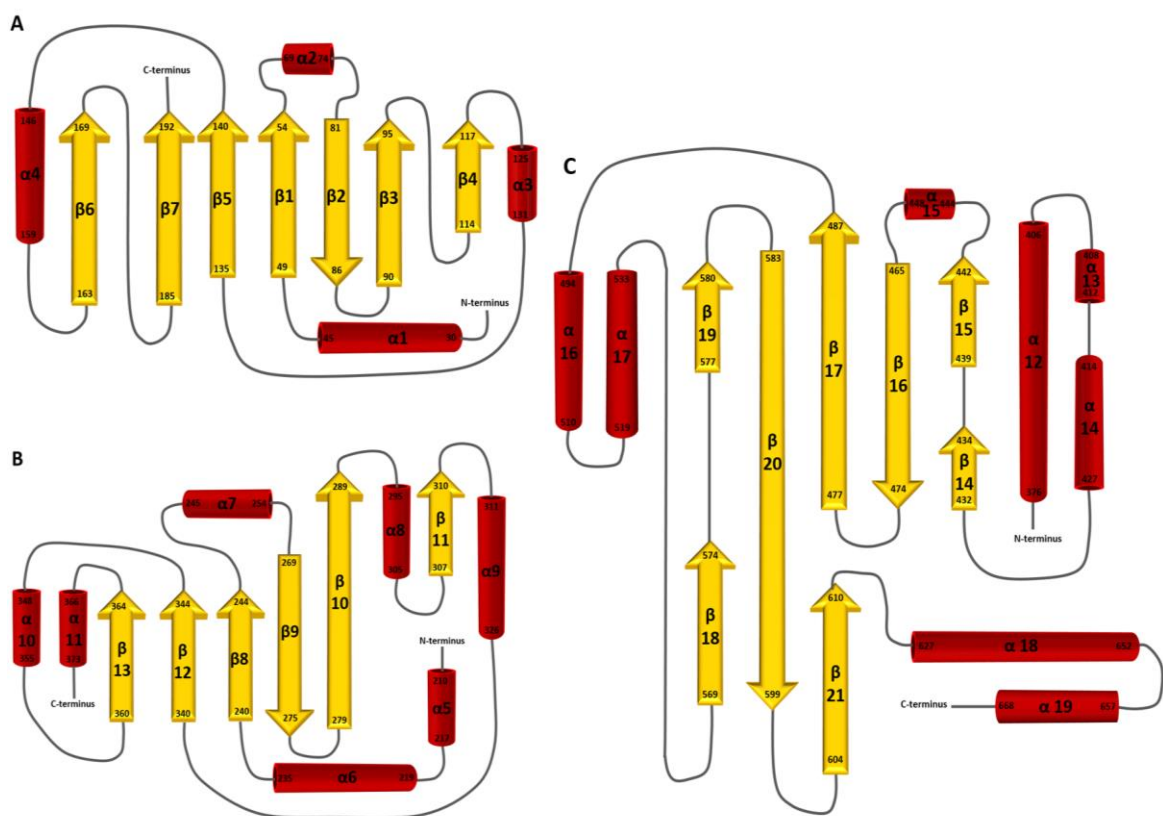


Figure 5-8: Schematic presentation of the topology details of the APP domains.

[A] The architecture of domain I reveals a central seven-stranded β -sheet (4-3-2-1-5-7-6, β_2 being antiparallel), flanked by the helices α_3 and α_4 on the one and α_1 and α_2 on the other side. [B] Domain I possesses a similar fold as domain I with six central β -strands (11-10-9-8-12-13, β_9 antiparallel) surrounded by the helices α_9 and α_{10} on one side and α_5 , α_6 , α_7 , α_8 and α_{11} on the other side. [C] Domain III contains two β -sheets, the first is built of four antiparallel strands (β_{14} extends to β_{15} , β_{16} (antiparallel) and β_{17}) and the second β -sheet has a long strand (β_{20}) which is flanked on the top end by β_{19} and on the bottom end by β_{18} and β_{21} . The first β -sheet is flanked by the α -helices α_{12} , α_{13} and α_{14} and the second β -sheet is surrounded by α_{15} , α_{16} and α_{17} . Two α -helices (α_{18} , α_{19}) bridge the two β -sheets in perpendicular orientation. α -helices in red and β -sheets in yellow are to scale, while the turns and loops (grey) are not to scale.

Domain III exhibits a “pita-bread” fold, which is typical for methionine aminopeptidases, aminopeptidase P and prolidases (Lowther & Matthews, 2002), and comprises of two central antiparallel β -sheets. The first one is four-stranded and contains the strands β_{14} which extends to β_{15} , β_{16} (antiparallel) and β_{17} . The second β -sheet is nearly perpendicular to the direction of the first β -sheet and contains a long curved strand β_{20} which on the top end is flanked by a short antiparallel strand β_{19} and on the bottom end on both sides by the antiparallel strands β_{18} and β_{21} . The first β -sheet is surrounded by three α -helices, α_{12} , α_{13} and α_{14} , while the second β -sheet is enclosed by α_{15} , α_{16} and α_{17} . Towards the C-terminus of APP two α -helices (α_{18} and α_{19}) bridge the two β -sheets in perpendicular orientation. The architecture of domain III is displayed in Figure 5-8 C.

The active site is formed by the conserved amino acids D₄₆₉, D₄₈₀, H₅₄₂, H₅₄₃, E₅₇₅ and E₅₈₉ in the center of the pseudo 2-fold-symmetric C-terminal domain. All six amino acids contribute to the coordination of two metal ions of a dinuclear center. The metal ions are most likely manganese ions because they are identified in human APP (Li *et al.*, 2008) and shown to be required for activity in *P. falciparum* APP (Ragheb *et al.*, 2009). The first Mn²⁺ ion (named Mn1 in Figure 5-9) is coordinated by D₄₆₉ (2.2 Å and 2.5 Å), D₄₈₀ (2.0 Å) and E₅₈₉ (2.1 Å) as well as by two water molecules (W1 and W3) with distances to the Mn²⁺ of 2.4 Å and 2.2 Å. The second Mn²⁺ is coordinated by D₄₈₀ (2.1 Å), E₅₈₉ (1.9 Å), E₅₇₅ (2.2 Å), H₅₄₃ (2.3 Å) and H₅₅₂ via a water molecule (2.6 Å), which has a distance to the Mn²⁺ of 2.1 Å. Additionally, the Mn²⁺ is stabilized by a second water (W3, 2.3 Å), which is coordinated by E₅₇₅ (2.6 Å). This results in octahedral coordination of both Mn²⁺ ions and B-factors of 19.6 and 20.5.

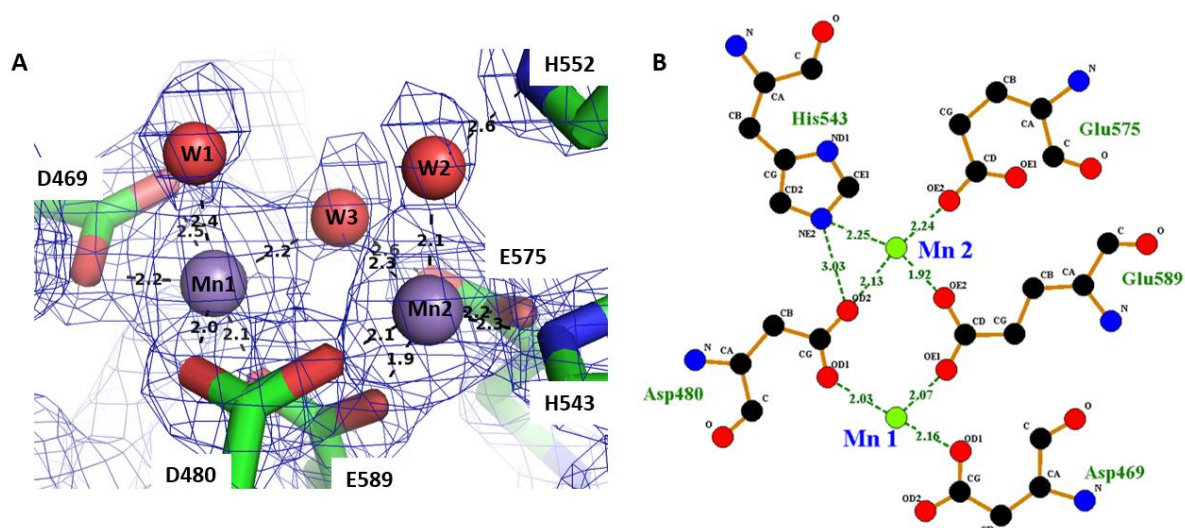


Figure 5-9: Active site of *P. falciparum* APP.

[A] Active site of APP with amino acids in stick representation colored by atom types (carbon in green, oxygen in red and nitrogen in blue). Two Mn²⁺ ions and three water molecules are shown as purple and red spheres, respectively. The $2F_o - F_c$ electron density map is superimposed (blue mesh), contoured at 2σ . Residues are labeled and distances between atoms are shown in angstrom. The figure was created with PyMOL (Schrödinger, LLC). [B] Schematic 2D representation of the molecular interactions between the amino acids in the active site and the Mn²⁺ ions. Distances are given in angstrom and for clarity reason water molecules are not shown. The figure has been prepared with Ligplot (Wallace *et al.*, 1995).

In previous studies of human and *E. coli* APP it was postulated that the manganese cluster is bridged by a water molecule (corresponding to W3 in Figure 5-9), which thereby is able to perform a nucleophilic attack on the X-pro bond of the substrate peptide (Li *et al.*, 2008; Graham *et al.*, 2004).

5.4 Conclusions

Codon optimization and truncation of the unfolded part of the N-terminal domain were the key steps that allowed establishing a protocol for APP expression and purification. Further, supplementation of manganese in the expression medium and protein buffer are substantial for correct APP folding. After improvement of the protocol, highly pure and active APP was obtained and showed a predominantly dimeric assembly in solution. Screening of crystallization conditions was successful and resulted in APP crystals with rhombical shape that diffracted up to 1.7 Å. The diffraction data could be indexed, scaled and merged and a structural model of APP was refined up to 1.89 Å resolution. The APP was found as a homodimer in the crystal and revealed the expected three-domain architecture. Domain I and domain II exhibit a similar fold and can be superimposed with an RMSD value of 2.4 Å. Domain III shows a typical “pita-bread” fold, which is known from other aminopeptidases. The resulting structural APP model shows a high structural homology to human APP (C α RMSD = 2.1 Å) and to *C. elegans* APP (C α RMSD = 1.7 Å). In particular, the active site is highly conserved and the di-nuclear Mn²⁺ cluster is coordinated similar to the human APP, which indicates that both enzymes share a common mode of substrate binding and a similar catalytic mechanism. In the future, highly interesting information about the still poorly understood substrate specificity for peptides with proline in P1` position can be obtained by co-crystallizing the APP with a non-cleavable peptide substrate. Also co-crystals with the known aminopeptidase inhibitors apstatin and bestatin might provide valuable insights into the mechanism of the enzymatic function of APP. By analyzing the structural differences and similarities between the enzyme-inhibitor complexes, new inhibitors can potentially be designed that are specific for *P. falciparum* APP.

APPENDIX

LIST OF ABBREVIATIONS

α	Alpha
Å	Angstrom
ACF	Autocorrelation function
AHT	Anhydrotetracycline
APTS	(3-Aminopropyl)trimethoxysilane
APP	Aminopeptidase P
β	Beta
C	Celsius
CCD	Charge-coupled device
Da	Dalton
DLS	Dynamic light scattering
DDLS	Depolarized dynamic light scattering
fs	Femtosecond
γ	Gamma
g	Gram
G	Gravitational constant
GPTS	(3-Glycidyoxypropyl)trimethoxysilane
h	Hour
IPTG	Isopropyl- β -D-thiogalactopyranosid
k	Kilo
K	Kelvin
l	Liter
LB	Lennox-Broth
LSW-theory	Lifshitz/Slezov/Wagner theory
m	Meter
min	Minute
Ni-NTA	Nickel-Nitrilotriacetic acid
mm	Millimeter
ms	Millisecond
M	Molar
M	Mega
MWCO	Molecular weight cutoff
ML1	Mistletoe lectin 1
μ	Micro
nm	Nanometer
ns	Nanosecond
O ₂	Oxygen
OD	Optical density
p	Pico
PDB	Protein Data Bank
PDMS	(Poly)dimethylsiloxane
PGMEA	Propylene glycol methyl ether acetate
Rpm	Rounds per minute
s	Second
σ	Sigma
ThiM	5-(hydroxyethyl)-4-methylthiazole kinase
TF	Thermofluor
TRX	Thioredoxin
UV	Ultraviolet
V	Volt
v/v	Volume per volume
W	Watt
w/v	Weight per volume

SCRIPTS

Bash scripts for automated data processing with XDS and XSCALE, in parts modified from Yorke *et al.*, 2014.

```
##### PREPARE FOLDER STRUCTURE #####
#!/bin/sh
PROCDIR= # processing directory
l=1 # starting scan number
k=60 # ending scan number
n=20 # number of images per scan
i=1
j=1
mkdir ./PROCDIR
while [ $l -le $k ]
do
mkdir ./PROCDIR/run-$i
while ((j<=$n))
do
cp PATH_TO_IMAGES/?_${l}_????$j.cbf ./PROCDIR/run-$i/
cp PATH_TO_IMAGES/?_${l}_???$j.cbf ./PROCDIR/run-$i/ << EOF
EOF
let j=j+1
done
let l=l+1
let j=1
let i=i+1
done

##### CREATE XDS.INP FILE FROM CBF HEADER #####
#!/bin/bash
# A script to generate an XDS.INP for a pilatus header and integrate batches of a dataset
# RLO 07/11/2011, edited by ARP 14/07/2015
TOPDIR= # insert path to image files here
OUTDIR= # insert path to output directory here
WEDGEID=run- # insert wedge ID
NUMBEROFWEDGES=20 # insert number of wedges
NUMBERIMAGE=20 #Total number of images collected
NBATCH=20 #Number of batches to split this into
#To integrate single images set NBATCH=NUMBERIMAGE
# NUMBERIMAGE/NBATCH MUST be an integer
# Spacegroup and unit cell
SPACEGROUPNUMBER=0
A=
B=
C=
ALPHA=
BETA=
GAMMA=
# Set Friedels law
FRIEDELRLAW=TRUE
# Set min and max resolution
MINIMUMRES=
MAXIMUMRES=
# Set beam centre.
BEAMX=
BEAMY=
mkdir $OUTDIR
for (( i=1; i<=NUMBEROFWEDGES; i++))
do
#Comment below in for individual image integration
for (( j=1; j<=NBATCH; j++))
do
cd $OUTDIR
mkdir run-$i > /dev/null
cd run-$i > /dev/null
touch XDS.INP
FULLLOCATION=$TOPDIR/$WEDGEID$i
FILE=$(ls $TOPDIR/$WEDGEID$i/*.cbf | head -1 | awk -F"/" '{print $NF}')
FILENAME=$(echo $FILE | awk -F"/" '{print $(NF)}')
LEADINGNAME=$(echo $FILE | awk -F"_000" '{print $1}')
#LOCALFILENAME=$(echo $LEADINGNAME"_$i"_"###.cbf")
STARTNUMBER=$(( 1+ ($j-1) * ($NUMBERIMAGE/$NBATCH) ))
FINISHNUMBER=$(( $j*($NUMBERIMAGE/$NBATCH) ))
ln -s $FULLLOCATION images
SILICONTICKNESS=$(head -31 $FULLLOCATION/$FILENAME | grep "Silicon sensor, thickness" | awk -F" " '{print $5}')
SILICONTICKNESS=$(echo "$SILICONTICKNESS*1000" | bc)
SILICONTICKNESS="0"$SILICONTICKNESS
EXPOSUREPERIOD=$(head -31 $FULLLOCATION/$FILENAME | grep "Exposure_period" | awk -F" " '{print $3}')
WAVELENGTH=$(head -31 $FULLLOCATION/$FILENAME | grep "Wavelength" | awk -F" " '{print $3}')
DETECTORDISTANCE=$(head -31 $FULLLOCATION/$FILENAME | grep "Detector_distance" | awk -F" " '{print $3}')
```

SCRIPTS

```

DETECTORDISTANCE=$(echo "$DETECTORDISTANCE * 1000" | bc)
if [ "$$BEAMCENTERFROMIMAGE" = "TRUE" ]; then
BEAMX=$(head -31 $FULLLOCATION/$FILENAME | grep "Beam_xy" | awk -F"(" '{print $2}' | awk -F", " '{print $1}')')
BEAMY=$(head -31 $FULLLOCATION/$FILENAME | grep "Beam_xy" | awk -F"(" '{print $2}' | awk -F", " '{print $1}')')
fi
FLUX=$(head -31 $FULLLOCATION/$FILENAME | grep "Flux" | awk -F" " '{print $3}')
FILTERTRANSMISSION=$(head -31 $FULLLOCATION/$FILENAME | grep "Filter_transmission" | awk -F" " '{print $3}')
OSCILLATIONANGLE=$(head -31 $FULLLOCATION/$FILENAME | grep "Angle_increment" | awk -F" " '{print $3}')
POLARIZATION=$(head -31 $FULLLOCATION/$FILENAME | grep "Polarization" | awk -F" " '{print $3}')
echo " JOB= ALL " >> XDS.INP
echo " NAME_TEMPLATE OF DATA_FRAMES=images/${LEADINGNAME}?????.cbf CBF" >> XDS.INP
echo " DATA_RANGE=$STARTNUMBER $FINISHNUMBER >> XDS.INP
echo " SPOT_RANGE=$STARTNUMBER $FINISHNUMBER >> XDS.INP
echo " BACKGROUND_RANGE=$STARTNUMBER $FINISHNUMBER >> XDS.INP
echo " OSCILLATION_RANGE= $OSCILLATIONANGLE !degrees (>0) " >> XDS.INP
echo " X-RAY_WAVELENGTH= $WAVELENGTH !(Angstrom) " >> XDS.INP
echo " DETECTOR_DISTANCE= $DETECTORDISTANCE !(mm) " >> XDS.INP
echo " ORGX=$BEAMX ORGY=$BEAMY !Detector origin (pixels). ORGX=NX/2; ORGY=NY/2" >> XDS.INP
echo " SPACE_GROUP_NUMBER=$SPACEGROUPNUMBER >> XDS.INP
echo " UNIT_CELL_CONSTANTS= $A $B $C $ALPHA $BETA $GAMMA " >> XDS.INP
echo " FRIEDEL'S LAW= $FRIEDEL'SLAW !Default is TRUE" >> XDS.INP
echo " DIRECTION_OF_DETECTOR_X-AXIS= 1 0 0" >> XDS.INP
echo " DIRECTION_OF_DETECTOR_Y-AXIS= 0 1 0" >> XDS.INP
echo " ROTATION_AXIS= 0.0 -1.0 0.0" >> XDS.INP
echo " INCIDENT_BEAM_DIRECTION=-0.0 0.0 1.0" >> XDS.INP
echo " FRACTION_OF_POLARIZATION=0.98" >> XDS.INP
echo " POLARIZATION_PLANE_NORMAL= 0 1 0" >> XDS.INP
echo " DETECTOR=PILATUS NX=2463 NY=2527 QX=0.172 QY=0.172" >> XDS.INP
echo " MINIMUM_VALID_PIXEL_VALUE=-1 OVERLOAD=1048500" >> XDS.INP
echo " MINIMUM_NUMBER_OF_PIXELS_IN_A_SPOT=3 ! Default is 6" >> XDS.INP
echo " !MINIMUM_ZETA=0.05" >> XDS.INP
echo " STRONG_PIXEL=3" >> XDS.INP
echo " SENSOR_THICKNESS=$SILICONTHICKNESS" >> XDS.INP
echo " !SILICON=0.0 >> XDS.INP
echo " TRUSTED_REGION=0.0 1.15 !Relative radii limiting trusted detector region" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 487 495 0 2528" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 981 989 0 2528" >> XDS.INP
echo " UNTRUSTED_RECTANGLE=1475 1483 0 2528" >> XDS.INP
echo " UNTRUSTED_RECTANGLE=1969 1977 0 2528" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 0 2464 195 213" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 0 2464 407 425" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 0 2464 619 637" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 0 2464 831 849" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 0 2464 1043 1061" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 0 2464 1255 1273" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 0 2464 1467 1485" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 0 2464 1679 1697" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 0 2464 1891 1909" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 0 2464 2103 2121" >> XDS.INP
echo " UNTRUSTED_RECTANGLE= 0 2464 2315 2333" >> XDS.INP
echo " !REFINE (IDXREF)=BEAM AXIS ORIENTATION CELL !DISTANCE" >> XDS.INP
echo " !REFINE (INTEGRATE)=BEAM ORIENTATION CELL !DISTANCE AXIS" >> XDS.INP
echo " !REFINE (CORRECT)=DISTANCE BEAM ORIENTATION CELL AXIS" >> XDS.INP
echo " !MINUTE=1" >> XDS.INP
echo " !MAXIMUM_NUMBER_OF_JOBS=8 !Speeds-up COLSPOT & INTEGRATE on a Linux-cluster" >> XDS.INP
echo " !MAXIMUM_NUMBER_OF_PROCESSORS=8!<25;ignored by single cpu version of xds" >> XDS.INP
echo " VALUE_RANGE_FOR_TRUSTED_DETECTOR_PIXELS= 7000 30000 !Used by DEFPPIX" >> XDS.INP
echo " INCLUDE_RESOLUTION_RANGE=$MINIMUMRES $MAXIMUMRES >> XDS.INP
chmod 755 XDS.INP
xds_par
cp XDS_ASCII.HKL XDS_ASCII_$j.HKL
cp CORRECT.LP CORRECT_$j.LP
cd - > /dev/null
done
done

##### CREATE INPUT FILE FOR XSCALE #####
#!/bin/sh
l= # Space group number of datasets
j= # Number of wedge
i= # Reference dataset name
grep -r --include \CORRECT_$j.LP "SPACE_GROUP_NUMBER=...*$l" >>temp1.txt
sed -r -e 's/^\{0\}/&'INPUT_FILE=/' <temp1.txt >temp2.txt
cat temp2.txt >> temp3.txt
echo "FRIEDEL'S LAW= TRUE
MERGE= FALSE
REFERENCE_DATA_SET=$i
MINIMUM_I/SIGMA=3" >> temp3.txt
rm temp1.txt
rm temp2.txt
sed -i 'li\' temp3.txt
sed '1,1s/^\{0\}/&'OUTPUT_FILE= xscale.hkl /' temp3.txt > temp4.txt
rm temp3.txt
sed -r -e 's/CORRECT.LP: SPACE_GROUP_NUMBER= '$l'/XDS_ASCII.HKL/' <temp4.txt >temp5.txt
sed -i '/as used in the INTEGRATE step/d' temp5.txt
sed -i '/(0: unknown symmetry and unit cell)/d' temp5.txt
awk '!a[$0]++' temp5.txt > XSCALE.INP

```

SCRIPTS

```
rm temp4.txt
rm temp5.txt
xscale # In case correlation factor for scaling is too low, single input files have to be removed

##### CONVERT HKL FILE TO MTZ #####
#!/bin/sh
cat XDSCONV.INP
echo "OUTPUT_FILE= temp.hkl CCP4
INPUT_FILE= xscale.hkl
FRIEDEL'S LAW= TRUE
MERGE= TRUE" >> XDSCONV.INP
xdsconv
f2mtz HKLOUT temp.mtz<F2MTZ.INP
cad HKLIN1 temp.mtz HKLOUT XDS_ASCII.mtz<<EOF
LABOUT H K L FP SIGFP
CTYPOUT H H H F Q
END
EOF
```

Calibration file for DLS measurements in microfluidic PDMS chip using the Spectrolight600 instrument

```
l 20
w 15
h 16
rows 2
columns 15
drops 1
x0 48.6
y0 33.6
px 0.99
py 6.4
dx0 0.25
dy0 0.25
dia 0.5
```

Search pattern for automated DLS measurement positioning

```
0.00 0.04 0.08 -0.04 -0.08 #Z-values (5 steps)
0.00 0.00 0.10 0.00 0.00 0.10 -0.10 0.00 0.00 -0.10 #X- and Y-values for 5 positions
```


AMINO ACID SEQUENCE OF *P. FALCIPARUM* APP

	-101		0
Trunc_APP_ChainA			
Trunc_APP_ChainB			0
Full-length_APP		MQLNFLLFVFIFLMVFHLNIFNKGKRQNLVSAYLNHFKKSYFSGVTSGSDCVNKS EVSSD	-42
		1	
Trunc_APP_ChainA		-----MHNNHHNNHHNNDYDIPT	19
Trunc_APP_ChainB		-----MHNNHHNNHHNNDYDIPT	19
Full-length_APP		NNNNNNNNKIAHNF FSK KYQRNF ENNLS ENQENNKNIYS GSNIFKNIYNTMMSNN	19
Trunc_APP_ChainA		TENLYFQSDNNPAARLEELRTIMKKNKIDVYILINSDEHNSEINEKDKKIVKITNYSGA	79
Trunc_APP_ChainB		TENLYFQSDNNPAARLEELRTIMKKNKIDVYILINSDEHNSEINEKDKKIVKITNYSGA	79
Full-length_APP		NTVDVNMNNNNPAARLEELRTIMKKNKIDVYILINSDEHNSEINEKDKKIVKITNYSGA *****	79
Trunc_APP_ChainA		DGILIVTKDKPILYVNALYELQAMNELDQNLFTLRISRIDNRDEIFETISSLEFNITIAFD	139
Trunc_APP_ChainB		DGILIVTKDKPILYVNALYELQAMNELDQNLFTLRISRIDNRDEIFETISSLEFNITIAFD	139
Full-length_APP		DGILIVTKDKPILYVNALYELQAMNELDQNLFTLRISRIDNRDEIFETISSLEFNITIAFD *****	139
Trunc_APP_ChainA		GKNTSVVFYEKLRKAL LNAYPK KIVEK IYNNN FDDV NK KDD ENV LNF LVL EKS LVE IK	199
Trunc_APP_ChainB		GKNTSVVFYEKLRKAL LNAYPK KIVEK IYNNN FDDV NK KDD ENV LNF LVL EKS LVE IK	199
Full-length_APP		GKNTSVVFYEKLRKAL LNAYPK KIVEK IYNNN FDDV NK KDD ENV LNF LVL EKS LVE IK *****	199
Trunc_APP_ChainA		DYPVNNKTLYIHDRKYNACAGEKIDKLKQSLMYDIKNVDNLLLSELDEIAYLLNLRGYD	259
Trunc_APP_ChainB		DYPVNNKTLYIHDRKYNACAGEKIDKLKQSLMYDIKNVDNLLLSELDEIAYLLNLRGYD	259
Full-length_APP		DYPVNNKTLYIHDRKYNACAGEKIDKLKQSLMYDIKNVDNLLLSELDEIAYLLNLRGYD *****	259
Trunc_APP_ChainA		YQYSPLFYSYLLFQFDREEQDFSKIVFFTIVKKNLPADVKNLLEINKVIVKEYEEIVPYLR	319
Trunc_APP_ChainB		YQYSPLFYSYLLFQFDREEQDFSKIVFFTIVKKNLPADVKNLLEINKVIVKEYEEIVPYLR	319
Full-length_APP		YQYSPLFYSYLLFQFDREEQDFSKIVFFTIVKKNLPADVKNLLEINKVIVKEYEEIVPYLR *****	319
Trunc_APP_ChainA		DVVIPSIPKHNDNDPDKFYDILSPYINLMIYKLFDRKNVLLQNSPVVKMKAVKNDVEI	379
Trunc_APP_ChainB		DVVIPSIPKHNDNDPDKFYDILSPYINLMIYKLFDRKNVLLQNSPVVKMKAVKNDVEI	379
Full-length_APP		DVVIPSIPKHNDNDPDKFYDILSPYINLMIYKLFDRKNVLLQNSPVVKMKAVKNDVEI *****	379
Trunc_APP_ChainA		DNMKQAHILDGLALLQFFHWCEQKRKTKELFNETEMSLRHKVDYFRSTKKNFIFPSFSTI	439
Trunc_APP_ChainB		DNMKQAHILDGLALLQFFHWCEQKRKTKELFNETEMSLRHKVDYFRSTKKNFIFPSFSTI	439
Full-length_APP		DNMKQAHILDGLALLQFFHWCEQKRKTKELFNETEMSLRHKVDYFRSTKKNFIFPSFSTI *****	439
Trunc_APP_ChainA		SASGPNAAVIHYECDKTNATI KPAIYL LDSGGQYLHGTTDVTRTHFGPEPTAEEKRIYT	499
Trunc_APP_ChainB		SASGPNAAVIHYECDKTNATI KPAIYL LDSGGQYLHGTTDVTRTHFGPEPTAEEKRIYT	499
Full-length_APP		SASGPNAAVIHYECDKTNATI KPAIYL LDSGGQYLHGTTDVTRTHFGPEPTAEEKRIYT *****	499
Trunc_APP_ChainA		LVLKGHLRLRKVI FASYTNSSA LDF IARENLFNNFMDYNHGTGHGVGLTLNVHEGGCSIG	559
Trunc_APP_ChainB		LVLKGHLRLRKVI FASYTNSSA LDF IARENLFNNFMDYNHGTGHGVGLTLNVHEGGCSIG	559
Full-length_APP		LVLKGHLRLRKVI FASYTNSSA LDF IARENLFNNFMDYNHGTGHGVGLTLNVHEGGCSIG *****	559
Trunc_APP_ChainA		PVGGAPLKKMML SNEPGYMKDKFGVR IENMQYVISKEITDTTEYLSFDDL TMYPYEKK	619
Trunc_APP_ChainB		PVGGAPLKKMML SNEPGYMKDKFGVR IENMQYVISKEITDTTEYLSFDDL TMYPYEKK	619
Full-length_APP		PVGGAPLKKMML SNEPGYMKDKFGVR IENMQYVISKEITDTTEYLSFDDL TMYPYEKK *****	619
Trunc_APP_ChainA		LLDFSLLTNQEIKELNEYHTTIRNTLLPLVKQSPQEYGESVEKYLI EITEP ----- 670	670
Trunc_APP_ChainB		LLDFSLLTNQEIKELNEYHTTIRNTLLPLVKQSPQEYGESVEKYLI EITEP ----- 670	670
Full-length_APP		LLDFSLLTNQEIKELNEYHTTIRNTLLPLVKQSPQEYGESVEKYLI EITEP IAIHNN 676 *****	676

Deleted N- and C-terminal regions (128 amino acids at N-terminus and 6 amino acids at C-terminus)

N-terminal His-tag with TEV cleavage site

Missing loops in the electron density

INSTRUMENTATION AND CHEMICALS

Instrumentation

Table 11: Instrumentation (listed alphabetically).

Instrument	Manufacturer
Agarose gel electrophoresis	- PerfectBlue™ Mini S (Peqlab, Germany)
	- PowerPac 200 (Bio-Rad, Germany)
	- PerfectBlue™ Mini S (Peqlab, Germany)
Äkta purifier	Äkta purifier 900 (GE Healthcare, USA)
Beamlines	- P13, EMBL, PETRA III, DESY, Hamburg
	- P14, EMBL, PETRA III, DESY, Hamburg
	- ID-23-2, EMBL, ESRF, Grenoble
Centrifuges	- 5415R/5415C/5804R/5810R MinispinPlus (Eppendorf, Germany)
	- Thinky ARE-250 (Intertronics, UK)
Crystallization robots	- Honeybee 961 (Genomic Solutions, USA)
	- Oryx4 (Douglas Instruments, UK)
CD-Spectrometer	J-815 (Jasco, UK)
DLS instrumentation	- Spectrolight300 (XtalConcepts, Germany)
	- Spectrolight600 (XtalConcepts, Germany)
DDLs instrument	Development project (XtalConcepts, Germany)
Freezer -20 °C	- Liebherr premium (Liebherr, Germany)
	- B35-85 (FRYKA-Kältetechnik, Germany)
Imaging	- CLSM Zeiss
	- CrystalScore (Diversified Scientific Inc., USA)
	- Microscope SZX12 with camera DP10 (Olympus, Japan)
Incubator	- RUMED 3001 (Rubarth, Germany)
	- Heraeus B6120 (Heraeus, Germany)
Mask Aligner	MJB4 (SÜSS Microtec, Germany)
Microbalance	Sartorius TE3102S (Sartorius, Germany)
pH Meter	SevenEasy (Mettler-Toledo, Switzerland)
Photospectrometry	Nanodrop 2000c (ThermoScientific, Peqlab, Germany)
Pipetting robots	Lissy (Zinsser, Germany)

Plasma cleaner	Zepto (Diener electronic, Germany)
Real-Time PCR instrument	MyiQ-RT (Biorad, Germany)
Scanning electron microscope	FEI XL-30 (FEI, Germany)
SDS-PAGE	- Four Gel Caster (SE275) - EV 231 (Peqlab, Germany) - SE260 Mighty Small II Deluxe Mini (Hoefer, US)
SONICC	SONICC (Formulatrix, Germany)
Sonifier ultrasonic cell disruptor	Sonifier S-250A 200 W (Emerson Electric Co, US)
Sputter coater	Q150T (Quorum Technologies, UK)
Thermocycler	Mastercycler gradient (Eppendorf, Germany)
Transmission electron microscope	FEI Tecnai G20 (FEI, Germany)
UV-light source	CrystalLIGHT 100 (Nabitec, Germany)
X-ray source	RU 200 X-ray generator (Rigaku, Germany)
XtalController	Spectrolight900 (XtalConcepts, Germany)

GHS and Risk Symbols



Figure Appendix 1: GHS pictograms (from <https://www.ohsa.gov>)

Chemicals used (GHS classification)

Table 12: Chemicals (listed alphabetically).

Compound	CAS-No.	Supplier	GHS hazard	Hazard Statements	Precautionary Statements
Acetic acid	64-19-7	Chem-solute	GHS02 GHS05	H226, H314	P280, P305+351+338, P310
Acrylamide 37%	79-06-1	Carl Roth	GHS06 GHS08	H301, H312, H315, H317, H319, H332, H340, H350, H361f, H372	P201, P280, P301+310, P305+351+338, P308+313
AHT	13803-65-1	IBA	GHS07 GHS08	H319, H361d	P264, P281, P305+P351+P338, P337+P313
APTS	919-30-2	Sigma	GHS05 GHS07	H302-H314- H317	P280-P305 +P351 +P338-P310
ATP	34369-07-8	Sigma	-	-	-
Agarose	9012-36-6	Serva	-	-	-
(NH ₄) ₂ SO ₄	7283-20-2	Carl Roth	-	-	-
NH ₄ NO ₃	6484-52-2	Applichem	GHS03	H272	P210
Ampicillin	69-52-3	Carl Roth	GHS08	H334, H317	P280, P261, P302+352, P342+311
APS	7727-54-0	Carl Roth	GHS03 GHS07 GHS08	H272, H302, H315, H317, H319, H334, H335	P280, P305+351+338, P302+352, P304+341, P342+311
Bromphenol blue	115-39-9	Applichem	-	-	-
CaCl ₂	10043-52-4	Merck	GHS07	H319	P305+351+338
Ca(H ₃ CCOO) ₂	114460-21-8	Sigma	-	H315, H319, H335	P261, P305+351+338
Chloramphenicol	56-75-7				
Citric acid	77-92-9	Sigma	GHS05	H318	P305+351+338, P311
Coomassie Brilliant Blue R250	6104-59-2	Serva	-	-	-
Desthiobiotin	533-48-2	Sigma	-	-	-
DTT	578517	Applichem	GHS07	H302, H315, H319, H335	P302+352, P305+351+338
EDTA	60-00-4	Sigma	GHS07	H319	P305+351+338
Ethanol	64-17-5	Carl Roth	GHS02	H225	P210

Compound	CAS-No.	Supplier	GHS hazard	Hazard Statements	Precautionary Statements
Ethidium bromide	1239-45-8	Sigma	GHS06 GHS08	H302, H331, H341	P260, P281, P284, P310
Glutaraldehyde	111-30-8	Sigma	GHS05 GHS06 GHS08 GHS09	H301+H331, H314-H317, H334-H335, H400-H411	P221-P273-P280-P301 +P310- P305 +P351 +P338-P310
Glycerol	56-81-5	Sigma	-	-	-
GPTS	2530-83-8	Sigma	GHS05	H318	P280-P305 +P351 +P338
HABA	1634-82-8	Fluka	GHS07	H315, H319, H335	P261, P305+351+338
Hepes	7365-45-9	Sigma Aldrich	-	-	-
Hydrochloric acid >25 %	7647-01-0	Merck	GHS05 GHS07	H314, H335	P261, P280, P310, P305+351+338
Imidazole	288-32-4	Carl Roth	GHS05 GHS06 GHS08	H301, H314, H361	P260, P281, P303+361+353, P301+330+331, P305+351+338, P308+313
IPTG	367-93-1	Sigma	-	-	-
Isopropanol	67-63-0	Carl Roth	GHS02 GHS07	H225, H319, H336.	P210, P233, P305+351+338
KCl	7447-40-7	Carl Roth	-	-	-
LiCl	7447-41-8	Merck	GHS07	H302, H315, H319, H335	P302+352, P305+351+338
Li2SO4	10102-25-7	Merck	GHS07	H302	-
Malonic acid	141-82-2	Sigma	GHS05 GHS07	H318, H302, H335, H315	P261, P280, P304+340, P305+351+338, P405, P501
Mg(HCOO)2	6150-82-9	Fluka	-	-	-
MgCl2	7786-30-3	Carl Roth	-	-	-
MPD	107-41-5	Carl Roth	GHS07	H315, H319	-
2-Mercaptoethanol	60-24-2	Fisher Scientific	GHS06 GHS09	H302, H411, H315, H335, H311, H319	P280, P312, P302+350, P261, P273, P301+312, P305+351+338
NaOAc	127-09-3	Applichem	-	-	-
NaCl	7647-14-5	Carl Roth	-	-	-
NaH2PO4	10049-21-5	Applichem	-	-	-
NaOH	1310-73-2	Merck	GHS05	H314	P280, P310, P305+351+338
Na3 citrate	6132-04-3	Sigma	-	-	-

Compound	CAS-No.	Supplier	GHS hazard	Hazard Statements	Precautionary Statements
Ni(II)SO4	10101-97-0	Applichem	GHS07 GHS08 GHS09	H302+332, H315, H317, H334, H341, H350i, H360d, H372 H410	P201, P261, P273, P280, P284, P304+340+312
Paraffin	8002-74-2	Applichem	-	-	-
PDMS	63148-62-9	Sigma	-	H413	-
PEG 10000	25322-68-3	Merck	-	-	-
PEG 1500	25322-68-3	Fluka	-	-	-
PEG 2000 MME	25322-68-3	Fluka	-	-	-
PEG 300	25322-68-3	Applichem	-	-	-
PEG 3350	25322-68-3	Sigma	-	-	-
PEG 400	25322-68-3	Sigma	-	-	-
PEG 4000	25322-68-3	Merck	-	-	-
PEG 6000	25322-68-3	Merck	-	-	-
PEG 8000	25322-68-3	Sigma	-	-	-
PGMEA	108-65-6	Sigma	GHS02	H226	P210-P403+P235
PMSF	329-98-6	Applichem	GHS06 GHS05	H301, H314	P280, P305 + P351 + P338, P310
SDS	151-21-3	Sigma	GHS02 GHS06	H228, H302, H311, H315, H319, H335	P210, P261, P280, P312, P305+351+338
Sodium borate	1303-96-4	Sigma	GHS08	H360FD	P201, P308 +313
Sodium citrate	1545832	Sigma	-	-	-
Sodium tartrate	868-18-8	Applichem	-	-	-
SU-8 3000	96-48-0 89452-37-9 71449-78-0 108-32-7 28906-96-9	MicroChem	GHS02 GHS07 GHS08 GHS09	H226, H302+H332, H315, H317, H319, H341, H411	P210, P261, P280, P233, P273, P201, P305+P351+P338, P312, P363, P308+P313, P333+P313, P337+P313, P370, P378, P391, P403+P235, P501
SYPRO Orange	67-68-5	Sigma	-	-	-
TEMED	110-18-9	Merck	GHS02 GHS05 GHS07	H225, H302, H314, H332	P261, P280, P305+351+338
Tris	1185-53-1	Fluka	GHS07	H315, H319, H335	P261, P305+351+338
Yeast Extract	8013-01-2	Serva	-	-	-

Protein crystallization and stability screens

Table 13: Protein crystallization and stability screens (listed alphabetically).

Compound	Supplier	GHS hazard	Hazard Statements	Precautionary Statements
AmSO₄ Suite	Qiagen	GHS02 GHS06 GHS08 GHS09	H225, H301, H330, H350, H340, H360FD, H372, H411	P101, P201, P273, P280, P309+311
Classics Suite	Qiagen	GHS02 GHS06 GHS07 GHS08 GHS09	H225, H301, H302, H315, H319, H331, H332, H335, H340, H350, H360FD, H373, H411	P101, P201, P270, P280, P305+351+338, P309+311, P313
Cryos Suite	Qiagen	GHS02 GHS06 GHS07 GHS08 GHS09	H225, H301, H302, H315, H319, H331, H332, H335, H340, H350, H360FD, H373, H411	P101, P201, P270, P273, P280, P305+351+338, P309+311, P313
JCSG-plus	Molecular Dimensions	GHS02 GHS05 GHS06 GHS07 GHS08	H225, H301, H312, H315, H318, H331, H335, H350, H411	P101, P201, P270, P280, P305+351+338, P309+311, P313
Morpheus	Molecular Dimensions	GHS02 GHS06 GHS07 GHS08 GHS09	H225, H301, H302, H315, H319, H331, H332, H335, H340, H350, H360Fd, H361d, H373, H411	P101, P201, P270, P273, P280, P305+351+338, P309+311, P313
PACT premier	Molecular Dimensions	GHS06	H301, H331, H412	P101, P270, P273, P280, P309+311
Stura FootPrint & MacroSol	Molecular Dimensions	GHS02 GHS06 GHS07 GHS08 GHS09	H225, H301, H302, H315, H319, H332, H335, H340, H350, H360FD, H373, H411	P101, P201, P270, P273, P280, P305+351+338, P309+311, P313
RUBIC buffer screen	Molecular Dimensions	GHS05 GHS07 GHS08	H315, H319, H302, H314, H318, H335, H360D	P261, P305+P351+P338, P201, P280, P310
RUBIC additive screen	Molecular Dimensions	GHS02 GHS05 GHS06 GHS07 GHS08 GHS09	H315, H225, H302, H301, H319, H316, H290, H303, H314, H272, H301+H311+H331, H311, H317, H313, H318, H335, H370, H331, H334, H360D, H333, H400, H410, H341, H412, EUH032, H336, H350i, EUH066, H360F, H372	P261, P305+P351+P338, P280, P201, P273, P301+P310, P220, P302+P352, P310, P311, P308+P313, P501

GHS Hazard Statements

H225	Highly flammable liquid and vapor
H226	Flammable liquid and vapor
H228	Flammable solid
H272	May intensify fire; oxidizer
H290	May be corrosive to metals
H301	Toxic if swallowed
H302	Harmful if swallowed
H303	May be harmful if swallowed
H311	Toxic in contact with skin
H312	Harmful in contact with skin
H313	May be harmful in contact with skin
H314	Causes severe skin burns and eye damage
H315	Causes skin irritation
H316	Causes mild skin irritation
H317	May cause an allergic skin reaction
H318	Causes serious eye damage
H319	Causes serious eye irritation
H330	Fatal if inhaled
H331	Toxic if inhaled
H332	Harmful if inhaled
H333	May be harmful if inhaled
H334	May cause allergy or asthma symptoms or breathing difficulties if inhaled
H335	May cause respiratory irritation
H336	May cause drowsiness or dizziness
H340	May cause genetic defects
H341	Suspected of causing genetic defects
H350	May cause cancer
H350i	May cause cancer by inhalation
H360	May damage fertility or the unborn child
H360D	May damage the unborn child
H360F	May damage fertility
H360Fd	May damage fertility. Suspected of damaging the unborn child
H360FD	May damage fertility. May damage the unborn child
H361	Suspected of damaging fertility or the unborn child
H361d	Suspected of damaging the unborn child.
H361f	Suspected of damaging fertility
H370	Cause damage to organs
H372	Causes damage to organs through prolonged or repeated exposure
H373	May cause damage to organs through prolonged or repeated exposure.
H400	Very toxic to aquatic life with long-lasting effects
H410	Very toxic to aquatic life with long lasting effects
H411	Toxic to aquatic life with long lasting effects
H412	Harmful to aquatic life with long lasting effects.
EUH032	Contact with acids liberates very toxic gas
EUH066	Repeated exposure may cause skin dryness or cracking

GHS Precautionary Statements

P101	If medical advice is needed, have product container or label at hand
P201	Obtain special instructions before use
P210	Keep away from heat/sparks/open flames/hot surfaces – No smoking
P233	Keep container tightly closed
P260	Do not breathe dust/fume/gas/mist/vapors/spray
P261	Avoid breathing dust/fume/gas/mist/vapors/spray
P264	Wash thoroughly after handling
P270	Do not eat, drink or smoke when using this product
P273	Avoid release to the environment
P281	Use personal protective equipment as required
P280	Wear protective gloves/protective clothing/eye protection/face protection
P284	Wear respiratory protection
P309	IF exposed or you feel unwell
P310	Immediately call a POISON CENTER or doctor/physician
P311	Call a POISON CENTER or doctor/physician
P312	Call a POISON CENTER or doctor/physician if you feel unwell
P321	Specific treatment (see respective MSDS)
P330	Rinse mouth
P362	Take off contaminated clothing and wash before reuse
P391	Collect spillage.
P405	Store locked up
P501	Dispose of contents/container in accordance with local/regional/national/international regulations
P301+P310	IF SWALLOWED: Immediately call a POISON CENTER or doctor/physician
P301+P312	IF SWALLOWED: Call a POISON CENTER or doctor/physician if you feel unwell
P301+P330+P331	IF SWALLOWED: Rinse mouth. Do NOT induce vomiting
P302+P352	IF ON SKIN: Wash with soap and water
P303+P361+P353	IF ON SKIN (or hair): Remove/Take off immediately all contaminated clothing. Rinse skin with water/shower
P304+P341	IF INHALED: If breathing is difficult, remove victim to fresh air and keep at rest in a position comfortable for breathing
P305+P351+P338	IF IN EYES: Rinse cautiously with water for several minutes. Remove contact lenses if present and easy to do - continue rinsing
P308+P313	IF exposed or concerned: Get medical advice/attention
P309+P311	IF exposed or you feel unwell: Call a POISON CENTER or doctor/physician
P332+P313	If skin irritation occurs: Get medical advice/attention
P333+P313	If skin irritation or rash occurs: Get medical advice/attention
P337+P313	If eye irritation persists: Get medical advice/attention.
P342+P311	Call a POISON CENTER or doctor/physician
P370+P378	In case of fire: Use for extinction: Alcohol resistant foam.
P370+P378	In case of fire: Use for extinction: Fire-extinguishing powder.
P370+P378	In case of fire: Use for extinction: Carbon dioxide.
P403+P233	Store in a well-ventilated place. Keep container tightly closed
P403+P235	Store in a well-ventilated place. Keep cool

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CURRICULUM VITAE

Education / Professional Career

- 07/2013 – 09/2016 Research Assistant (PhD student)
Excellence Cluster: Hamburg Center for Ultrafast Imaging (CUI)
“Laboratory for Structural Biology of Infection and Inflammation”
University of Hamburg, Germany
Project title: „Preparation and scoring of protein micro- and nano-
crystals for FEL and synchrotron applications”, Prof. Dr. Christian
Betzel
- 10/2010 – 12/2012 Study of Molecular Life Sciences (Master of Science), University of
Hamburg, Germany
Master thesis with the topic: „Functional and structural
characterisation of pre-processed polyproteins in SARS-
Coronavirus”, Prof. Dr. Christian Betzel
- 10/2006 – 09/2009 Study of Cell biology (Bachelor of Science), University of
Osnabrück, Germany
Bachelor thesis with the topic: „Diffusion dynamics in polymer
supported membranes“, Prof. Dr. Piehler

EIDESSTATTLICHE ERKLÄRUNG

Hiermit versichere ich an Eides statt, die vorliegende Dissertation selbst verfasst und keine anderen als die angegebenen Hilfsmittel benutzt zu haben. Ich versichere, dass diese Dissertation nicht in einem früheren Promotionsverfahren eingereicht wurde. Ferner versichere ich, dass ich noch keine Promotionsversuche an anderen Universitäten unternommen habe.

Hamburg, 15.08.2016

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